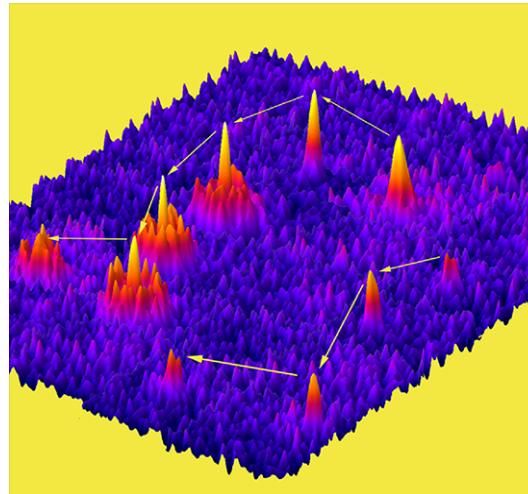


## Course „Optics, Forces & Development“



### Microscopy Tools

Ulrich Kubitscheck

Clausius-Institute of Physical and Theoretical Chemistry  
Rheinische Friedrich-Wilhelms-Universität Bonn

# Contents

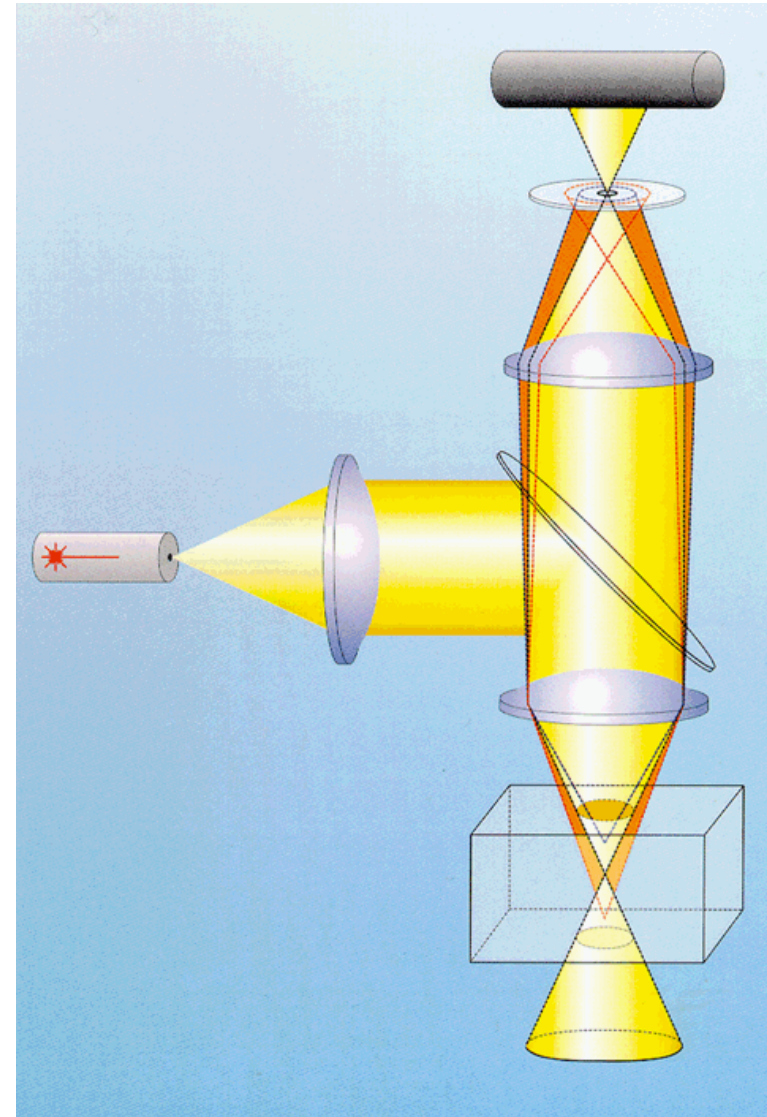
1. Additional Information
2. Basics: waves, diffraction, lenses, aberrations
3. Microscope
4. Two stage microscope
5. Resolution and point spread function (PSF)
6. More PSF: convolution
7. Image detection by cameras and pixel size
8. Objectives
9. Fluorescence
10. Fluorescence microscopy
11. Confocal Microscope
12. 2 photon microscopy
13. Nipkow disk confocal microscope
14. Light sheet fluorescence microscopy
15. Super resolution microscopy: expansion and STED microscopy
16. Light as tool: fluorescence photobleaching and optical tweezers

# The confocal principle

---

Combination of focussed laser illumination  
and  
detection through pinhole placed in a  
conjugated optical plane

yields efficient background subtraction  
and axial resolution:  
„Optical Sectioning“

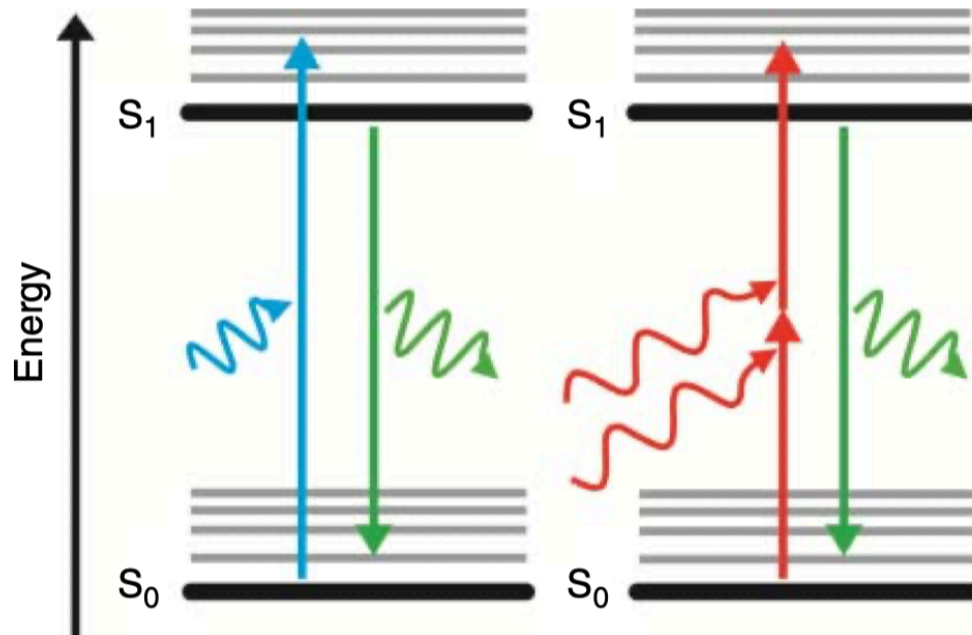


## 12. 2-photon microscopy



# 2-photon fluorescence excitation

---

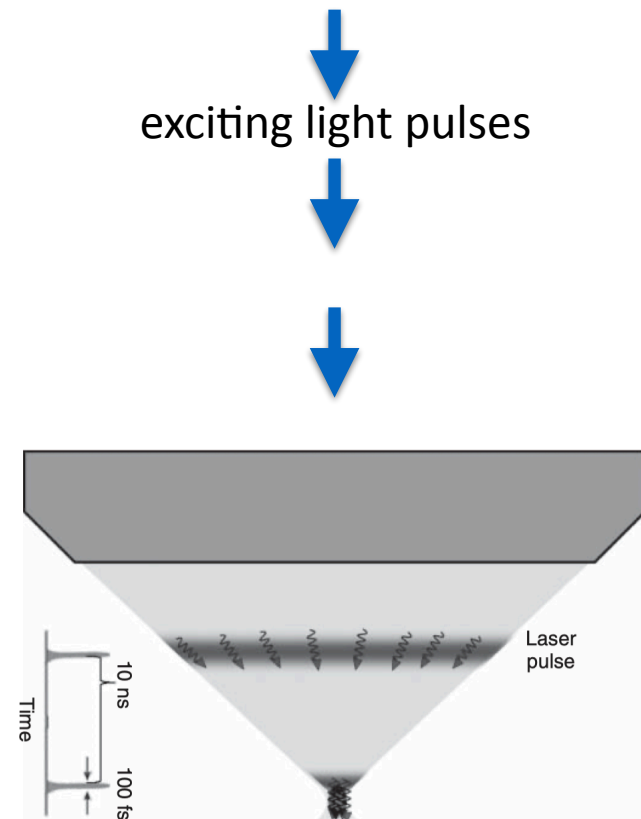
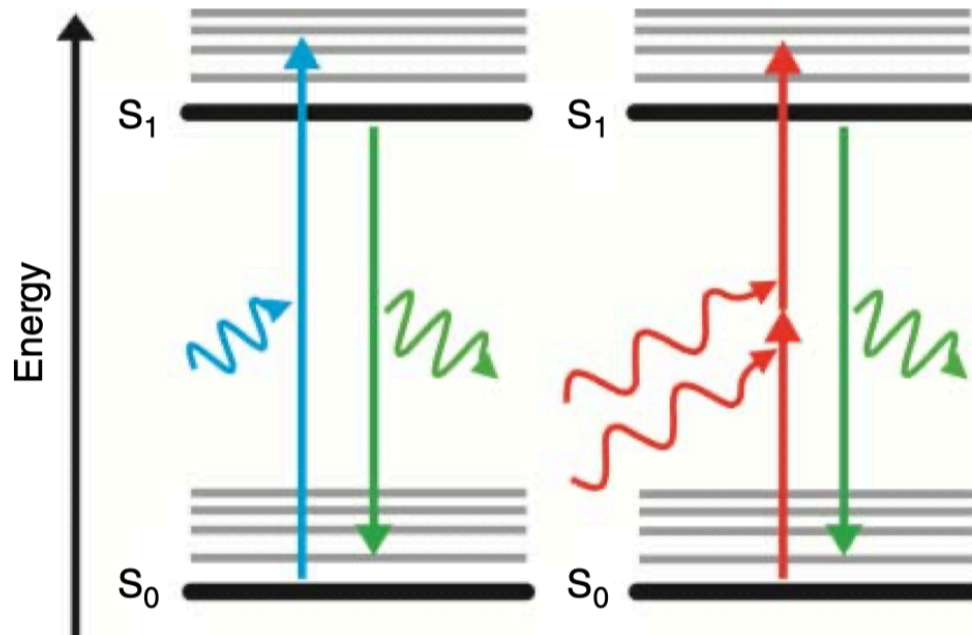


# Parameters for 1 and 2 photon excitation microscopy

---

	<b>One-photon (linear) absorption</b>	<b>Two-photon (non-linear) absorption</b>
1	$N_{\text{ex}} = \sigma I$	$N_{\text{ex}} = \delta I^2$
2	$\sigma = 10^{-16} \text{ cm}^2$	$\delta = 10^{-50} \text{ cm}^4 \text{ s/photon}$
3	$I_{\text{ex}} = 1 \text{ MW cm}^{-2}$	$I_{\text{ex}} = 10^6 \text{ MW cm}^{-2}$
4	CW laser	$t = 10^{-13} \text{ s}$ Freq. = 100 MHz
5	$P_{\text{sat}} = 1 \text{ mW}$	$P_{\text{sat}} = 10 \text{ mW}$

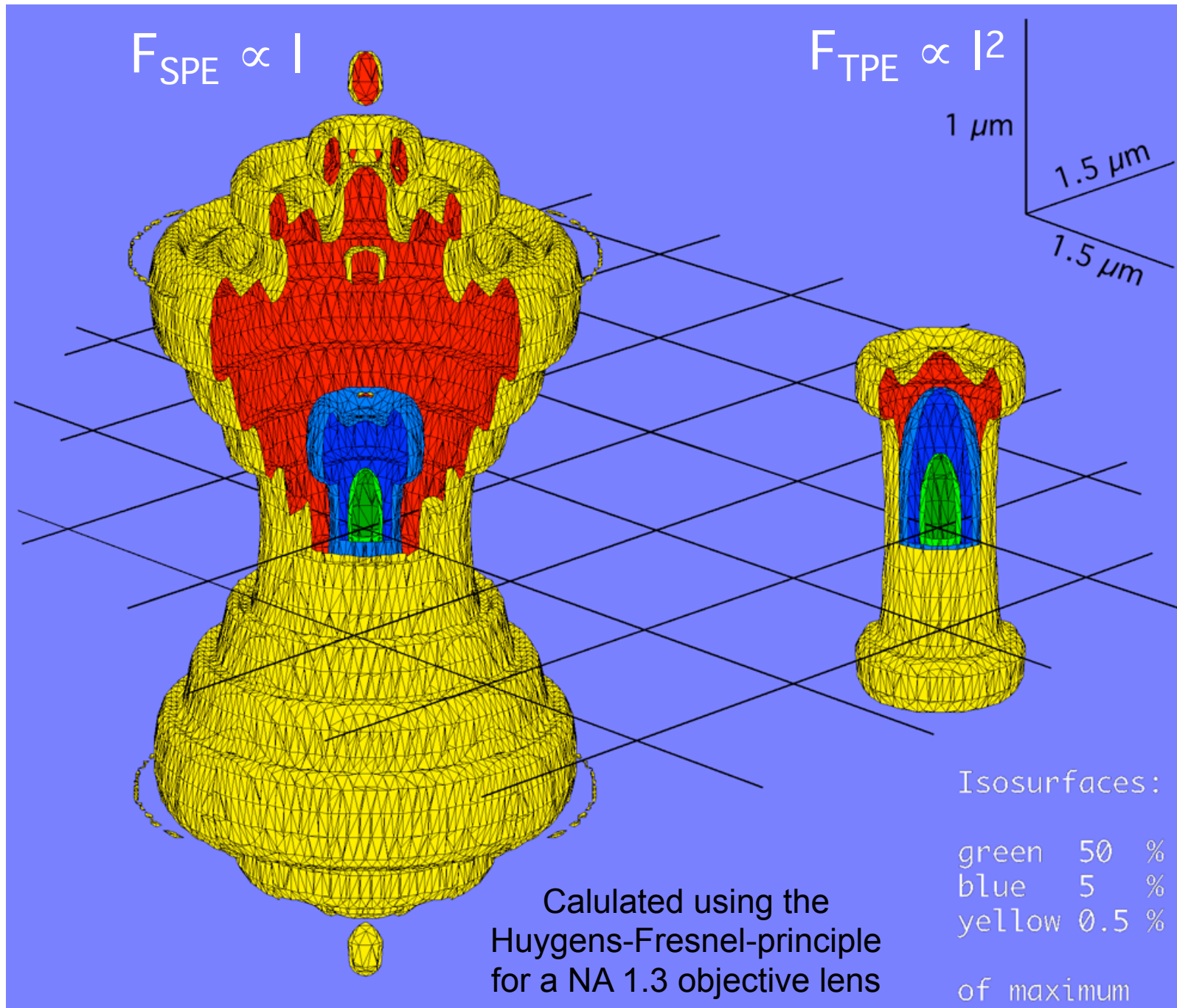
# 2-photon fluorescence excitation



# 1- and 2-Photon Excitation Profiles

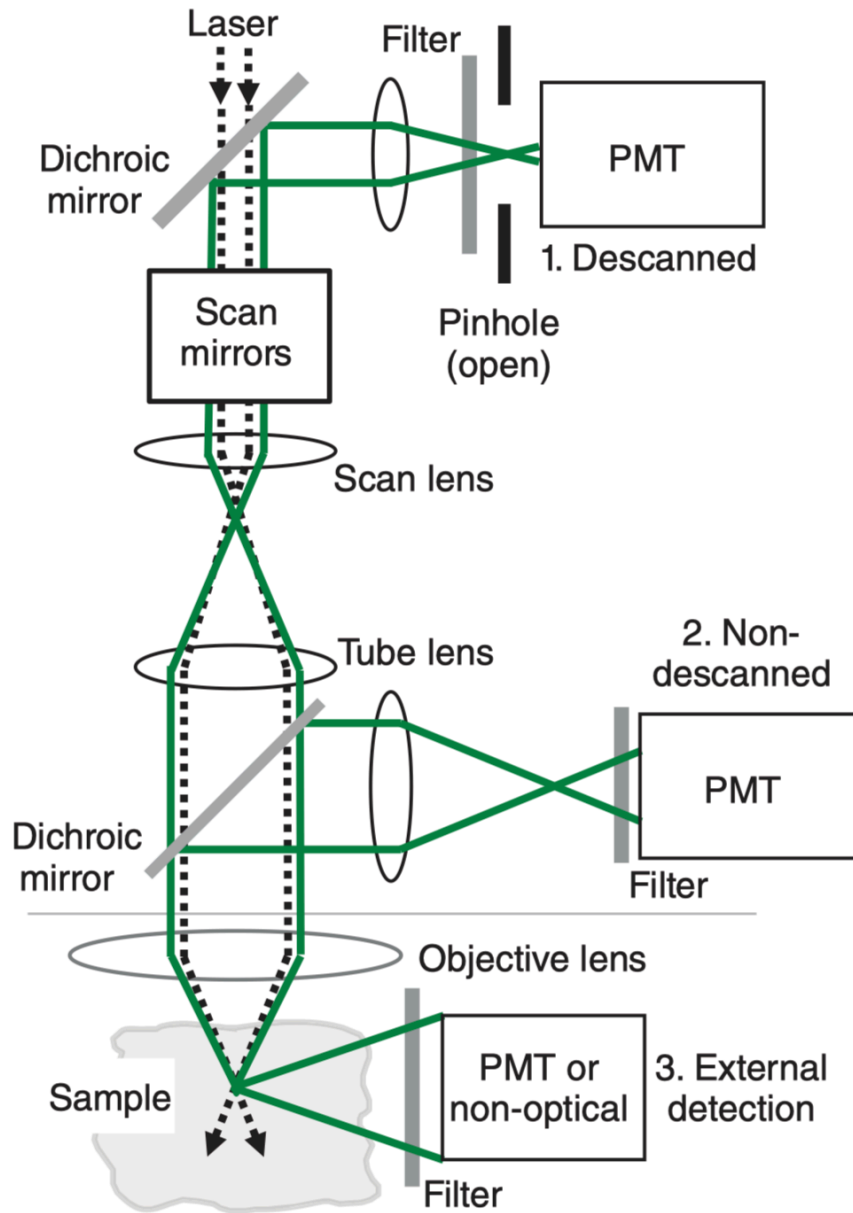
SPE,  $\lambda=488$  nm

TPE,  $\lambda=800$  nm



Calculated using the Huygens-Fresnel-principle for a NA 1.3 objective lens

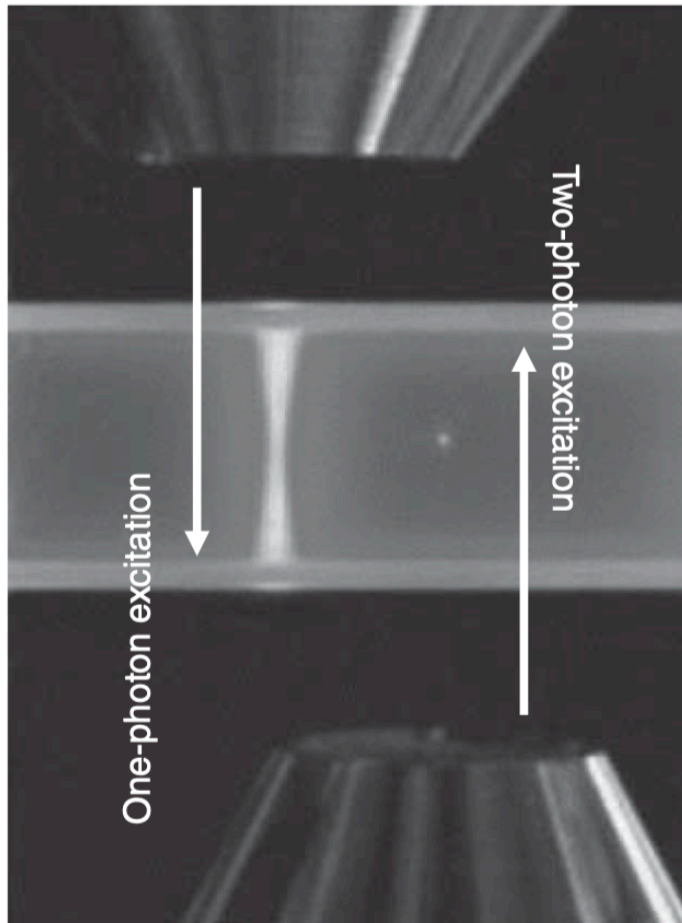
# 2 photon fluorescence microscope



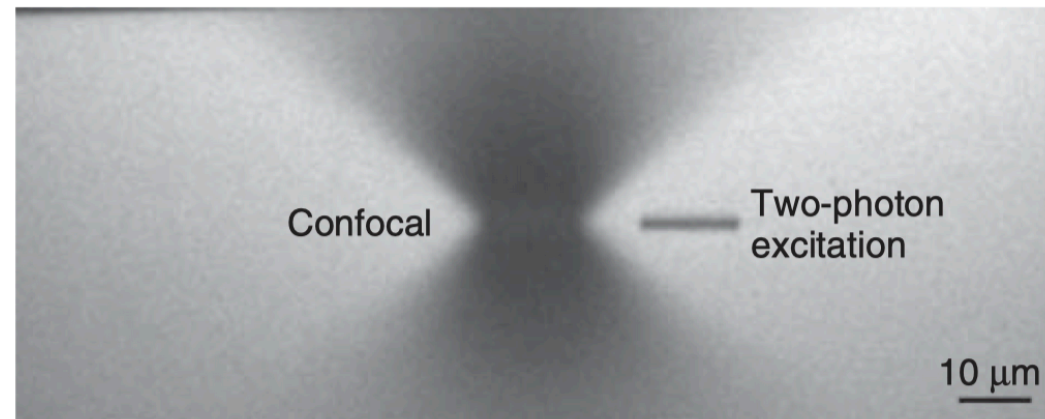
# Localized excitation and bleaching in 2 photon excitation microscopy

---

Excitation



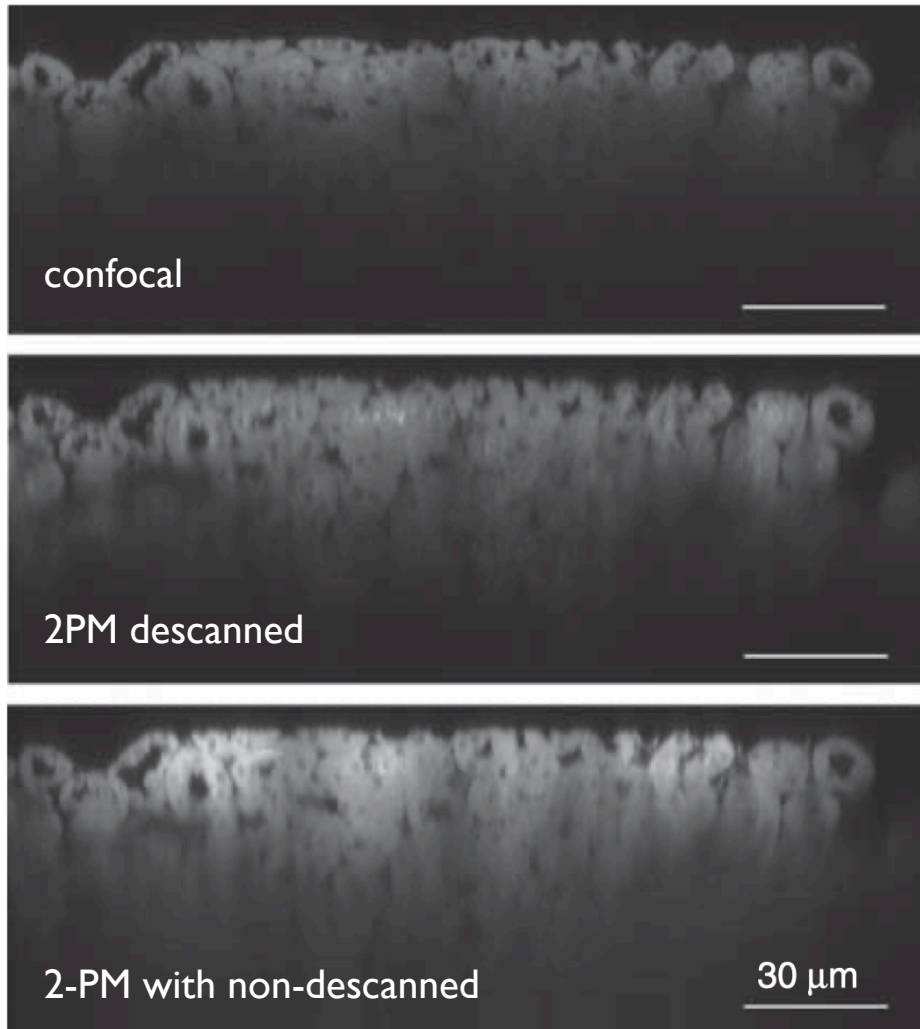
Photobleaching



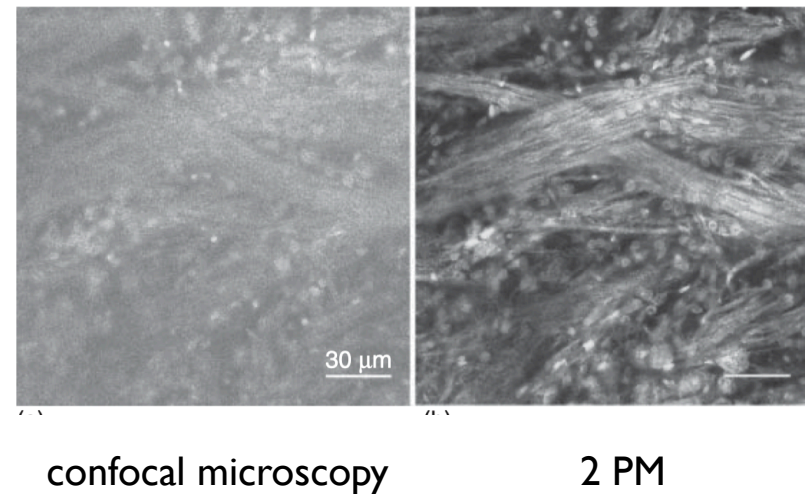


# Penetration depth and contrast in 1 and 2p microscopy

X-Z profiles through an eosin-stained mouse kidney sample imaged in a depth of 70  $\mu\text{m}$  with various detection schemes



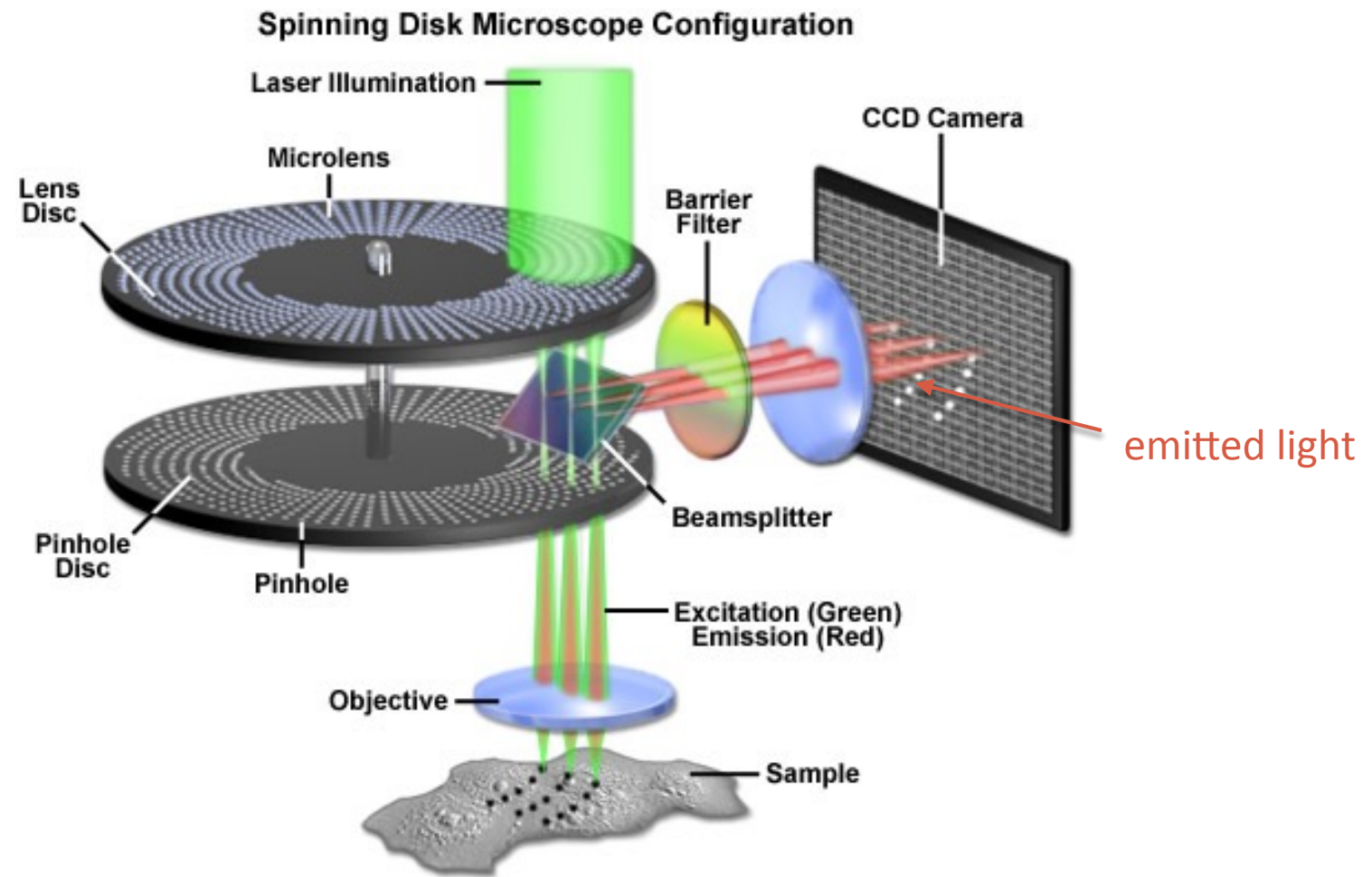
Same X-Y plane imaged 50  $\mu\text{m}$  deep in a rhodamine-stained slice of mouse brain



### 13. Spinning disk confocal microscopy



# Spinning disk confocal microscope



Sketch of how the two Nipkow disks are mounted in the microscope.

Source:  
<http://zeiss-campus.magnet.fsu.edu/articles/livecellimaging/techniques.html>

## Summary: confocal microscopy

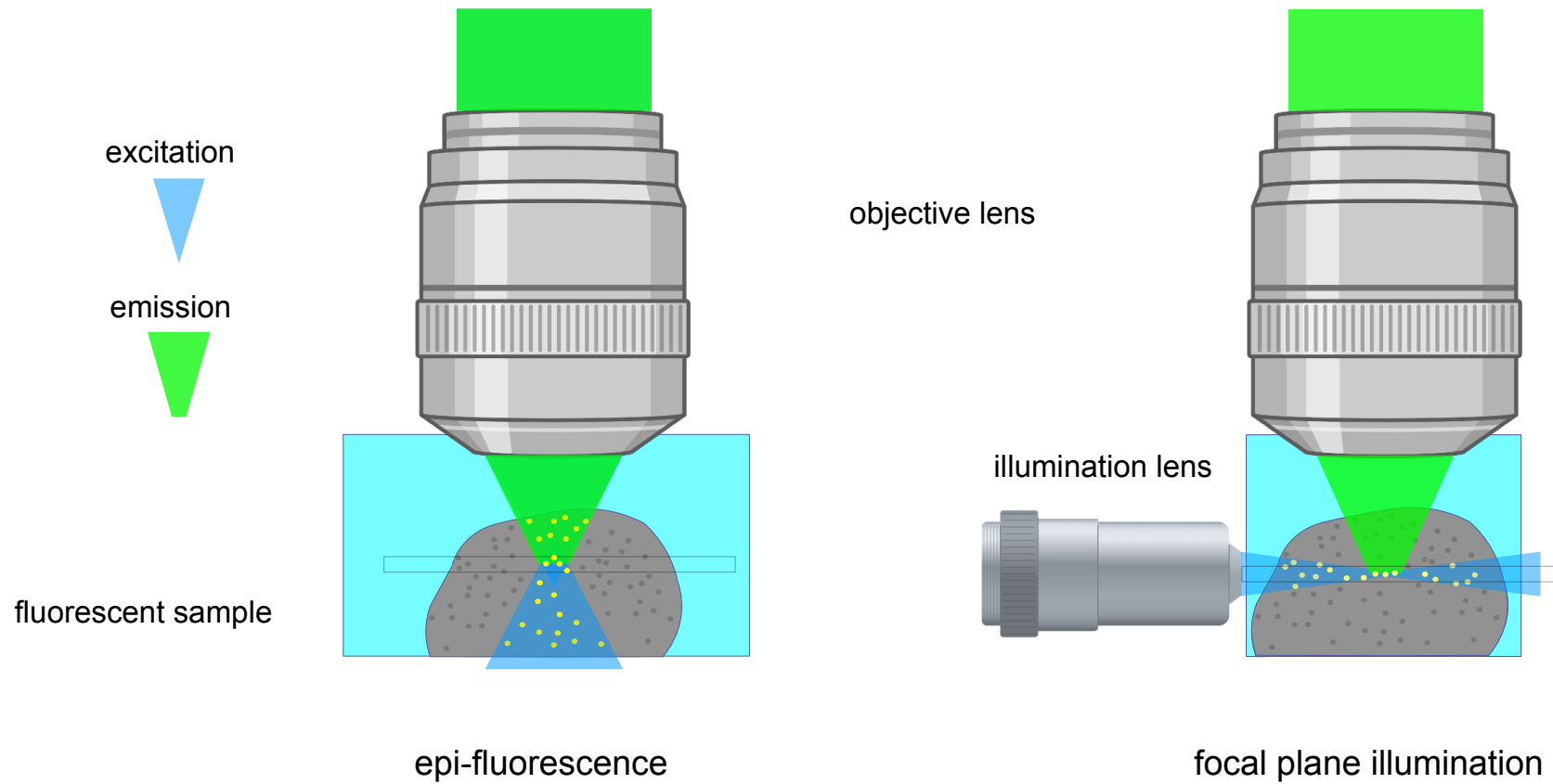
---

- out-of-focus light is reduced by confocal pinhole
- lateral resolution is improved by a factor of up to 1.4
- optical sectioning is possible
- measured intensity is proportional to dye concentration
- 3D-data sets describe spatial structure of objects
- rendering and ray-tracing allow 3D-visualization
- high hard- and software demands
- low light efficiency: about 1‰ - 1% (video microscope 3-10 %)
- 2 photon excitation microscopy yields specific features
- Nipkow disk microscopy allows to speed up imaging

## 14. Light sheet fluorescence microscopy

# High contrast by light-sheet based microscopy

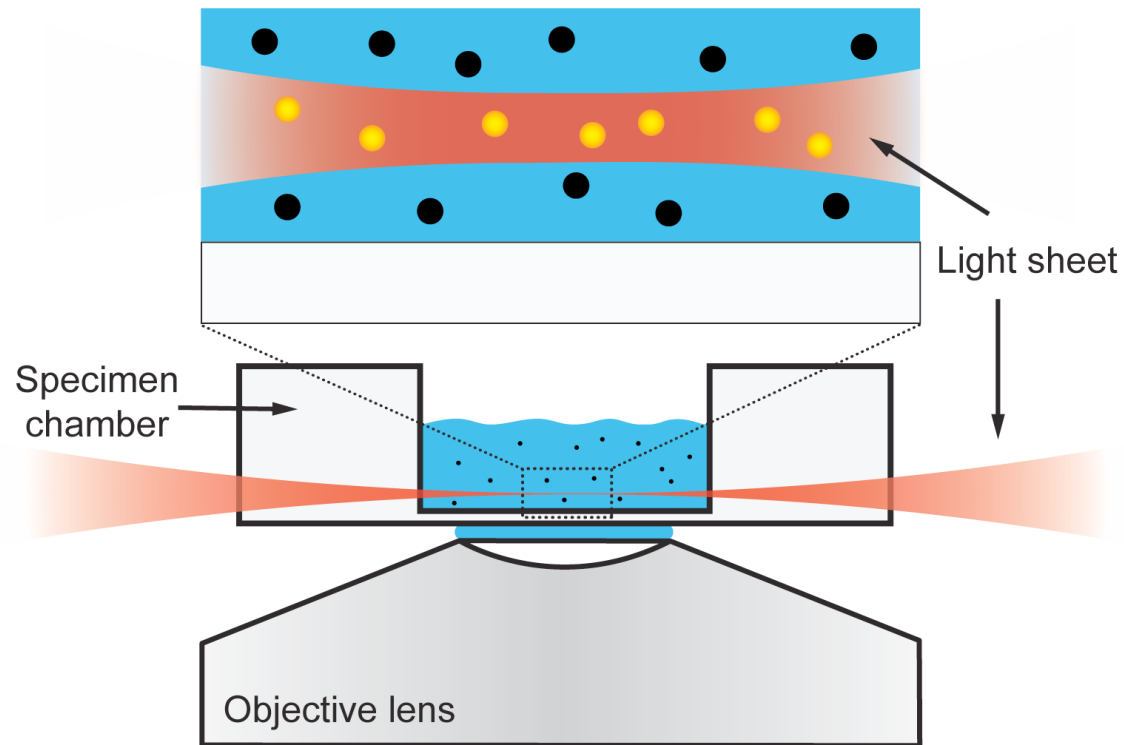
---



Zsigmondy, 1903  
Voie et al, 1993  
Huisken et al., 2004  
Dodt et al., 2007  
.....

# Single molecule imaging in solution

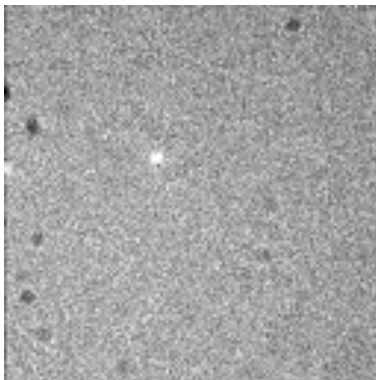
---



# Comparison between epi- and light sheet illumination

---

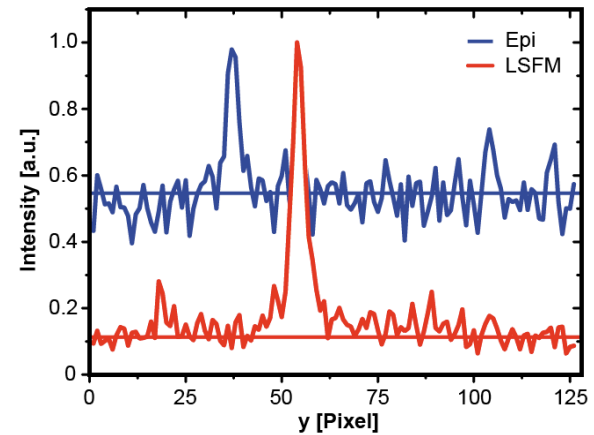
500 kDa dextran-Atto633 in buffer  
40X, NA 1.2W objective lens  
Image field 19.2  $\mu\text{m}$   
Image acquisition 100 Hz, display 33 Hz



Epi-illumination  
Contrast 0.37



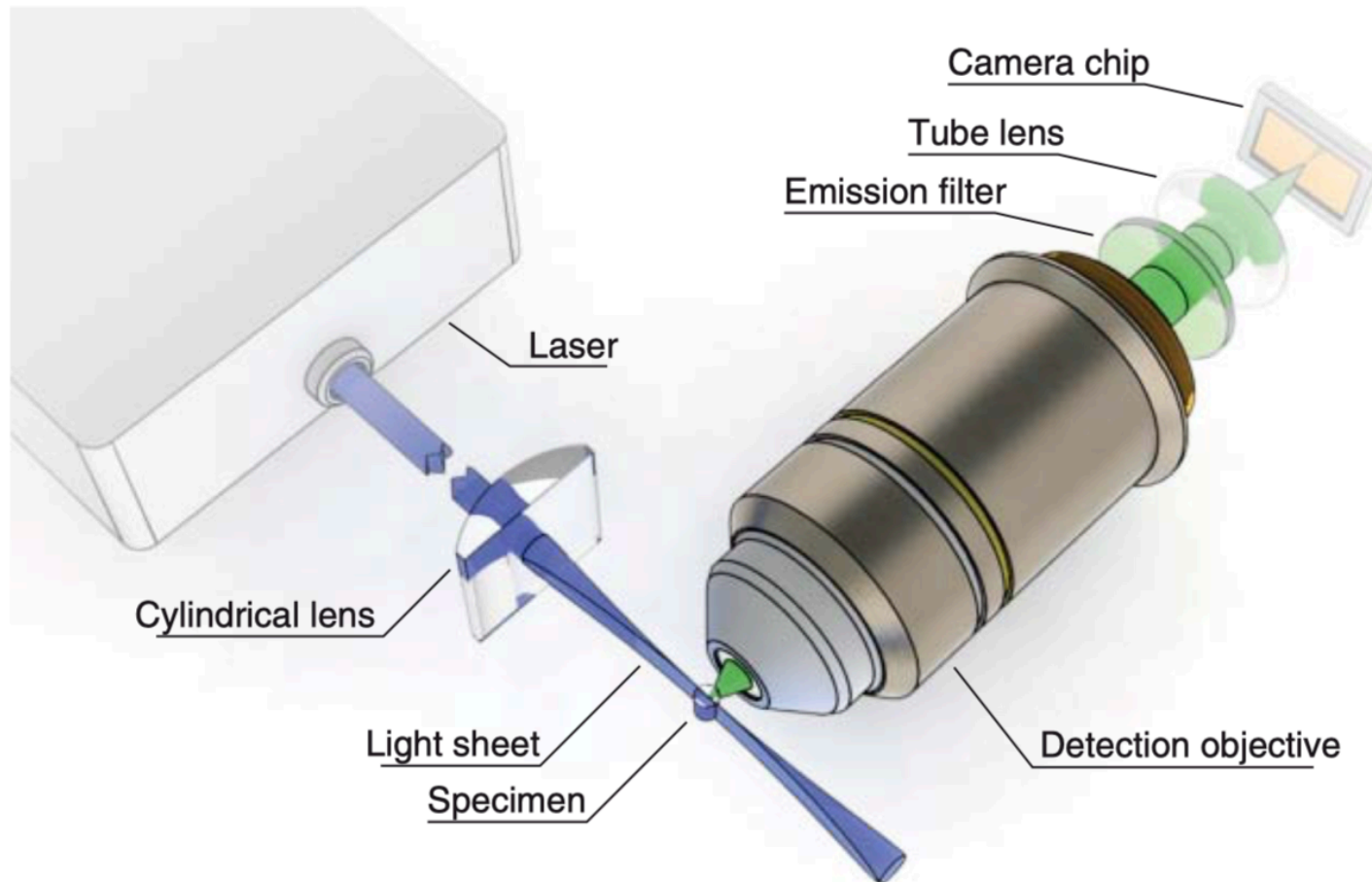
Sheet illumination  
Contrast 0.97



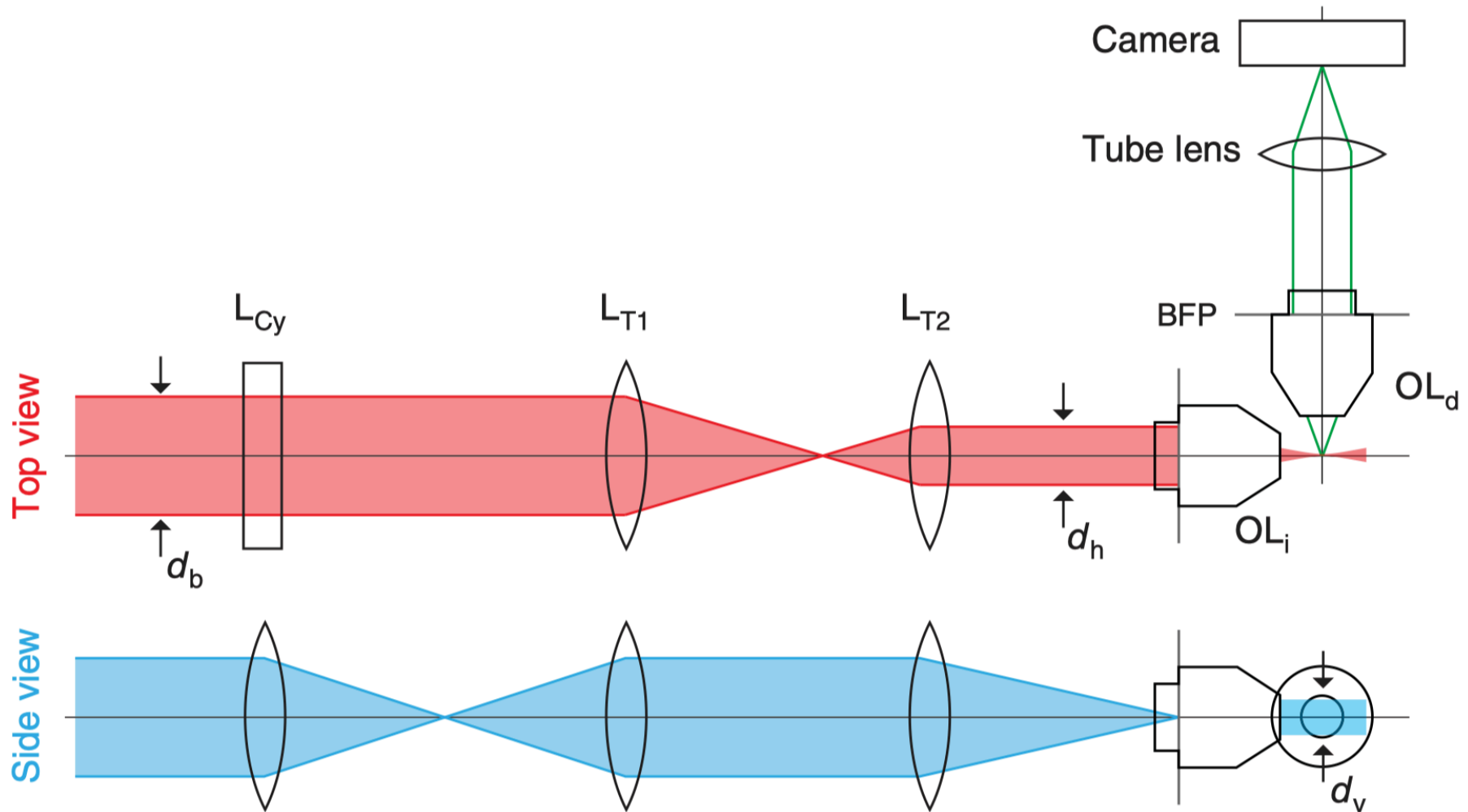
$D = 7.1 \pm 0.2 \mu\text{m}^2/\text{s}$   
as theoretically expected

# Principle of light sheet microscopy

---

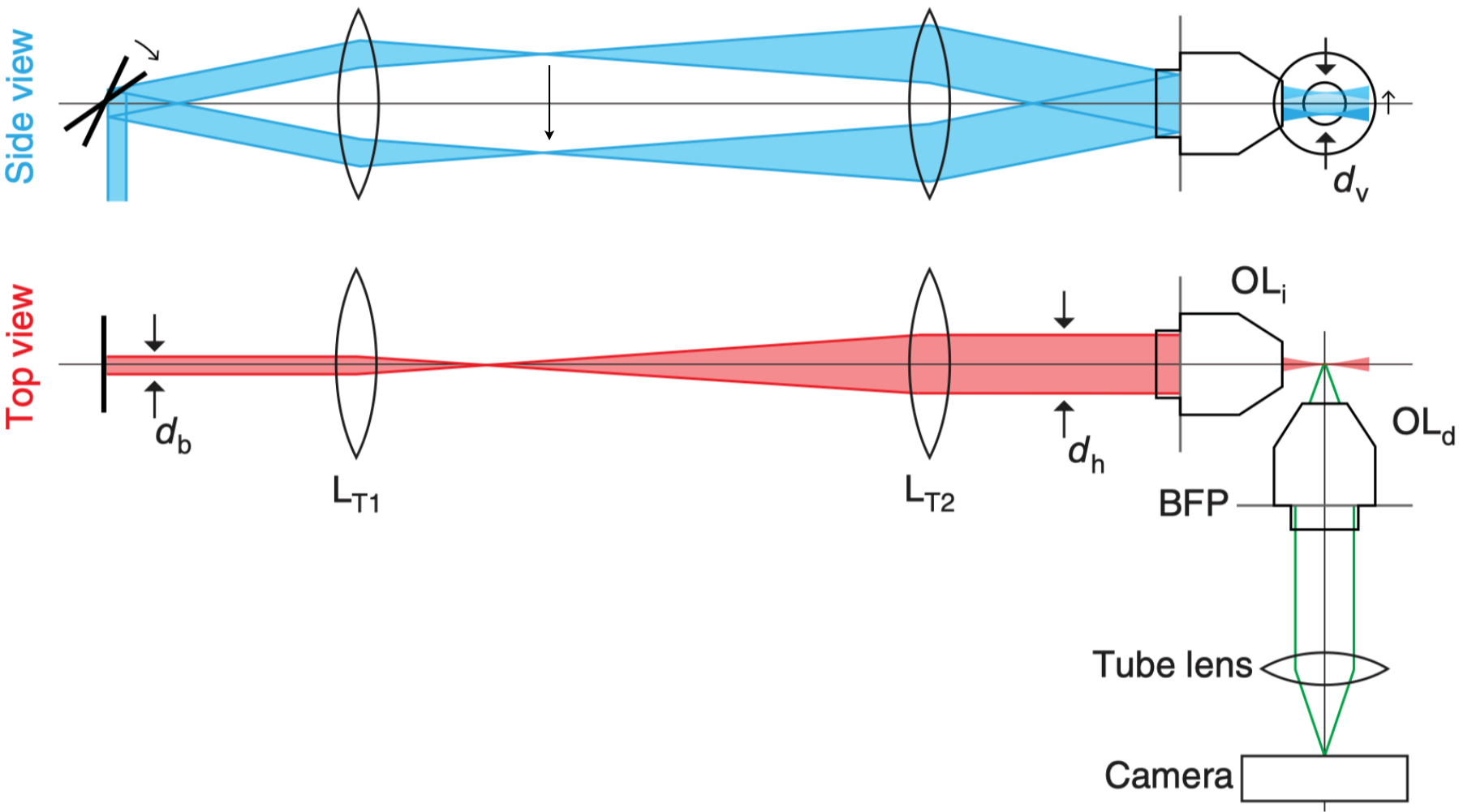


# Light Sheet Microscopy using a cylindrical lens

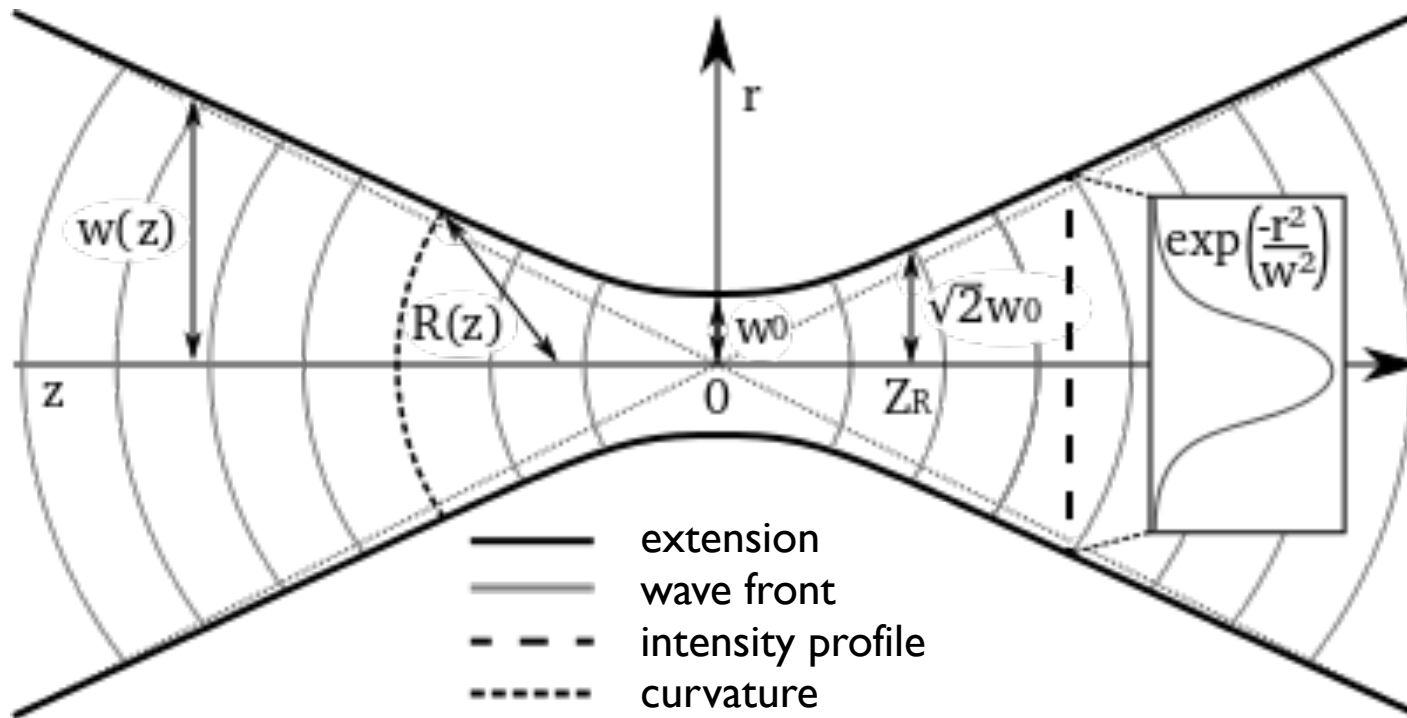




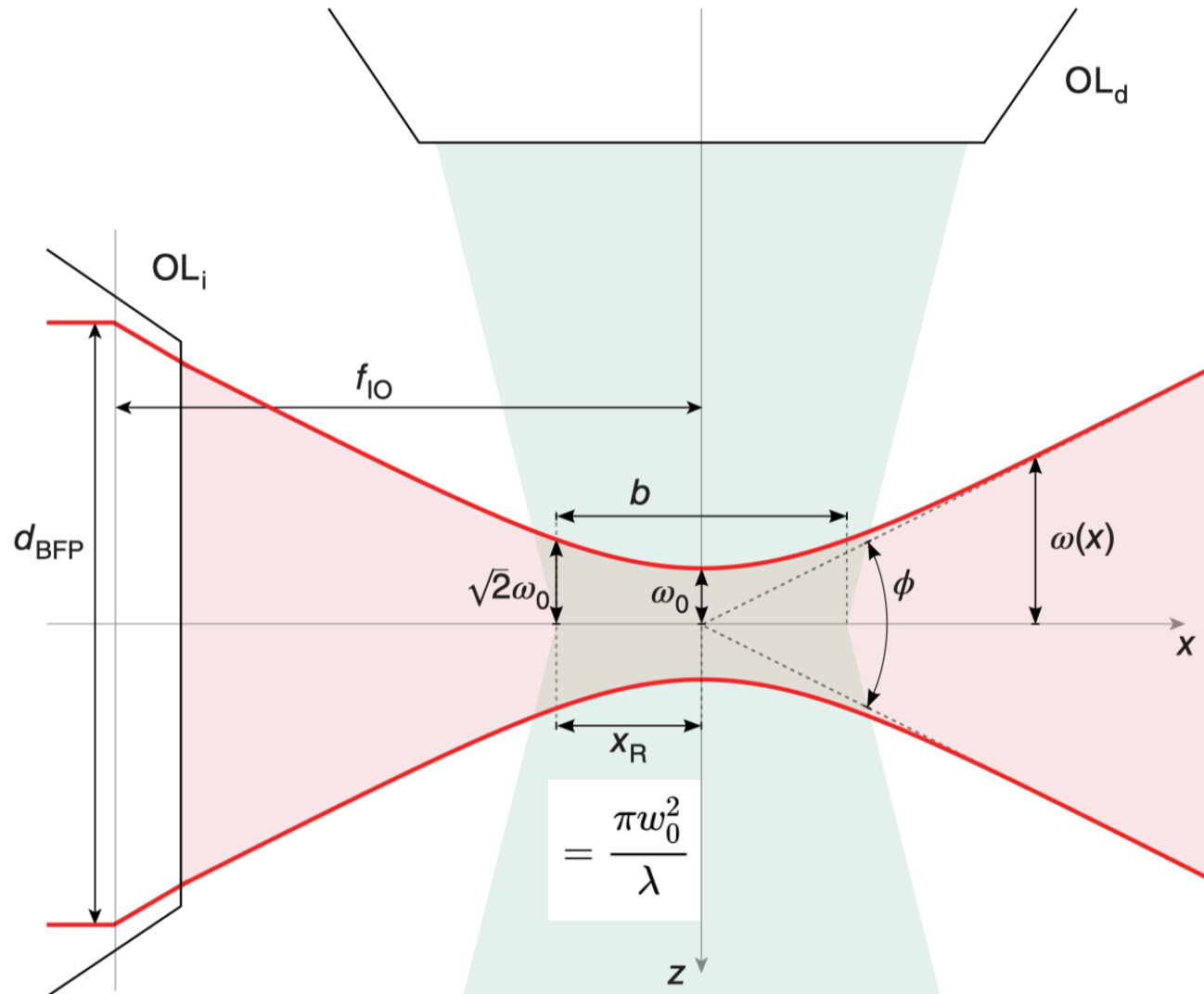
# Scanned Light Sheet Microscopy



# Gaussian beam

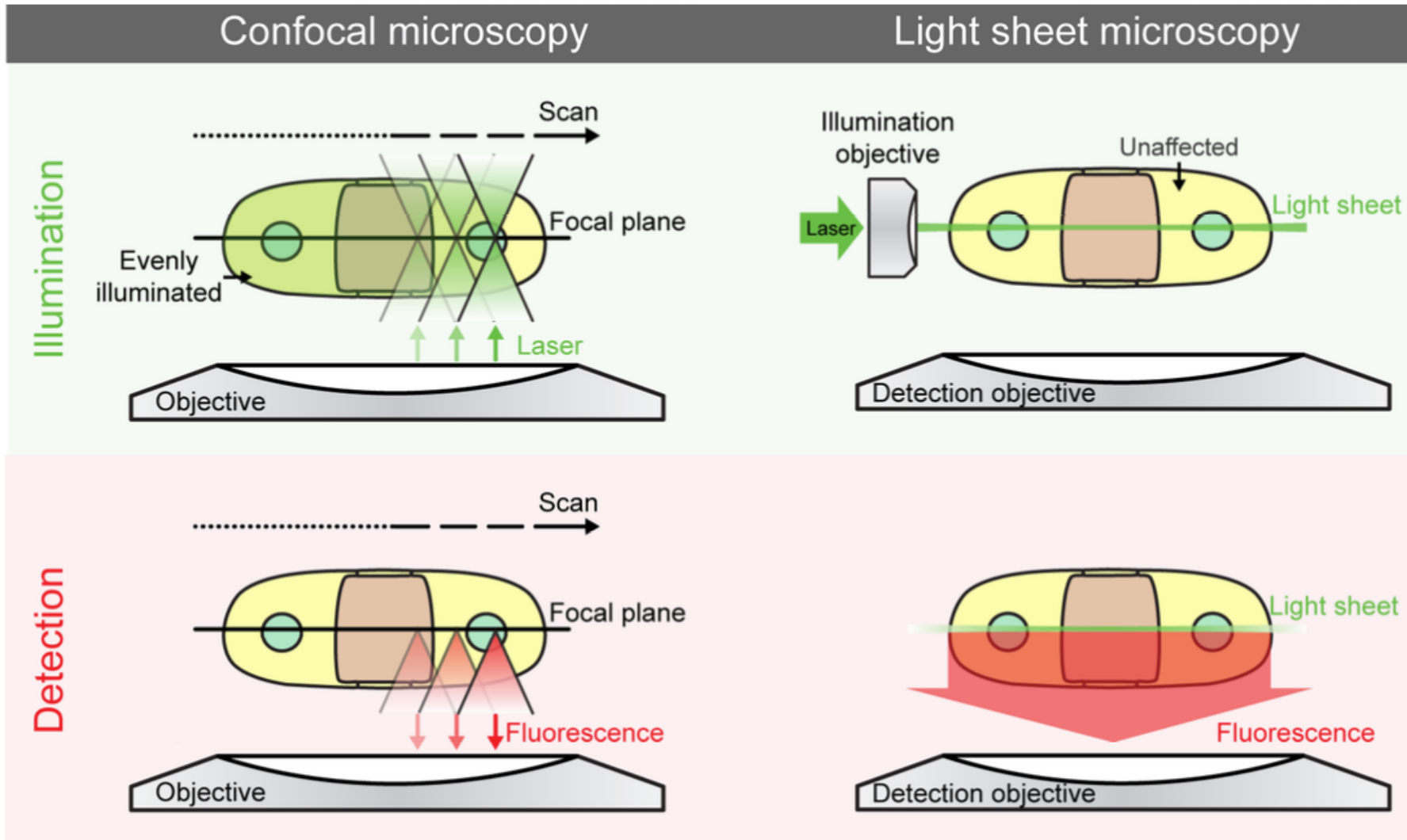


# Relationship between light sheet dimensions and field of view



Gaussian beam illumination:  
limited observation field size  
Width and length are closely related to each other

# Image generation in confocal and light sheet microscopy



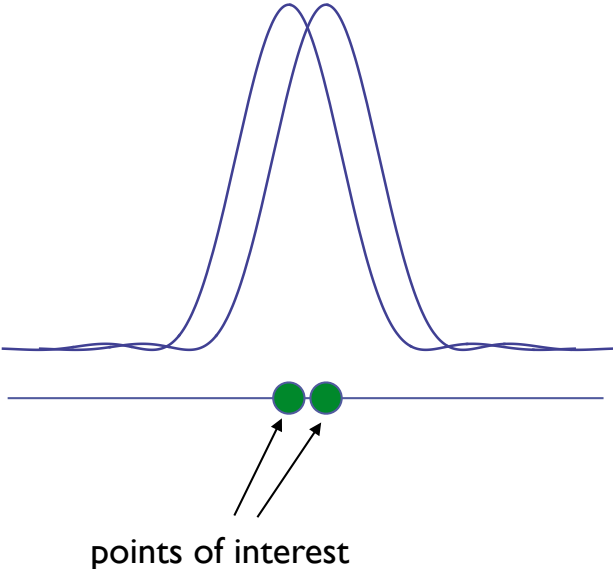
## 15. Super resolution microscopy

- (a) Expansion microscopy
- (b) STED microscopy

# How to image a sample with sub-resolution features?

---

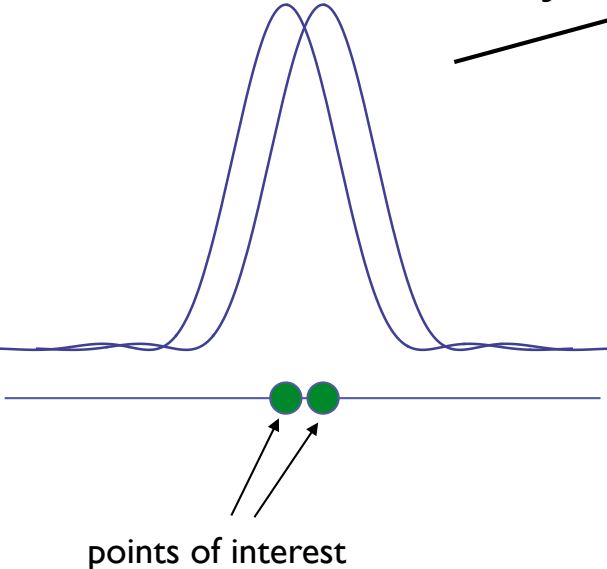
classical microscopy



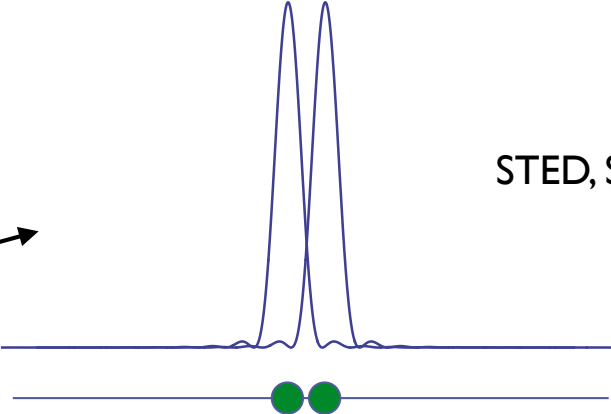
# Increase optical resolution by „sharpening“ the point spread function

---

classical microscopy



sharpen PSF

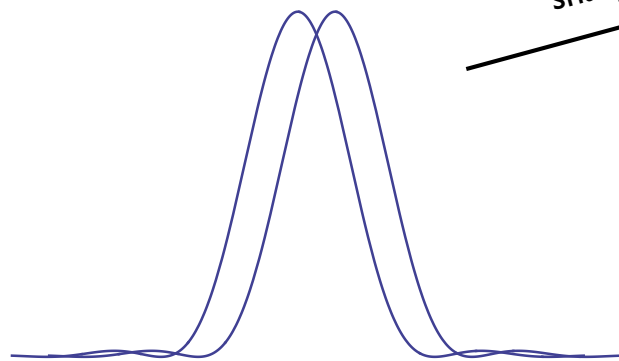


STED, SIM, STORM

# ... or use expansion microscopy

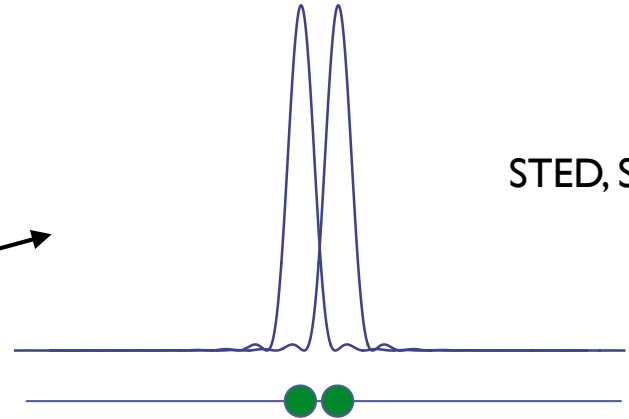
---

classical microscopy



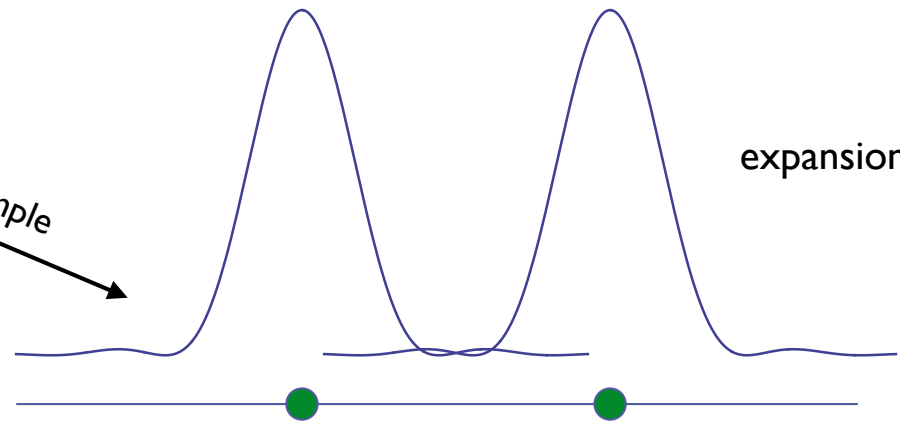
points of interest

sharpen PSF



STED, SIM, STORM

expand sample



expansion microscopy



## I 5a. Expansion microscopy

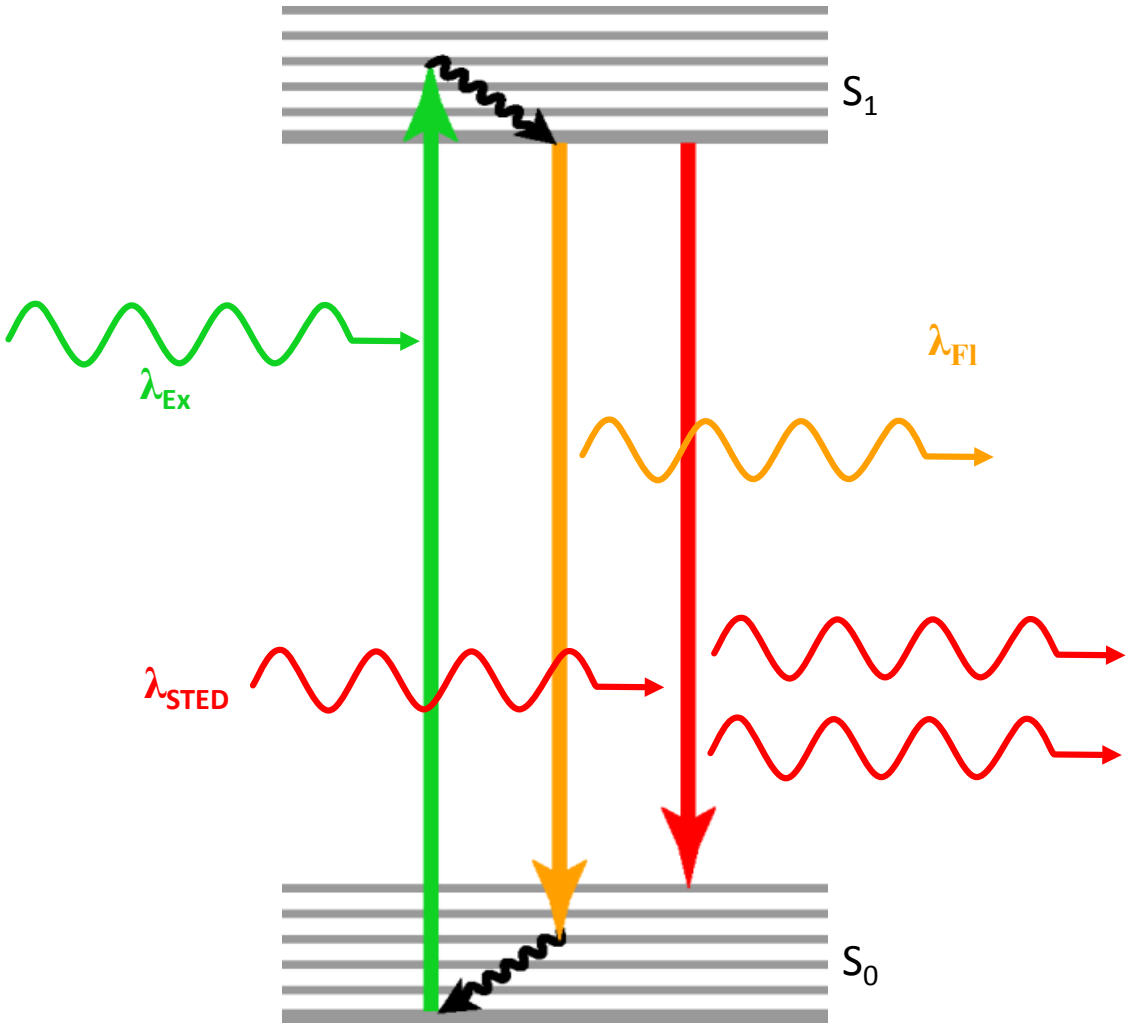
Light sheet fluorescence expansion microscopy

→ PhD defense Dr. Juan Eduardo Rodríguez-Gatica

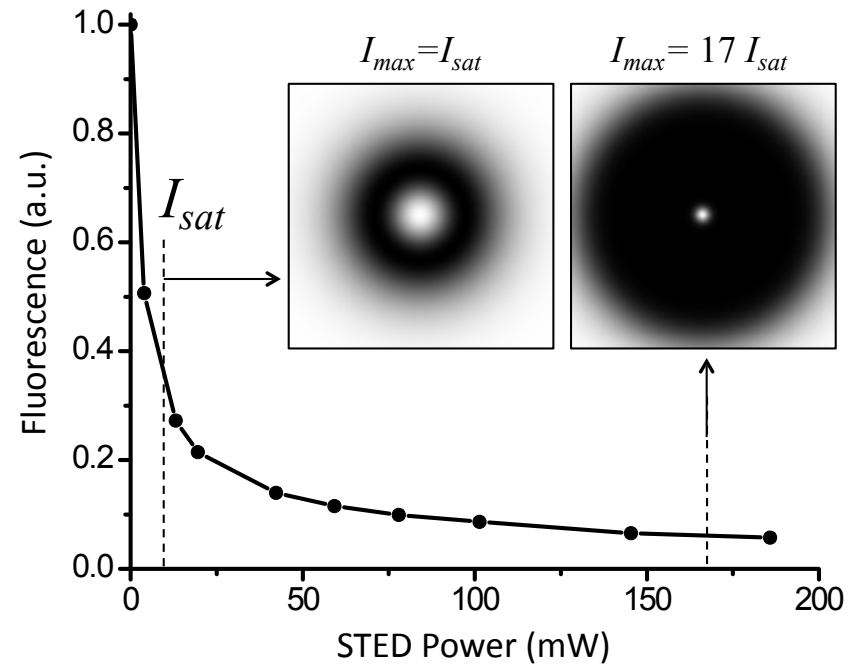
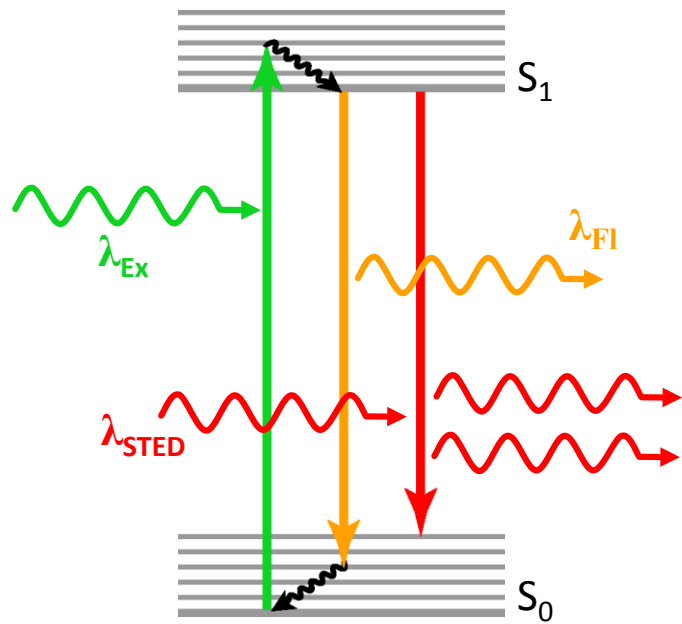
February 22nd, 2024

## 15b. Stimulated emission depletion microscopy STED

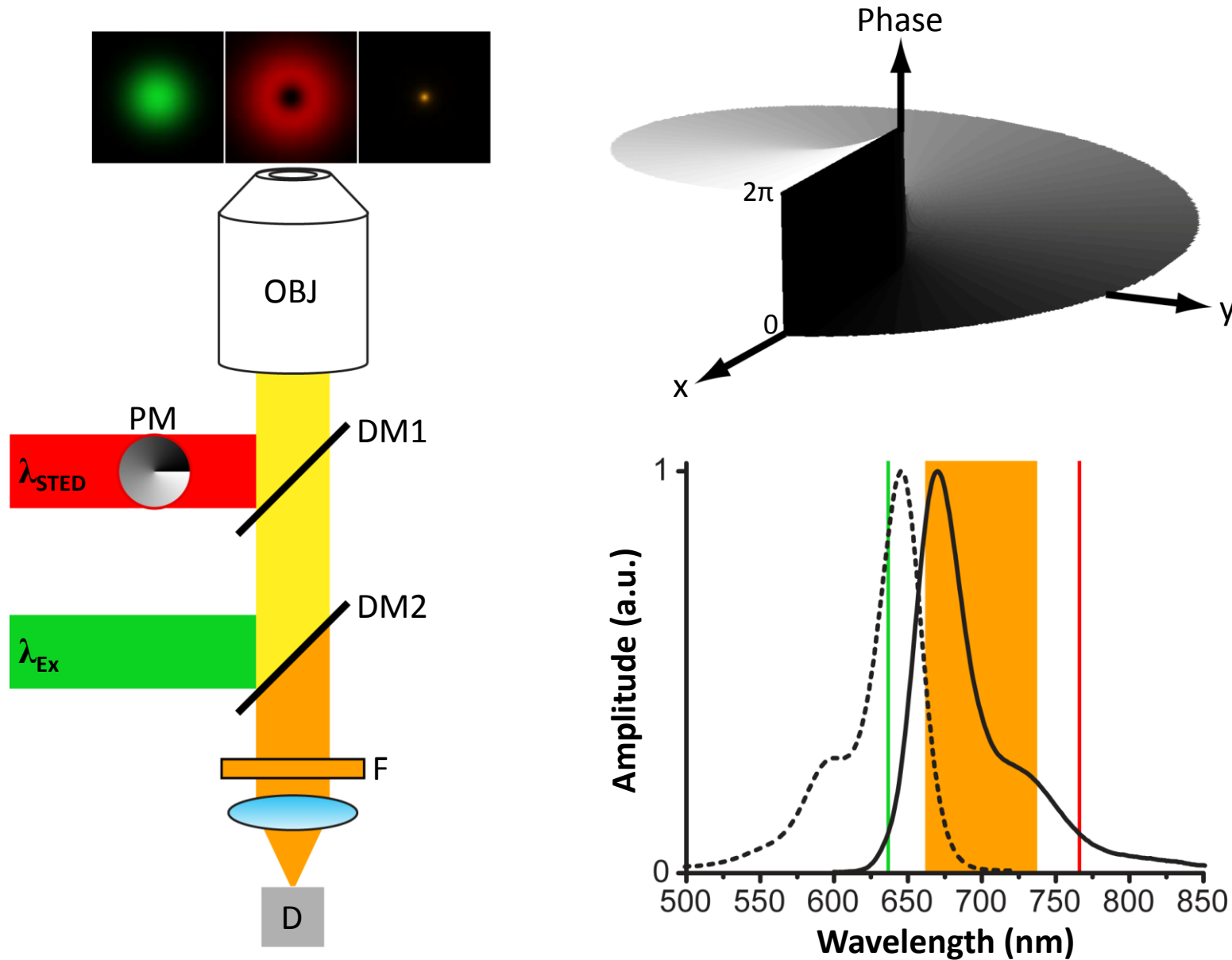
# Stimulated emission



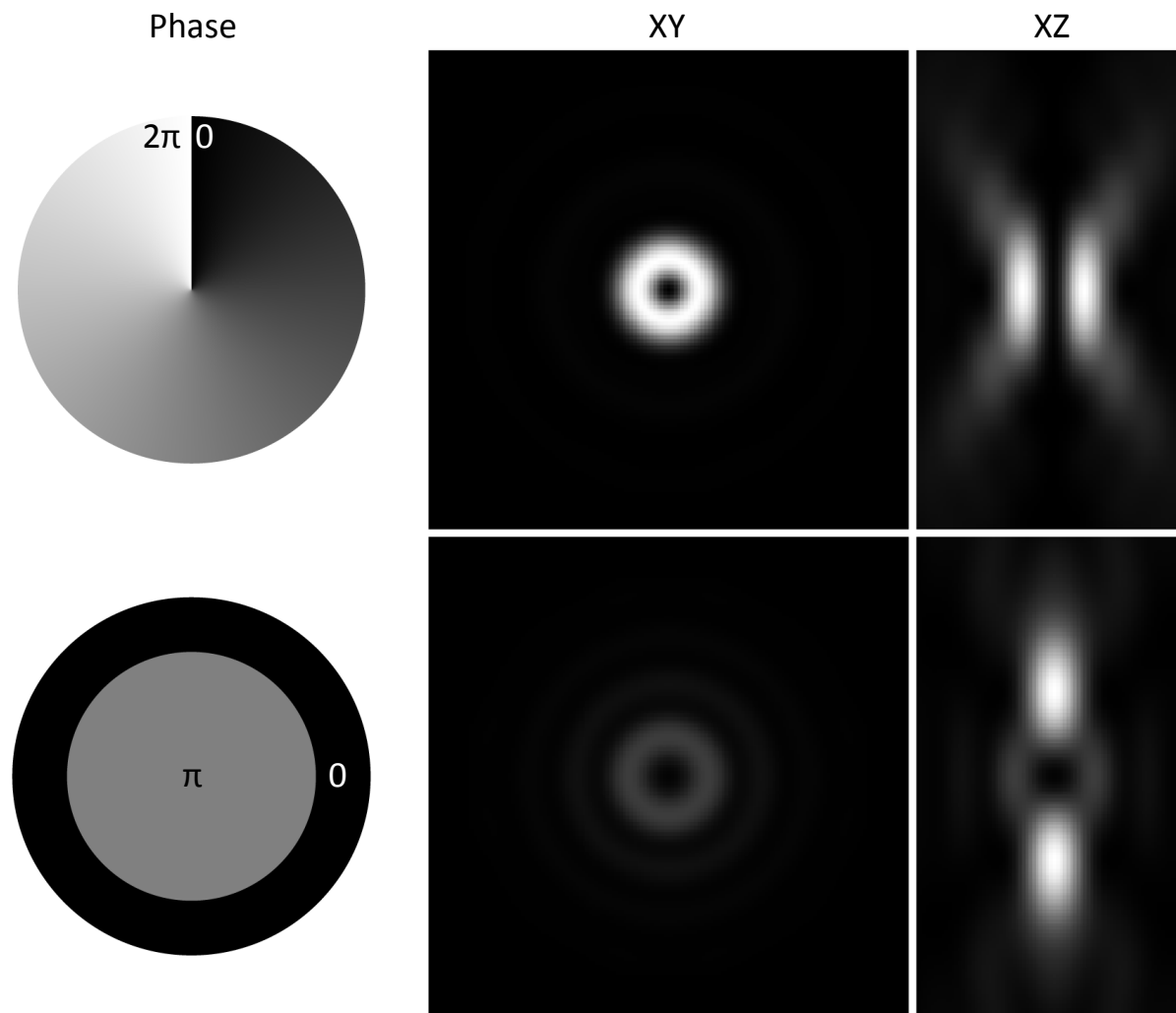
# Stimulated emission



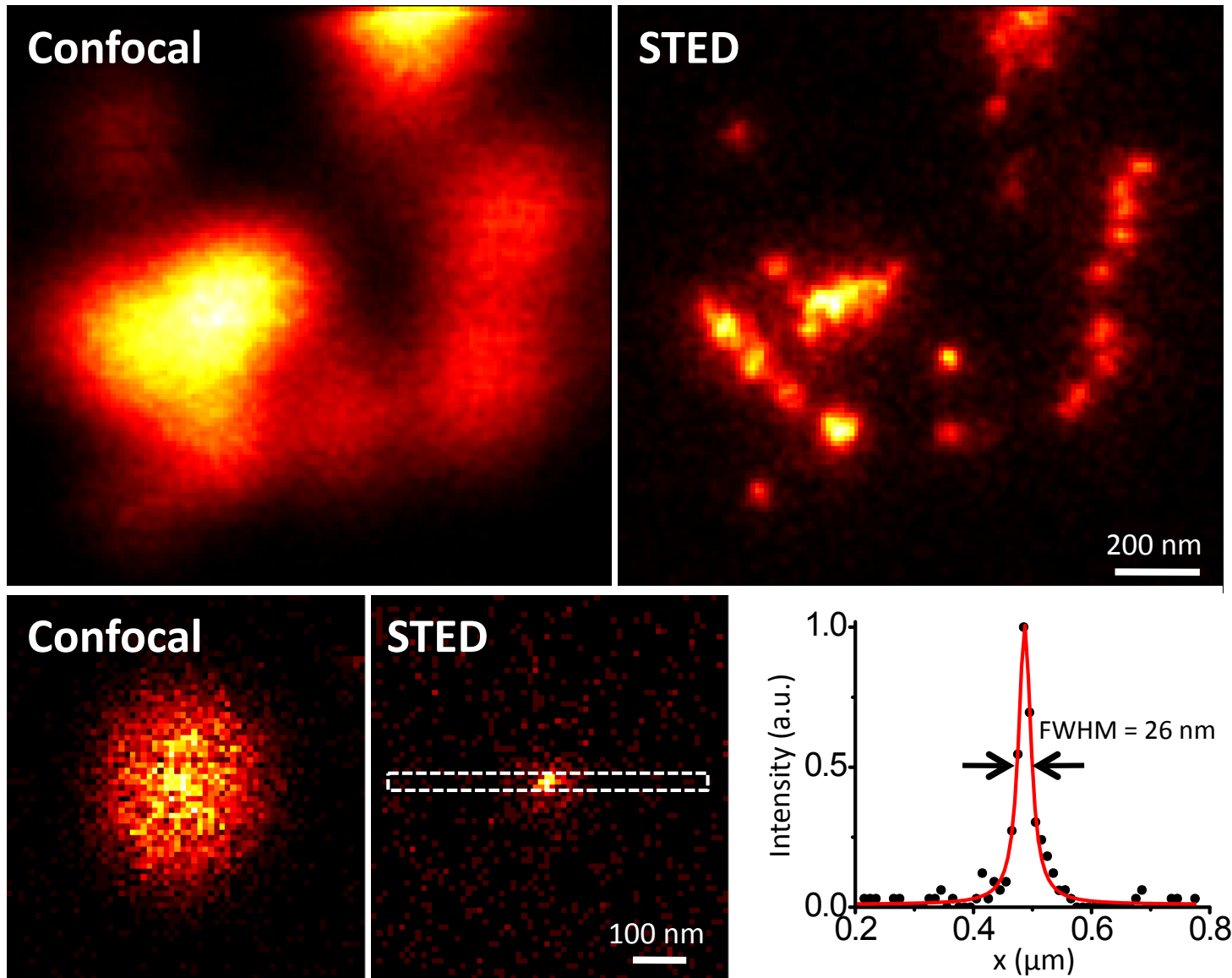
# Realisation of STED microscopy



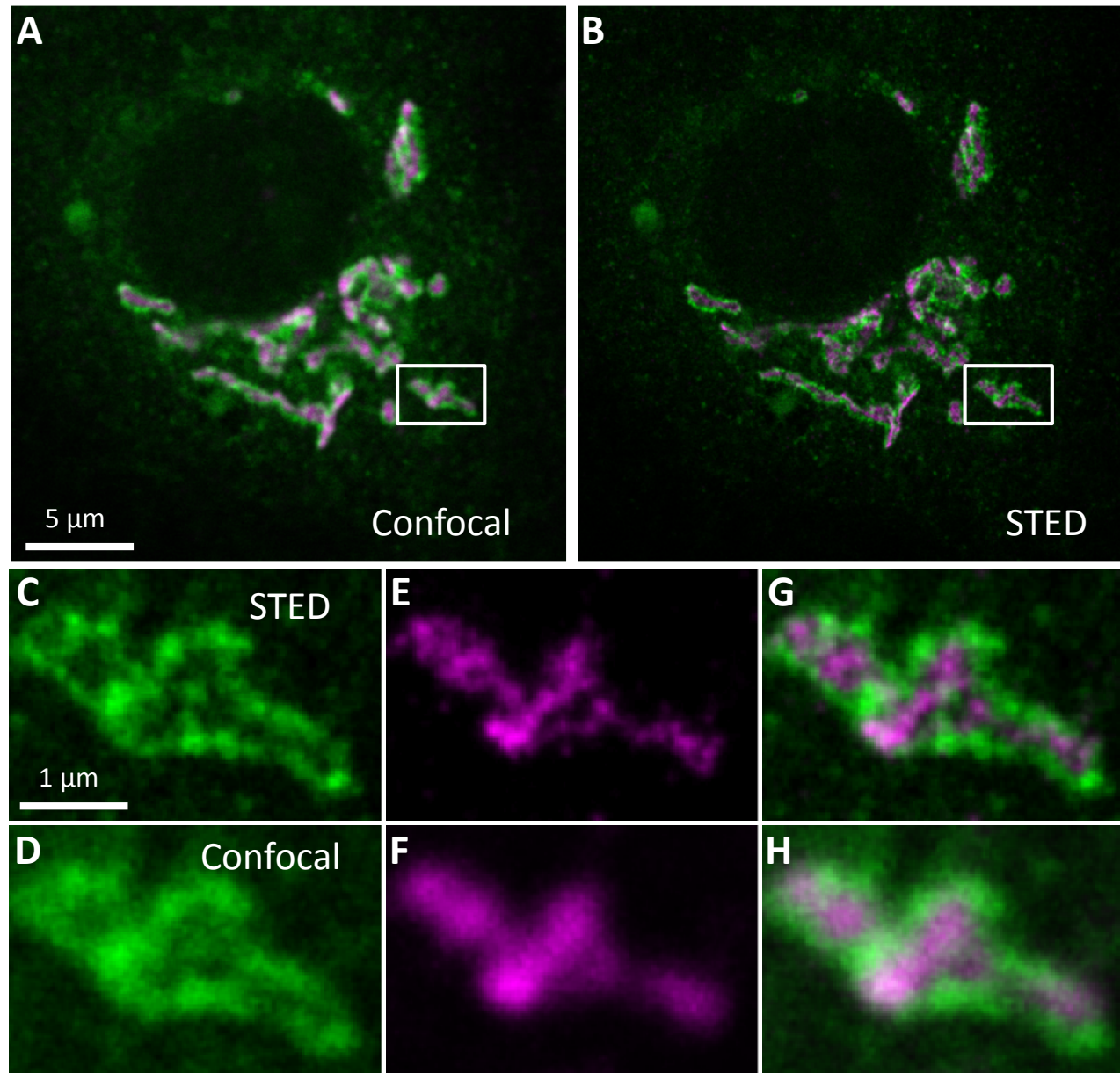
# Phase masks used in the back focal plane in STED microscopy



# Imaging 20 nm fluorescent beads



# STED imaging



Dual-color STED image of the endoplasmic reticulum (ER) and mitochondria. (a) Overlay of images of ER labeled with Atto594 (green) and mitochondria labeled with ATTO647N (magenta). (b) Corresponding STED image. (c–h) Zoom-in of boxed areas in (a) and (b). Images were obtained using a custom-built STED instrument and smoothed by Gaussian filters.



## 16. Molecular Mobility

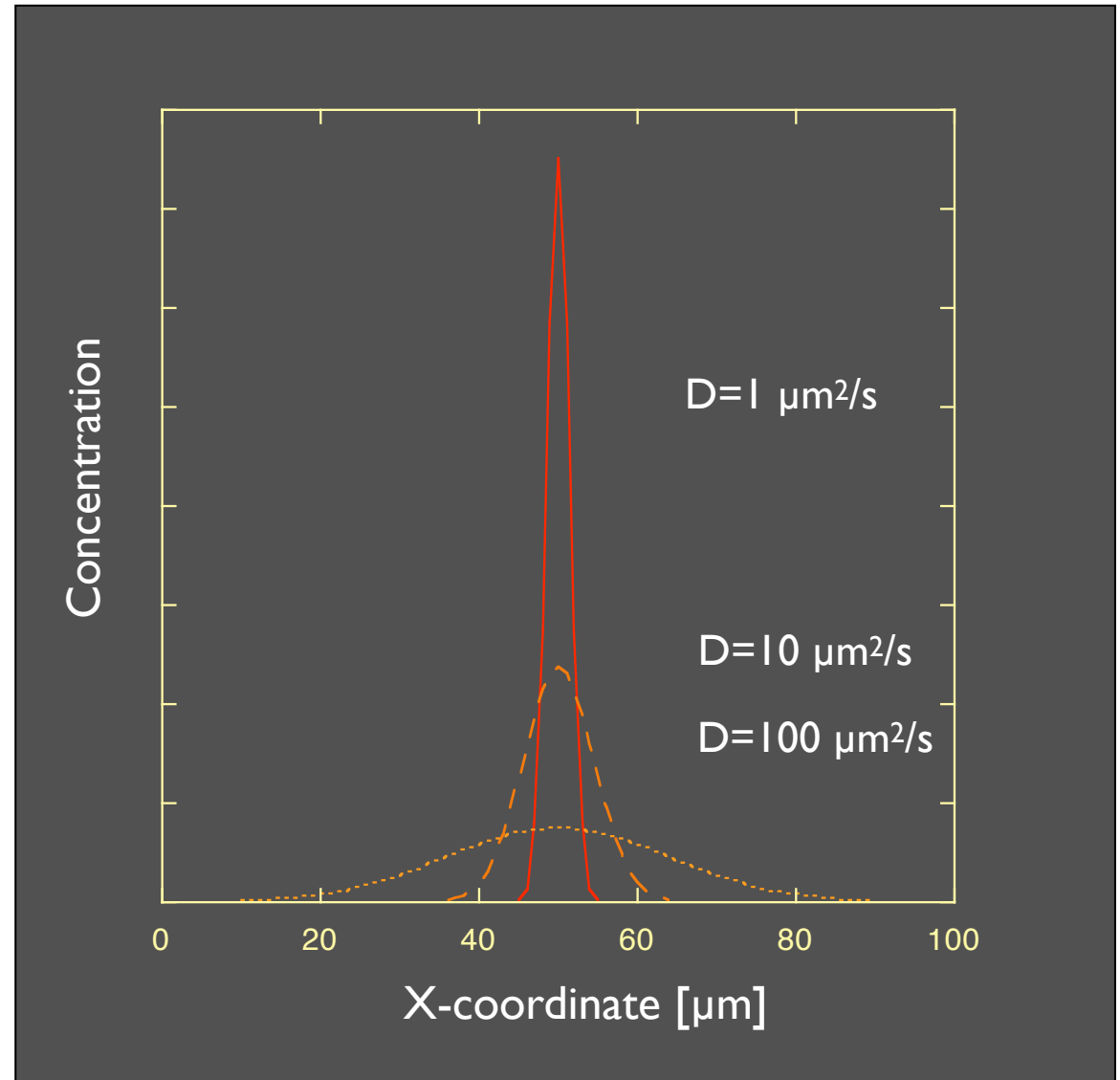
Fluorescence recovery after photobleaching  
FRAP

# Particle transport by diffusion

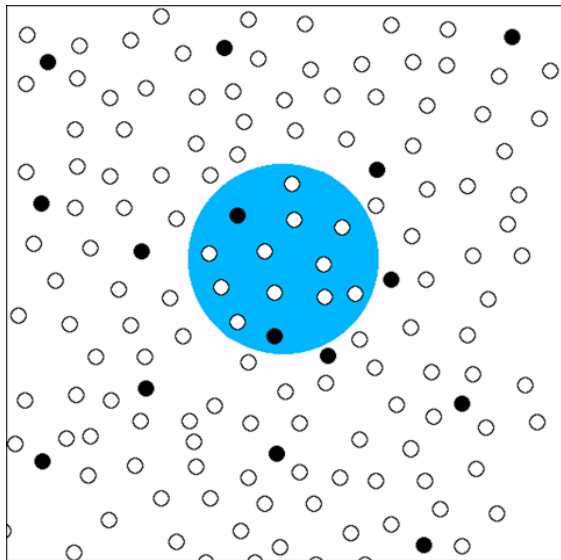
$$c(x, t) = \frac{I}{2\sqrt{\pi Dt}} e^{-\frac{x^2}{4Dt}}$$

Start position:  $x=50$

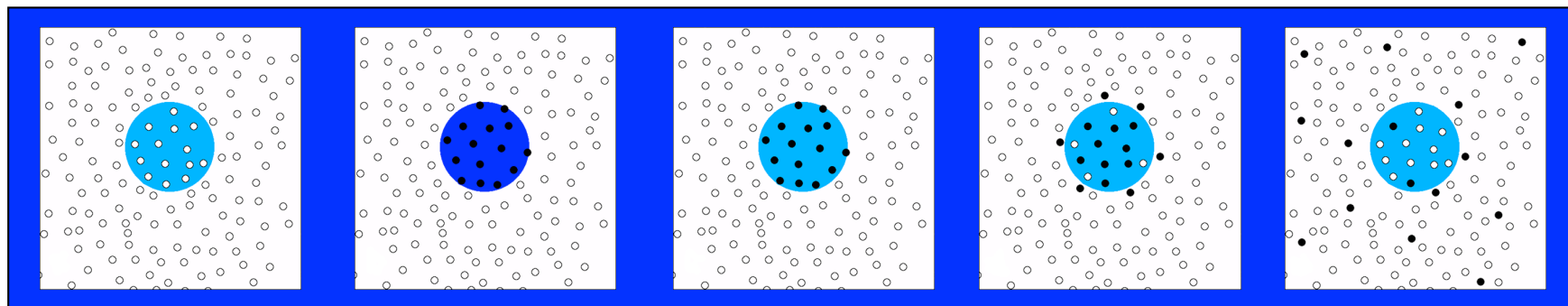
Distribution after 1 second:



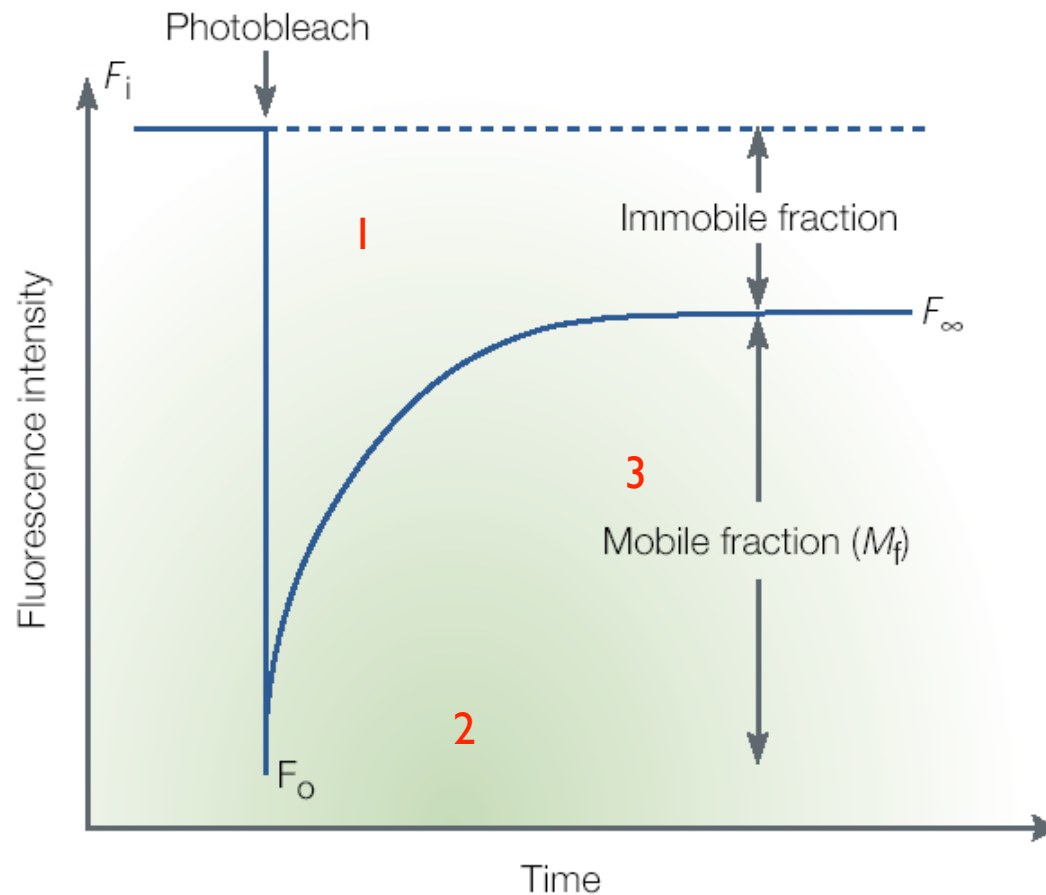
# Transport measurements by photobleaching: „Fluorescence Recovery After Photobleaching“ FRAP or FPR



- (1) Low intensity: prebleach measurement
- (2) High intensity: bleaching (microphotolysis)
- (3) Low intensity: monitoring measurement



# Time dependence of fluorescence in a FRAP experiment



(1) Low intensity: prebleach measurement

(2) High intensity: bleaching (microphotolysis)

(3) Low intensity: monitoring measurement

Preconditions:

Instantaneous bleaching

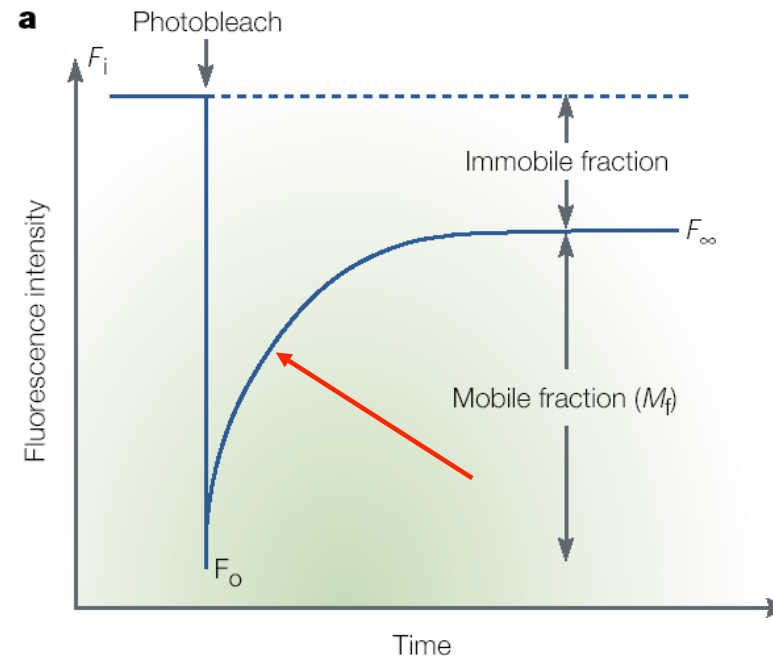
No bleaching during monitoring

# Diffusion time, $\tau_D$

Diffusion time:

$$\tau_D = \frac{w^2}{4D}$$

w, radius of the focussed laser beam  
D, diffusion constant

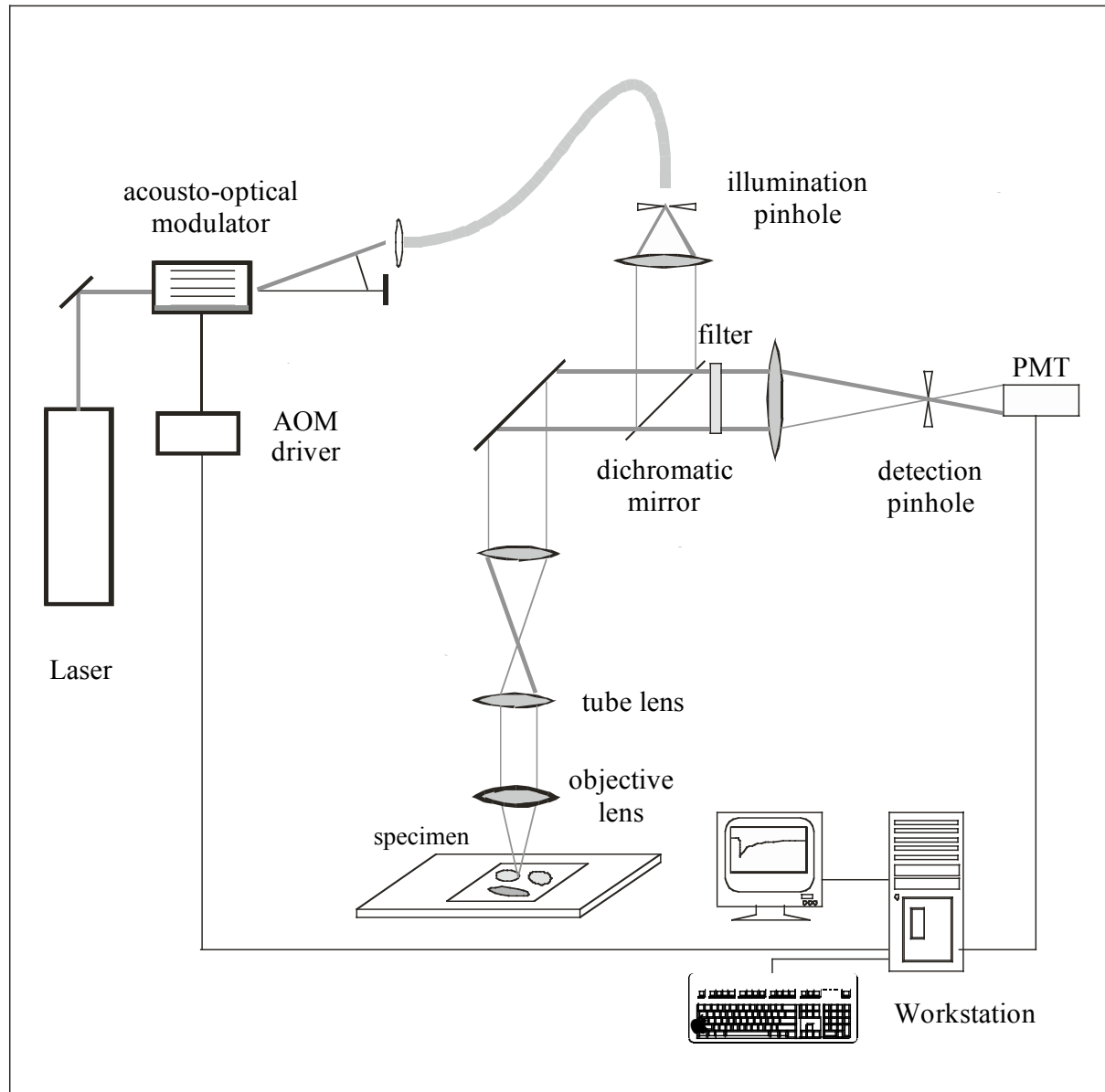


$\tau_D$  is obtained plotting the recovery of the relative fluorescence intensity within a bleached area as a function of time, and by fitting this curve by a specific mathematical model

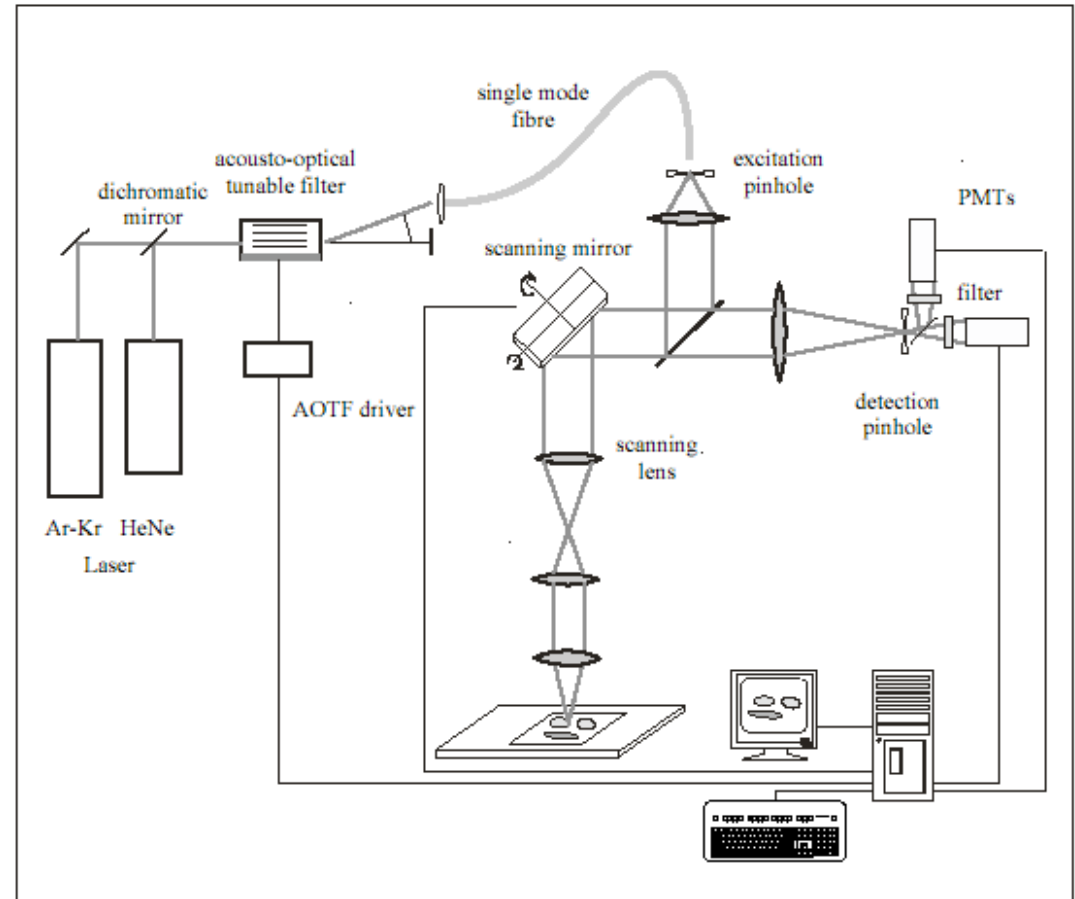
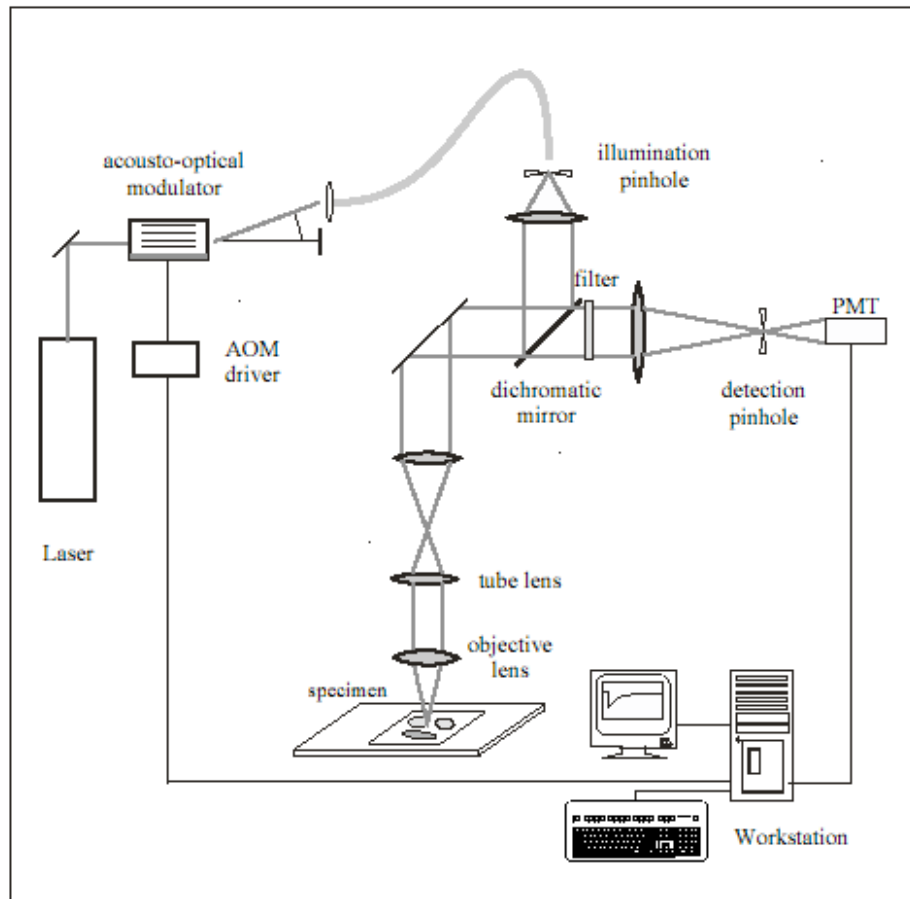
(w is measured)

→ determination of D

# Photobleaching Instrument



# Photobleaching instrument & CLSM



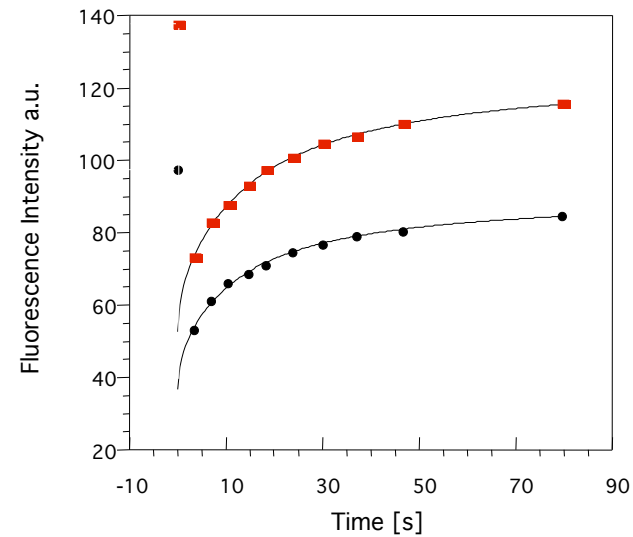
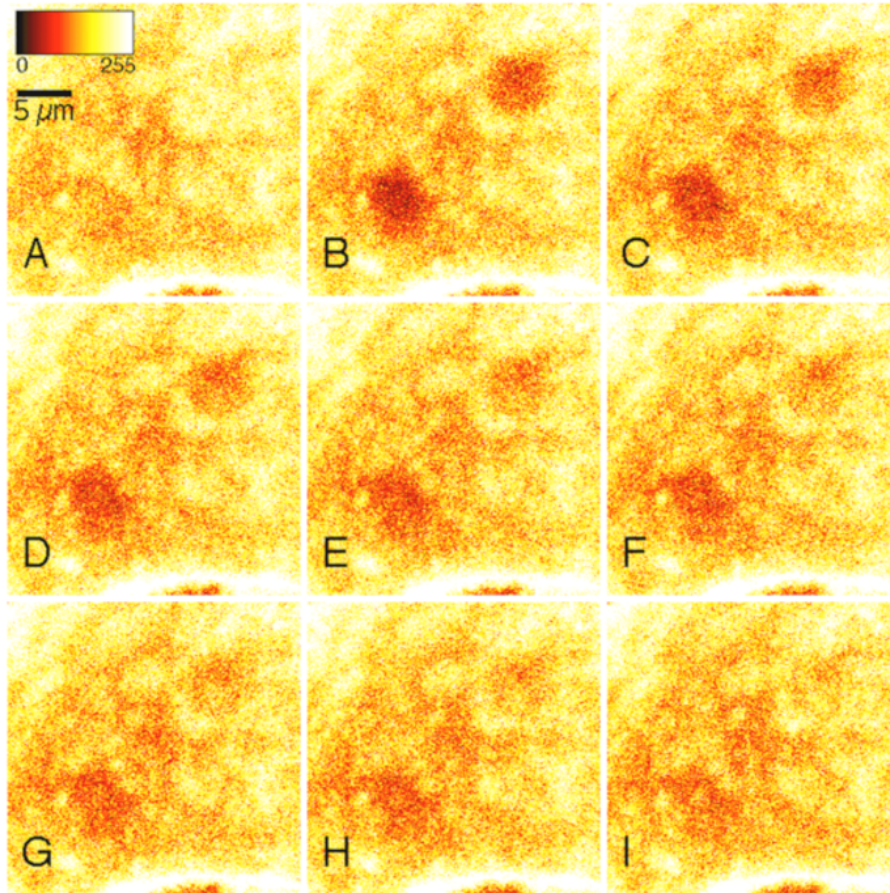
# Lateral membrane transport by CLSM-FRAP

Sample:

Membranes of 3T3 cells labeled by fluorescent lipid analogs

$D = 0.2 \mu\text{m}^2/\text{s}$

Fraction of immobile molecules  $\approx 5\%$





## 16. Optical tweezers

# Photon momentum

---

$$p = m \cdot v$$

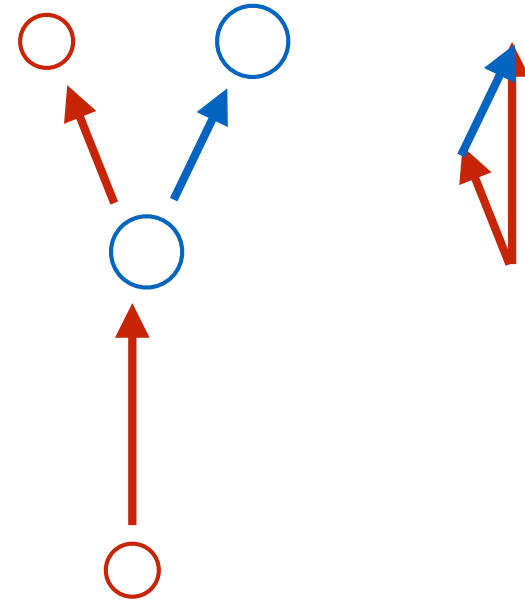
$$E = m \cdot c^2 \Rightarrow m = E/c^2$$

$$E = h\nu \quad \nu\lambda = c$$

$$p = E/c = h\nu/c = h/\lambda$$

$$dp/dt = F$$

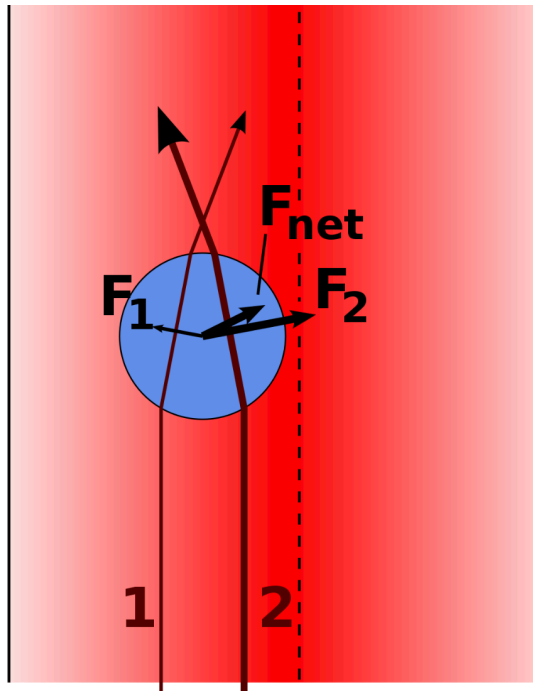
Change of light momentum causes a force  
Principle of conservation of momentum applies



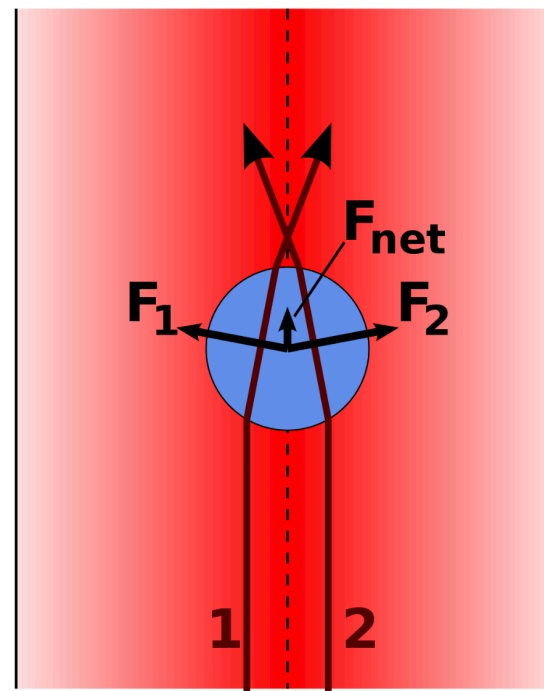
# Force on a particle in an unfocused light beam

---

If diameter  $d$  of a trapped particle is significantly greater than  $\lambda$ , the trapping phenomenon can be explained using ray optics



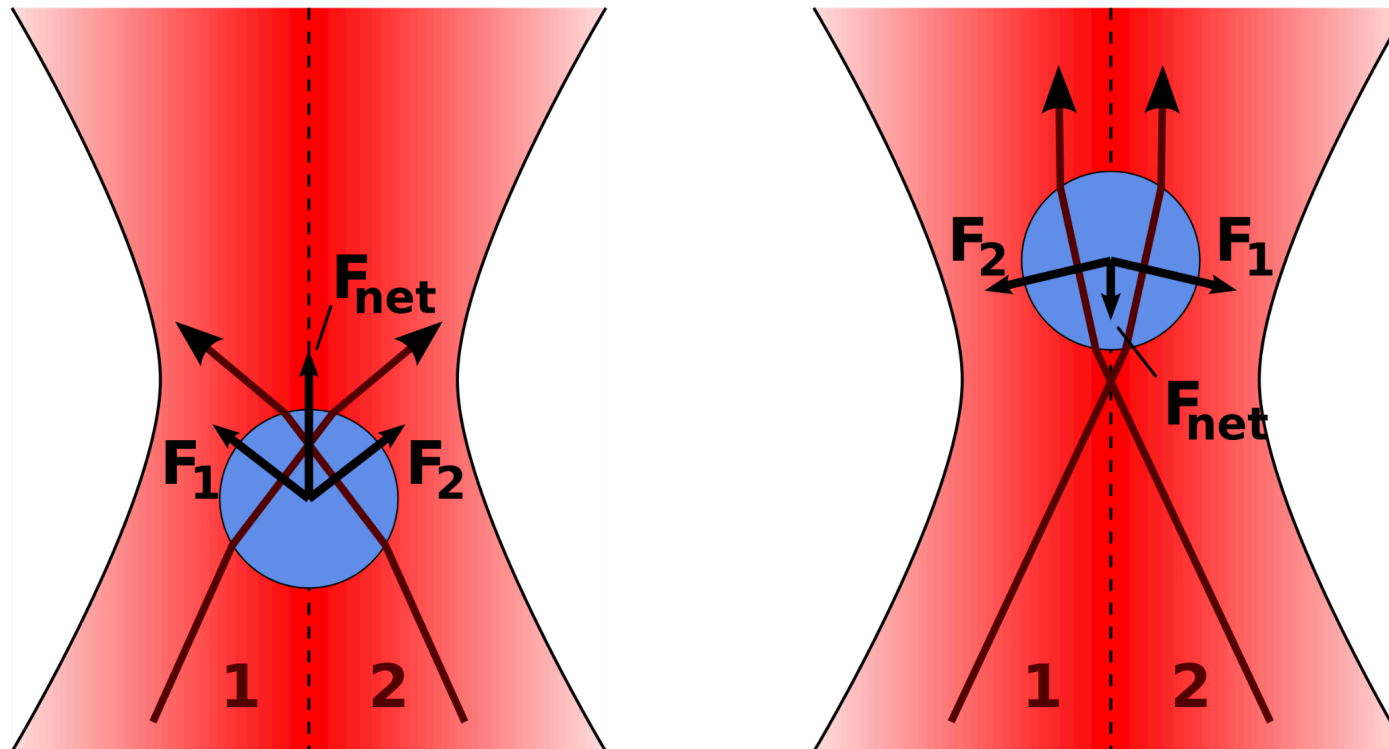
When the bead is displaced from the beam center, the larger momentum change of the more intense rays cause a net force to be applied back toward the center of the laser.



When the bead is laterally centered on the beam (left), the resulting lateral force is zero. But an unfocused laser still causes a force pointing away from the laser

# Force on a particle in a focused light beam

---



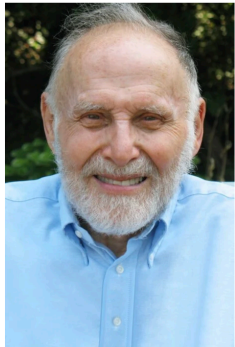
In addition to keeping the bead in the center of the laser, a **focused** laser also keeps the bead in a fixed axial position: The momentum change of the focused rays causes a force towards the laser focus, both when the bead is in front (left) or behind (right) the laser focus.

So, the bead will stay slightly behind the focus, where this force compensates the scattering force.

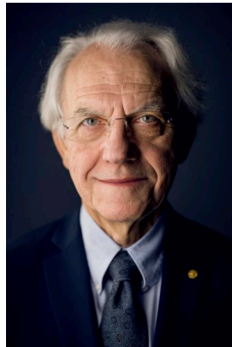
# Example: multiple optical foci

---

## The Nobel Prize in Physics 2018



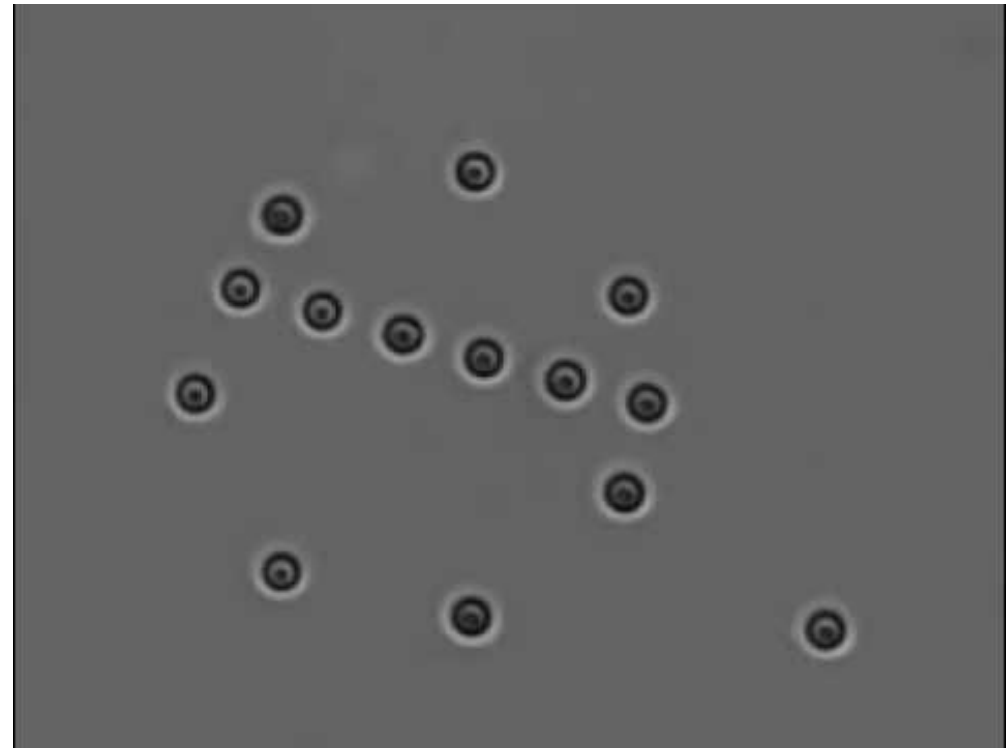
© Arthur Ashkin  
**Arthur Ashkin**  
Prize share: 1/2



© Nobel Media AB. Photo: A. Mahmoud  
**Gérard Mourou**  
Prize share: 1/4



© Nobel Media AB. Photo: A. Mahmoud  
**Donna Strickland**  
Prize share: 1/4



Nobel prize 2018 to Arthur Ashkin for “for the optical tweezers and their application to biological systems”

<https://www.nobelprize.org/prizes/physics/2018/summary/>

## Example: multiple optical foci

---

Force on the particle due to the field gradient:

$$\mathbf{F} = \frac{1}{2}\alpha\nabla E^2 = \frac{2\pi n_0 a^3}{c} \left( \frac{m^2 - 1}{m^2 + 2} \right) \nabla I(\mathbf{r})$$

+ scattering force pushing the particle forward

where

$a$  is the particle radius,

$n_0$  is the index of refraction of the particle and

$m = n_p/n_1$

is the relative refractive index between the particle and the medium

Nobel prize 2018 to Arthur Ashkin for “for the optical tweezers and their application to biological systems”

<https://www.nobelprize.org/prizes/physics/2018/summary/>

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Thank you very much for your attention!