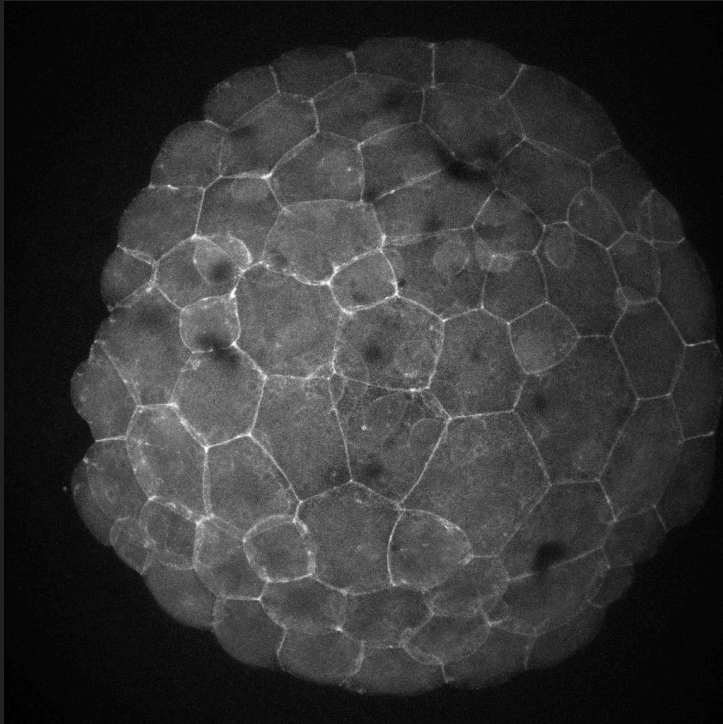


# PRINCIPLES OF MECHANICS IN BIOLOGY



RODRIGO SOTO

PHYSICS DEPARTMENT

UNIVERSIDAD DE CHILE

Optics, Forces & Development 2024

**ACTIVE MATTER**

Núcleo Milenio Física de la Materia Activa



**MOLECULAR MOTORS**

$$F = m a$$

**VECTORS**

**FORCES**

**TENSORS**

**NEWTON**

**TENSION**

**STRESSES**

**ACTION-REACTION**

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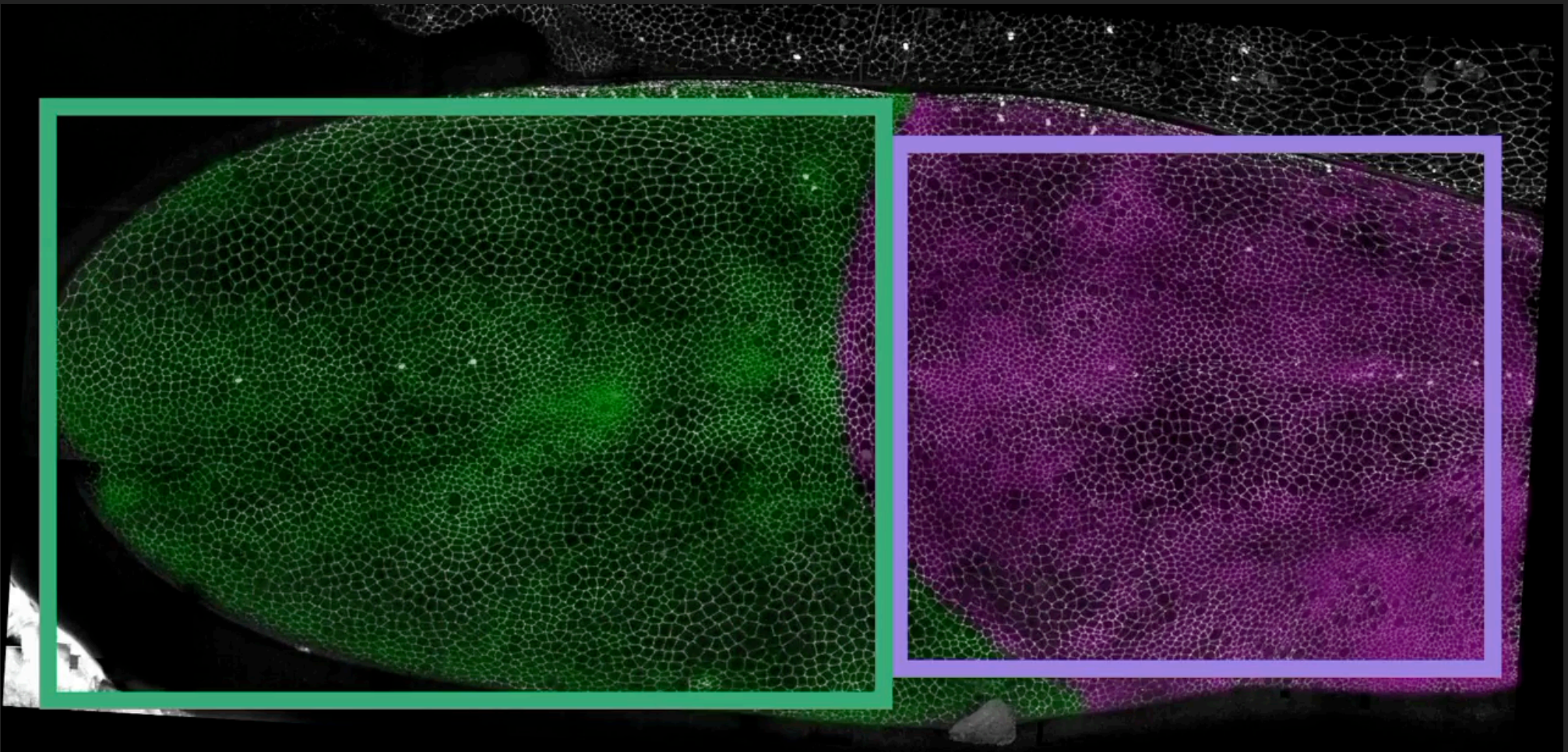
**MECHANICS?**



**fcfm**

Física  
FACULTAD DE CIENCIAS  
FÍSICAS Y MATEMÁTICAS  
UNIVERSIDAD DE CHILE

# FORCES ACTING ON DEVELOPMENT



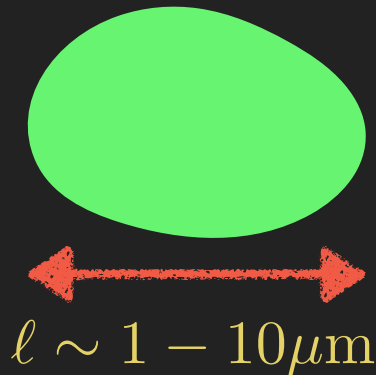
**IN THE GREEN DOMAIN, IN WHICH DIRECTION DO THE FORCES ACT?**

**AT THE FINAL EQUILIBRIUM STATE, ARE THERE FORCES ACTING?**

**IS THE TISSUE UNDER STRESS?**

Drosophila pupal wing  
R. Etournay et al, eLife 2015

# FORCES IN THE MICROSCOPIC WORLD



$$F = ma$$

$$m \sim \rho \times \text{vol}$$

$$m \sim l^3$$

## SCALING OF DIFFERENT FORCES

Adhesion:  $F \sim \text{area} \sim l^2$

Weight:  $F \sim \text{mass} \sim l^3$

Friction by weight:  $F \sim \text{mass} \sim l^3$

Friction by compression:  $F \sim \text{area} \sim l^2$

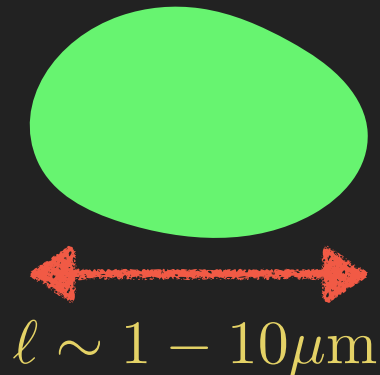
Viscous friction:  $F \sim \text{area} \sim l^{1-2}$

Elastic:  $F \sim \text{area} \sim l^{0-2}$

**AT THE MICROSCOPIC SCALE, MASS AND WEIGHT ARE NEGLIGIBLE.**

**NO INERTIA**

# FORCES IN THE MICROSCOPIC WORLD



AT THE MICROSCOPIC SCALE, MASS AND WEIGHT ARE NEGLIGIBLE.

NO INERTIA

Newton's law reduces to

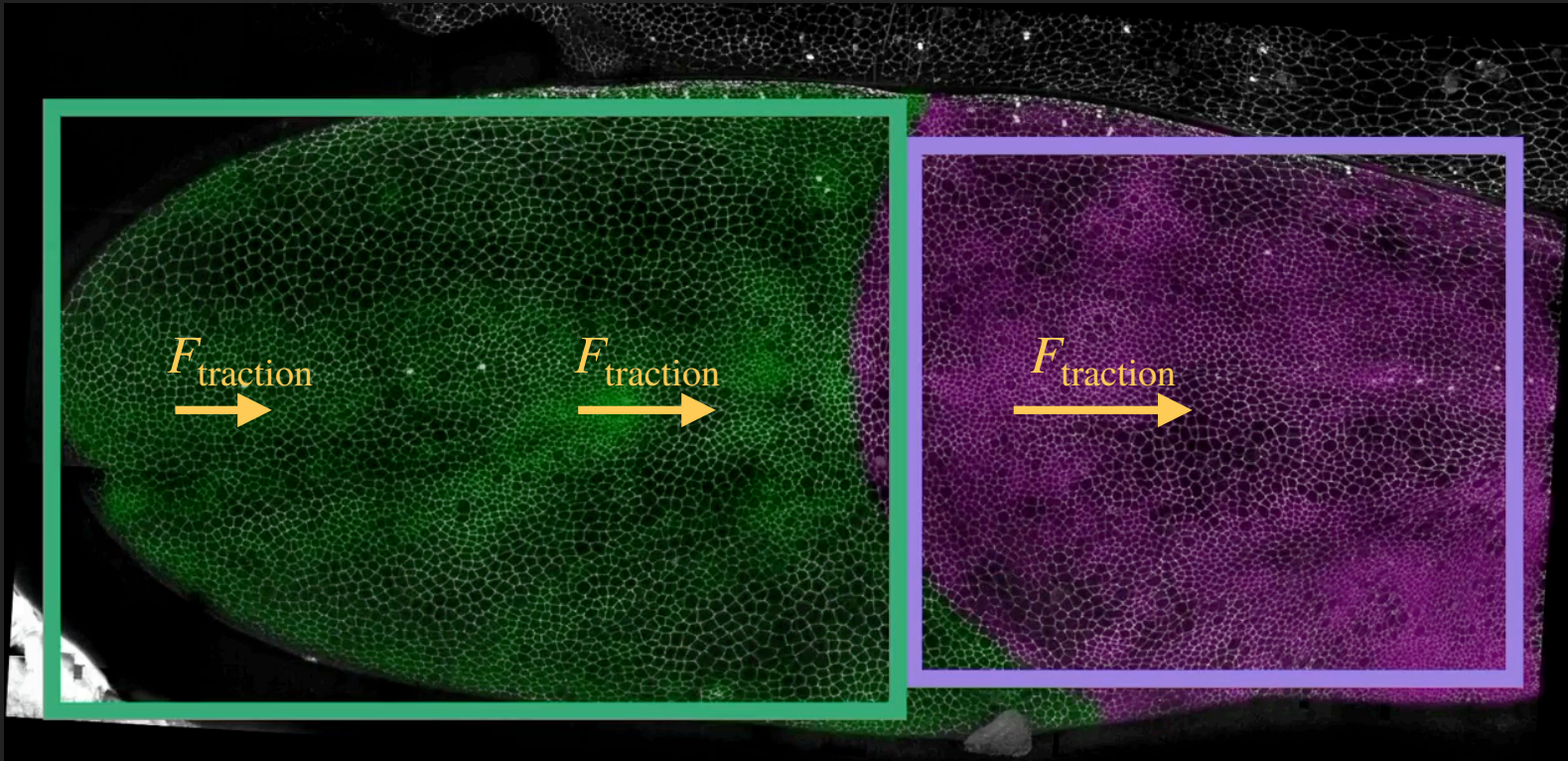
$$F_1 + F_2 + F_3 + \dots + F_n = 0$$

At every instant, not only on average

How is it possible that  $F=0$  gives rise to motion?

# FORCES ACTING ON DEVELOPMENT

Drosophila pupal wing  
R. Etournay et al, eLife 2015

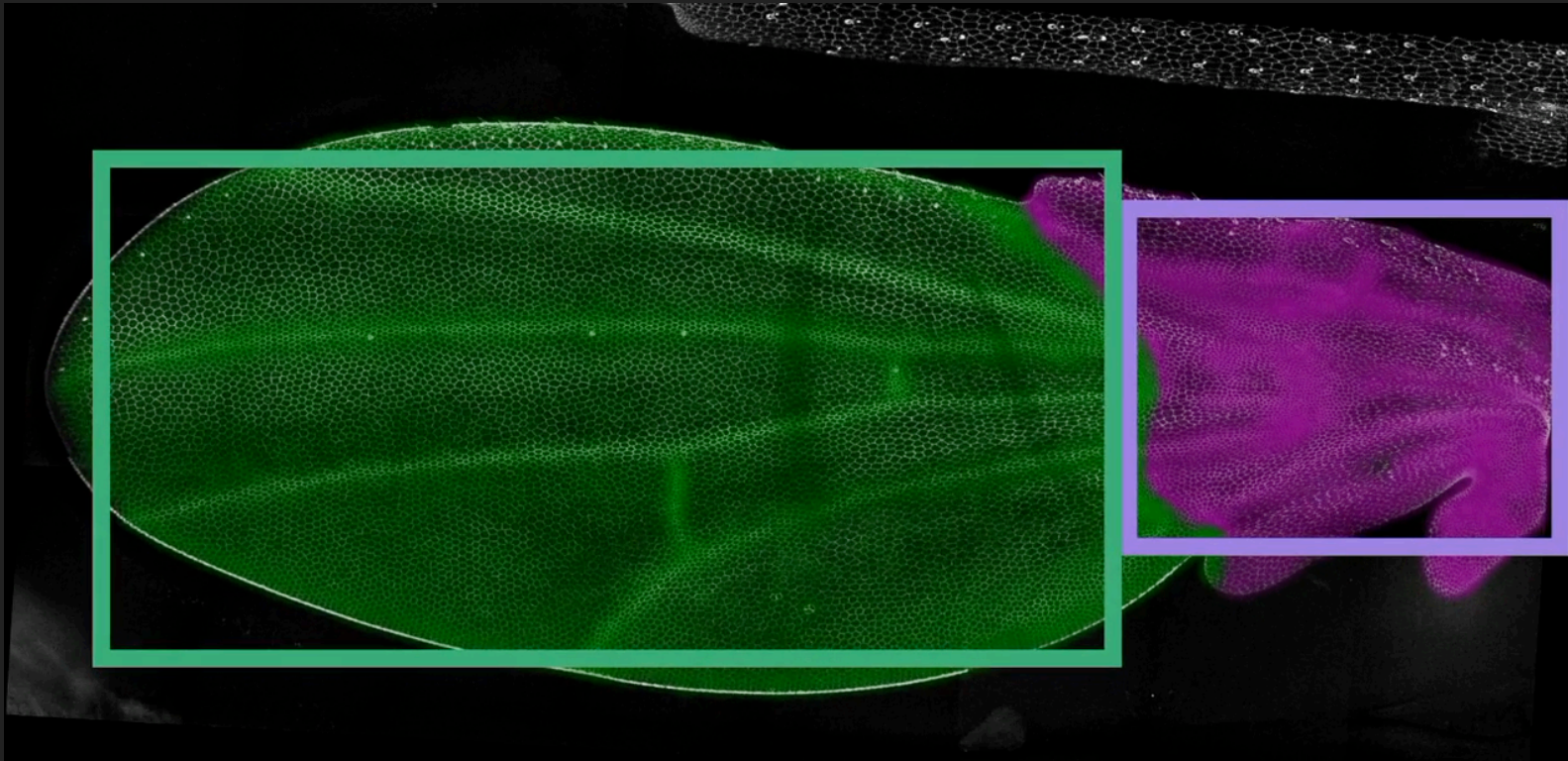


On each cell,  $F_{\text{total}} = F_{\text{friction}} + F_{\text{traction}} = 0$

$F_{\text{friction}} = -\gamma V$       Then,  $F_{\text{traction}} = \gamma V$

**THE TRACTION FORCES PRESENT A GRADIENT**

# FORCES ACTING ON DEVELOPMENT



Drosophila pupal wing  
R. Etournay et al, eLife 2015

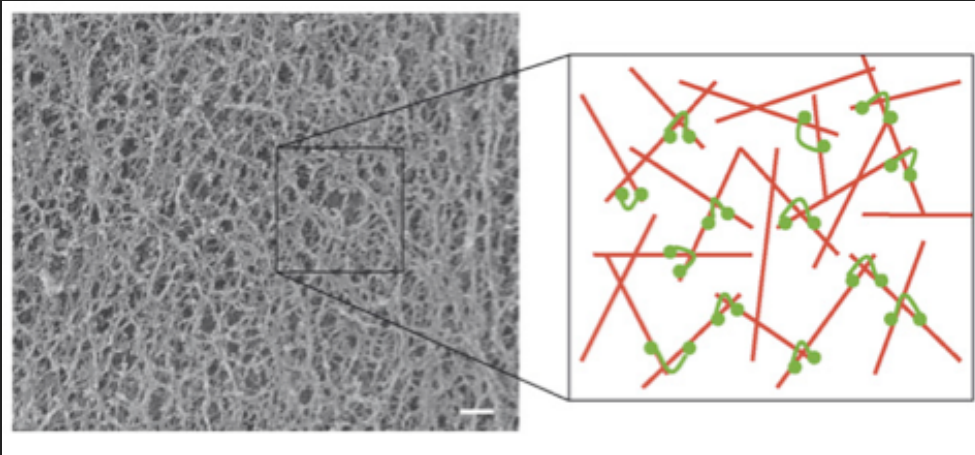
At the final state, there is no motion ( $V=0$ ).

Then  $F_{\text{traction}} = 0$

How is that compatible with the idea of the **tissue being under stress**?

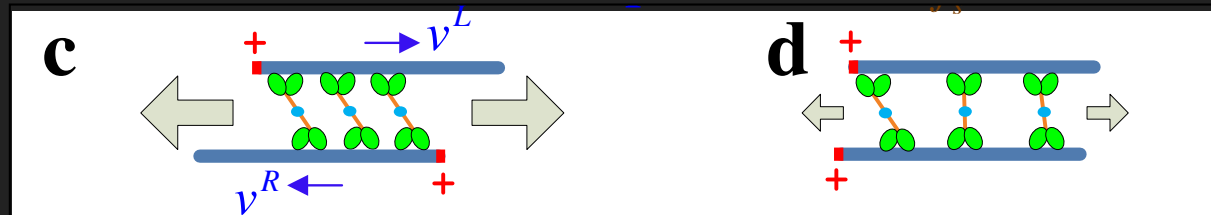
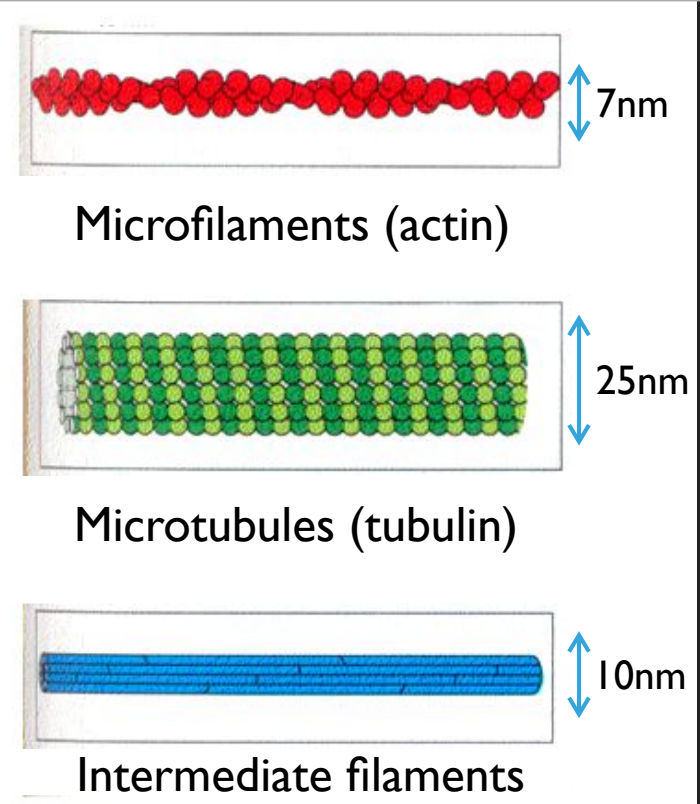
# CELULAR STRESSES

( DETAILS IN ANDREA RAVASIO'S AND CRISTINA BERTOCCHI'S LECTURES )



Kasza et al. Curr Opin Cell Biol (2007)

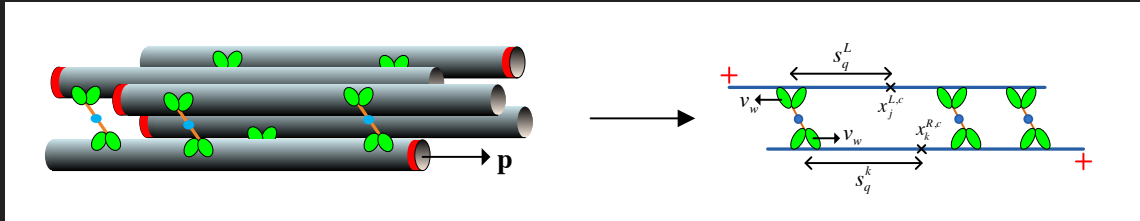
The filaments are polar and the molecular motors can "walk" in a specified direction



Gao et al. (2015)



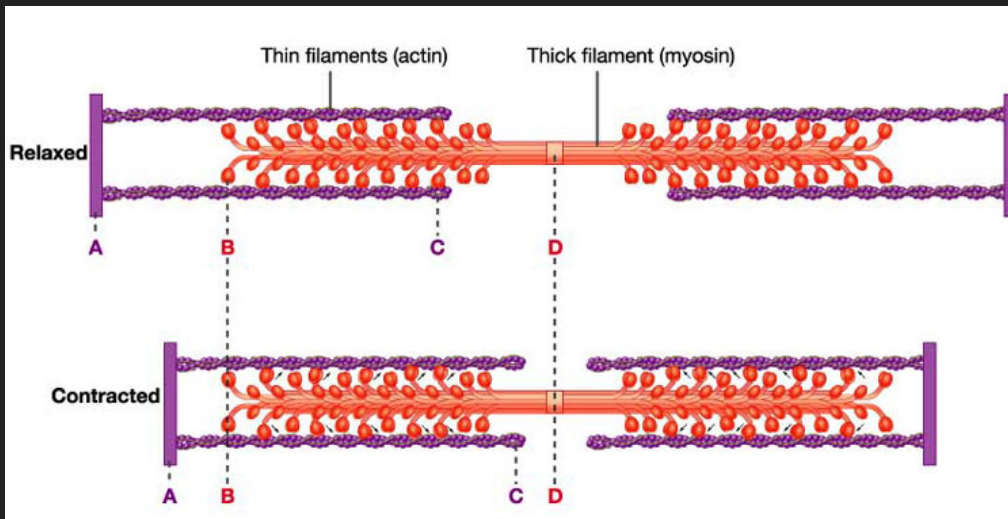
# CELULAR STRESSES



Gao et al. (2015)

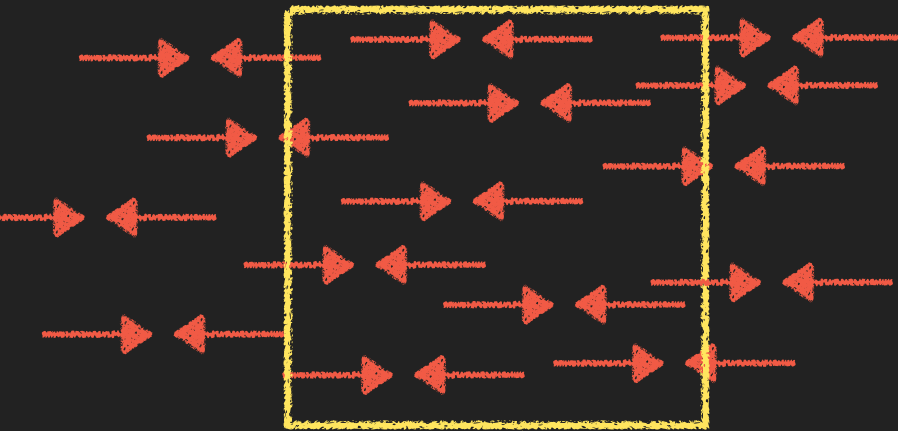


**PAIR OF OPPOSITE FORCES.  
SEPARATED BY FEW NANOMETERS.  
A FORCE DIPOLE**

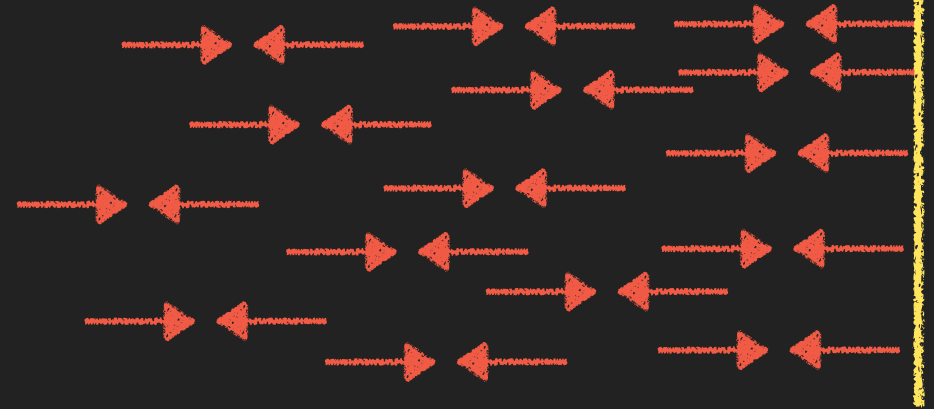


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# CELULAR STRESSES

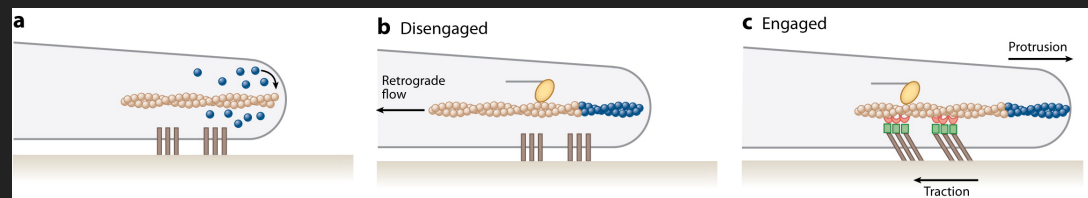


THE STRESSES ARE FINITE,  
BUT THE SUMMED FORCE VANISHES



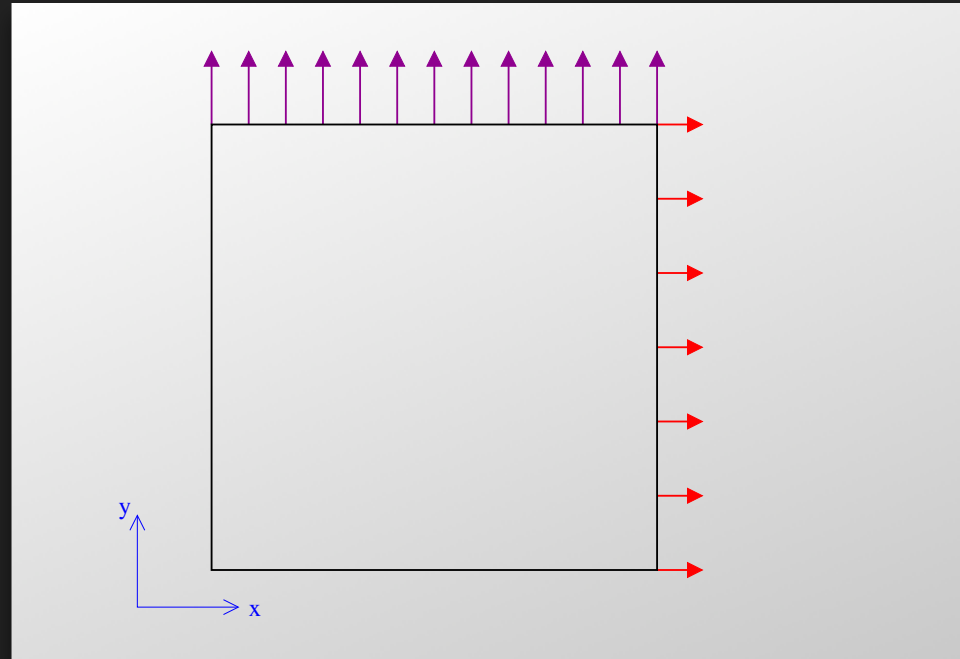
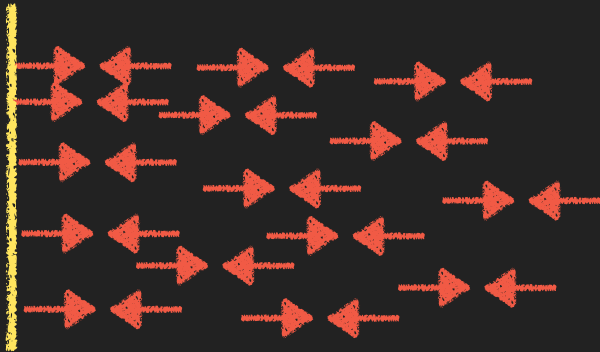
BUT ON THE SURFACE THERE IS A NET FORCE  
A TENSILE OR TRACTION STRESS.

THE NET FORCE IS PROPORTIONAL TO THE AREA



Gardel et al., Annu Rev Cell Dev Biol

# STRESS TENSOR (TENSOR DE ESFUERZOS O DE TENSIONES)



$$F_x \propto L_y$$

$$F_y \propto L_x$$

$$\sigma_x = F_x / L_y$$

$$\sigma_y = F_y / L_x$$

$$\sigma = \begin{pmatrix} \sigma_x & 0 \\ 0 & \sigma_y \end{pmatrix}$$

## Stress tensor:

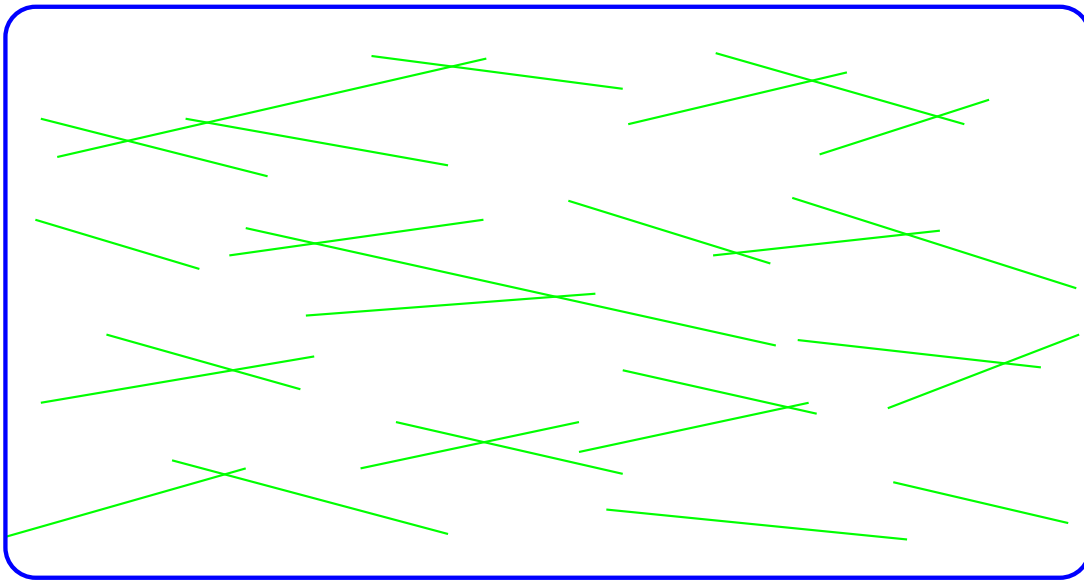
It gives the stress on each direction (principal directions), two or three

Stresses (or tensions) are forces per unit of length or surface

The direction of the force depends on the stresses and the surface

# ACTIVE STRESS (CYTOSKELETON)

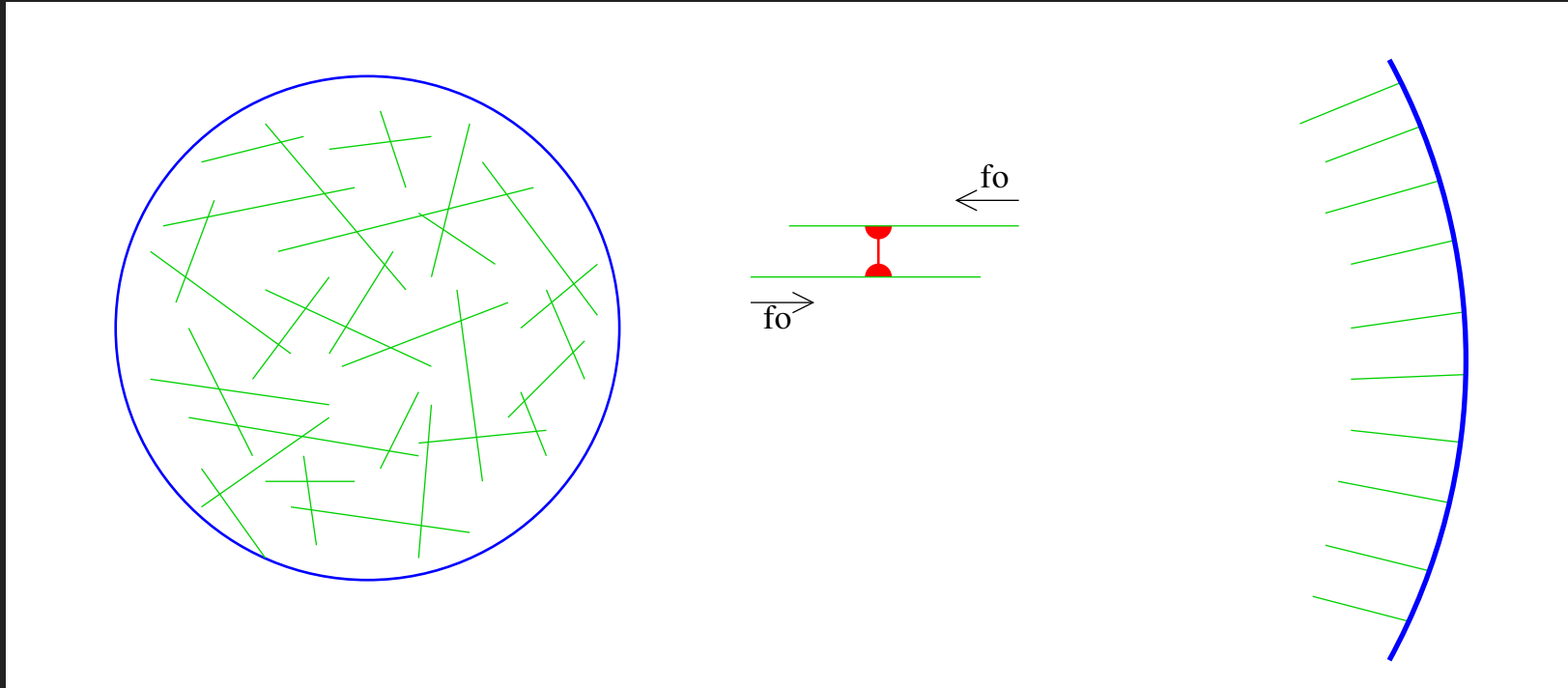
Polarized cytoskeleton



$$\sigma_x > \sigma_y$$

$$\sigma^a = \begin{pmatrix} \sigma_x & 0 \\ 0 & \sigma_y \end{pmatrix}$$

# ACTIVE STRESS (CYTOSKELETON)



$$F = N f_o$$

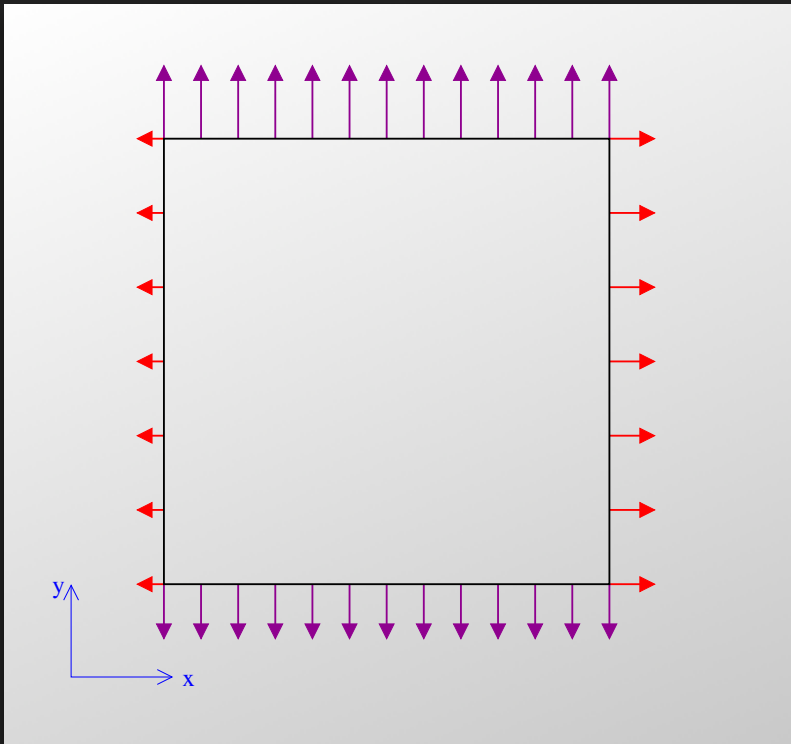
$$= \left( \frac{N f_o}{L_y} \right) L_y$$

$$= \sigma_a L_y$$

$$\sigma_a = n_{\text{filam}} f_o$$

Active stress

# EQUILIBRIUM CONDITION



$$\vec{F}_{\text{total}} = [\sigma_x(x + L_x) - \sigma_x(x)] L_y \hat{x} + [\sigma_y(y + L_y) - \sigma_y(y)] L_x \hat{y}$$

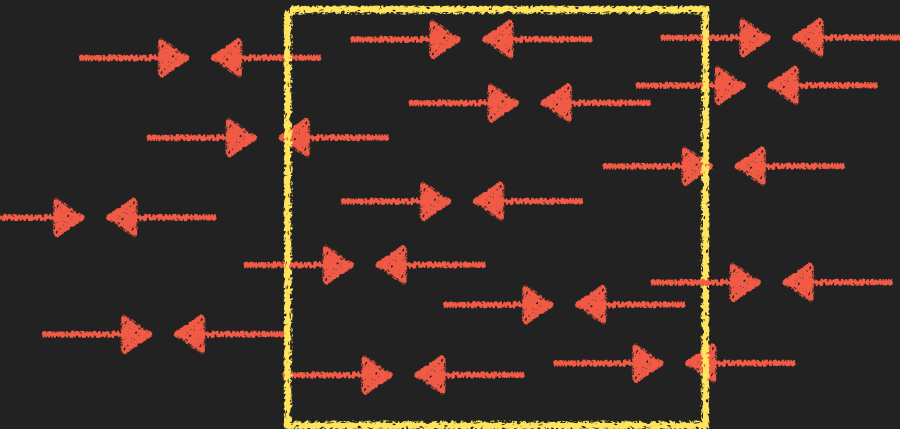
Force equilibrium,  $F=0$ :

$\sigma_x \approx \text{cte.}$       **But, different**  
 $\sigma_y \approx \text{cte.}$       **between directions**

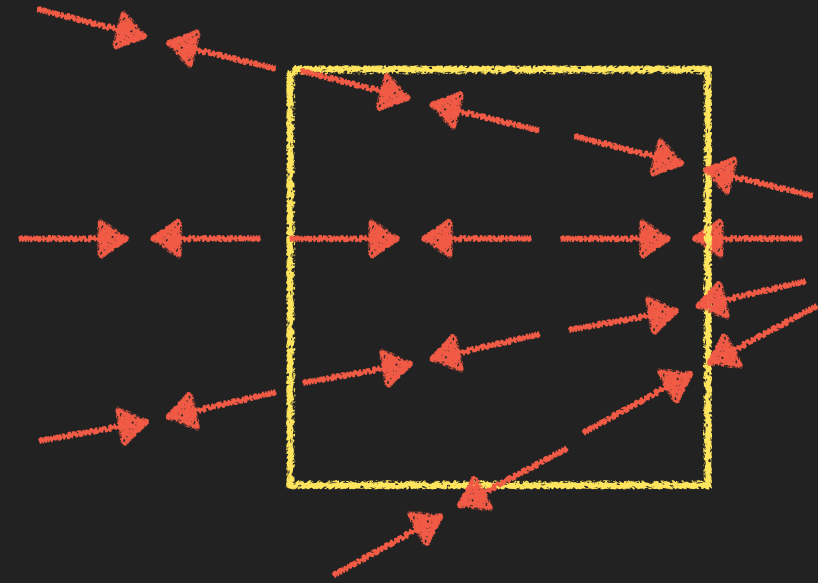
$$\sigma = \begin{pmatrix} \sigma_x & 0 \\ 0 & \sigma_y \end{pmatrix}$$

**IN EQUILIBRIUM, FORCES VANISH, AND STRESSES ARE UNIFORM  
CAN BE ANISOTROPIC  $\sigma_x \neq \sigma_y$**

# STRESS TENSOR



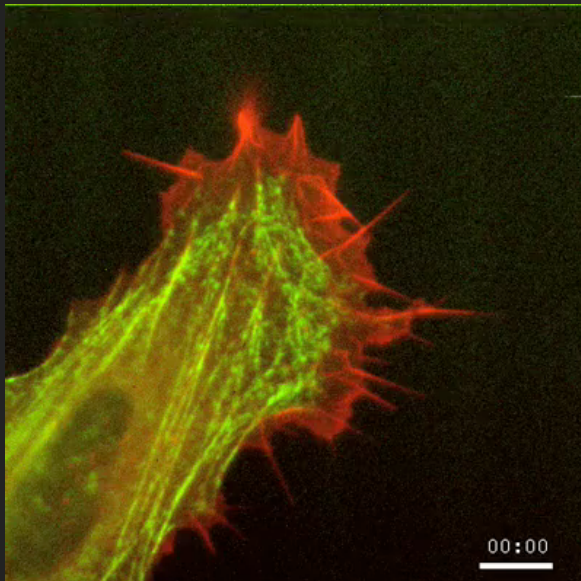
THE SUMMED FORCE VANISHES



THE SUMMED FORCE IS NOT ZERO

A NET FORCE APPEARS BECAUSE THE FILAMENT CONCENTRATION IS NOT HOMOGENEOUS

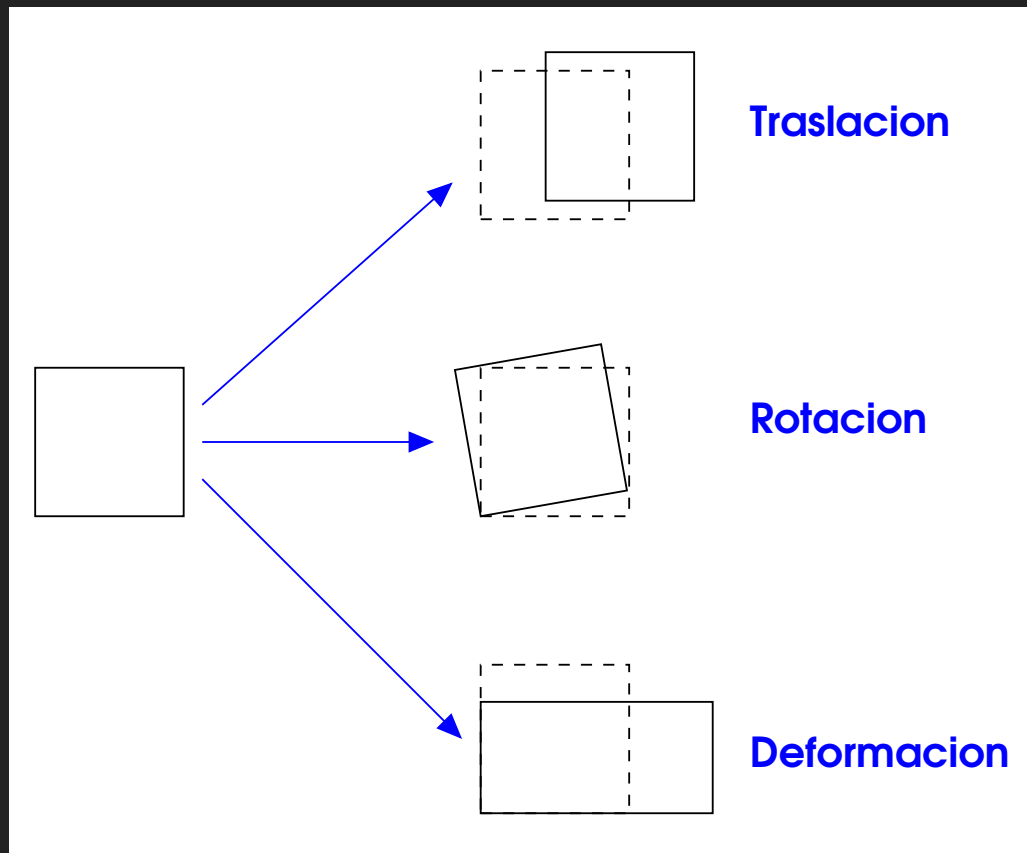
THIS FORCE MUST BE BALANCED WITH ANOTHER FORCE (E.G. FRICTION, THEN MOTION)



$$f = \nabla \cdot \sigma_A \quad \text{force density}$$

# DEFORMATION (STRAIN) TENSOR

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Only deformations have  
energy cost

That is, require forces



# DEFORMATION (STRAIN) TENSOR

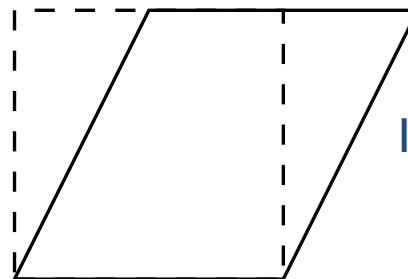
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Deformations can be described in terms of principal axis (directions)

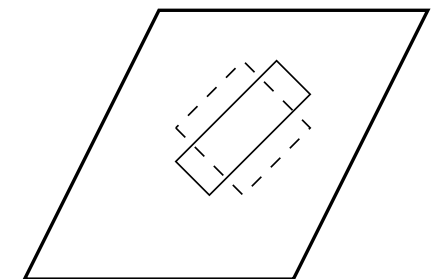
They are identified as the directions for which a rectangle deforms into a rectangle

These directions are perpendicular

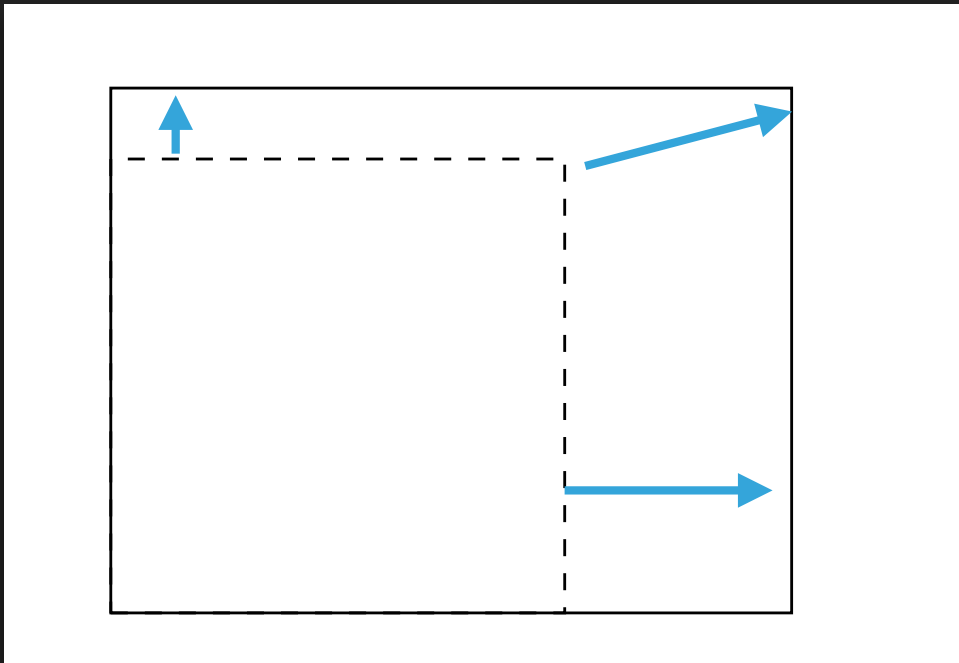
FOR EXAMPLE



IS EQUIVALENT TO



# DEFORMATION (STRAIN) TENSOR



$$\varepsilon_x = \frac{\Delta x}{L_x}$$
$$\varepsilon_y = \frac{\Delta y}{L_y}$$

$\varepsilon > 0$  stretched

$\varepsilon < 0$  compressed

$$\varepsilon = \begin{pmatrix} \varepsilon_x & 0 \\ 0 & \varepsilon_y \end{pmatrix}$$

Deformation matrix:

Strain tensor

# STRAIN - STRESS RELATION

---

## 1) Elastic materials

$$\sigma \propto \varepsilon$$

$$\sigma = Y\varepsilon$$

$Y$  Young modulus

Interpretation of the Young modulus

If  $\sigma = 1Y$ , then  $\varepsilon = 1$

$$\varepsilon = 1 = \frac{\Delta x}{L_x}$$

Deformation of 100%

Typical values: 1 kPa ... 1 GPa

## 2) Fluid materials

$$\sigma \propto \dot{\varepsilon}$$

$\eta$  Viscosity

$$\sigma = \eta\dot{\varepsilon}$$

# STRAIN - STRESS RELATION

---

## 3) Visco-elastic materials

$$\sigma = Y\varepsilon + \eta\dot{\varepsilon}$$

## 4) Active materials (living materials)

The stress tensor depends on the polarization axes and the intensity of the activity

# EXAMPLE: CELLULAR DEFORMATION

$$\begin{aligned}\sigma &= \sigma_E + \sigma_A \\ &= Y \begin{pmatrix} \varepsilon_x & 0 \\ 0 & \varepsilon_y \end{pmatrix} + \begin{pmatrix} \sigma_a & 0 \\ 0 & 0 \end{pmatrix}\end{aligned}$$

With free boundaries

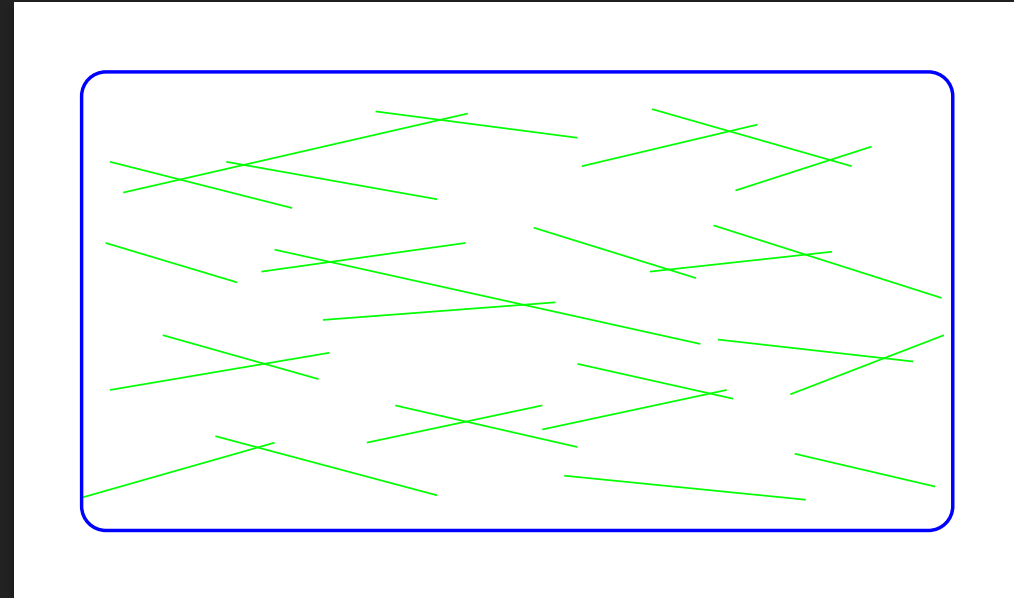
In the borders,  $\sigma = 0$

But, the mechanical equilibrium dictates that  $\sigma = \text{cte}$ .

Then, in all the cell,  $\sigma = 0$

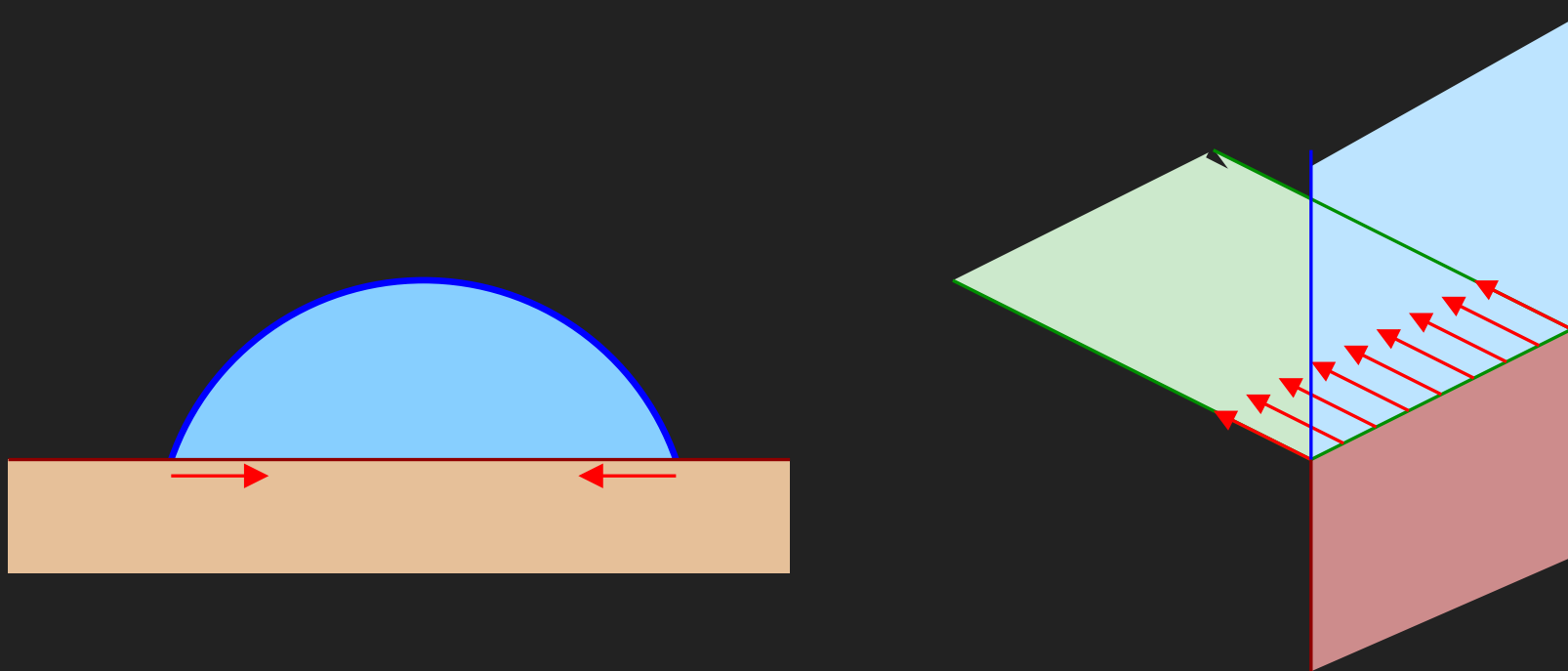
$$\boxed{\varepsilon_x = -\sigma_a/Y, \quad \varepsilon_y = 0}$$

The cell contracts



# EXAMPLE: CELL TRACTION

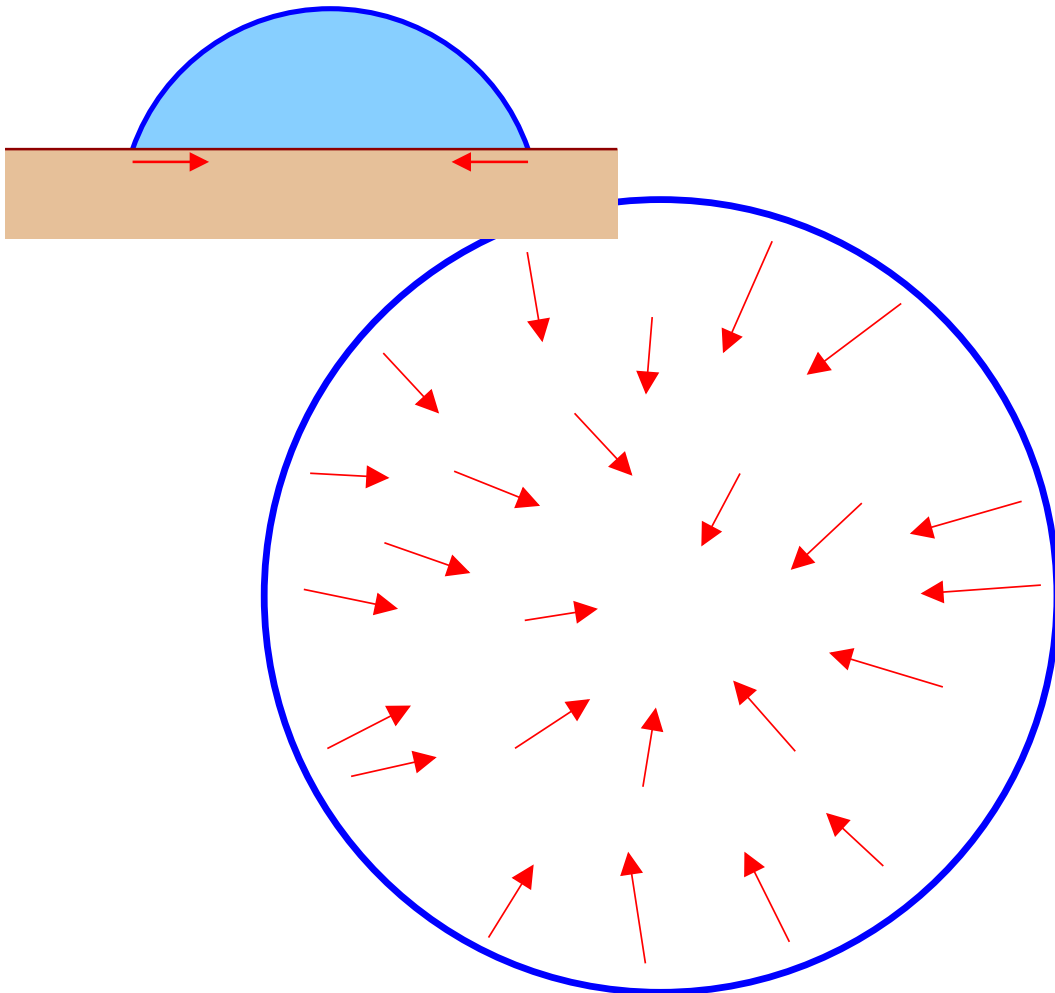
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The substrate is elastic. Then, it deforms

$$\epsilon_r = -\sigma_a / Y$$

# TRACTION FORCE MICROSCOPY



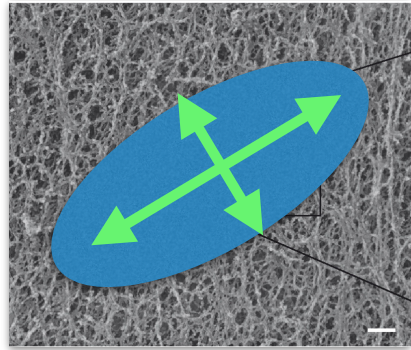
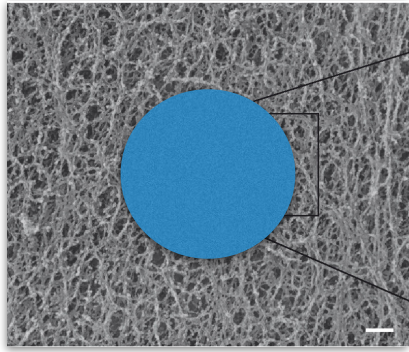
Place fluorescent beads  
in the substrate

Measure their  
displacement  $\vec{u}(\vec{r})$

Deduce the deformation  
tensor of the substrate  $\varepsilon$

Using  $\varepsilon = \sigma_a / Y_{\text{substrate}}$ ,  
compute the applied  
stresses  $\sigma_a$

# DEFORMABLE MICRO-DROPLETS



Spherical droplets are immersed in the cell

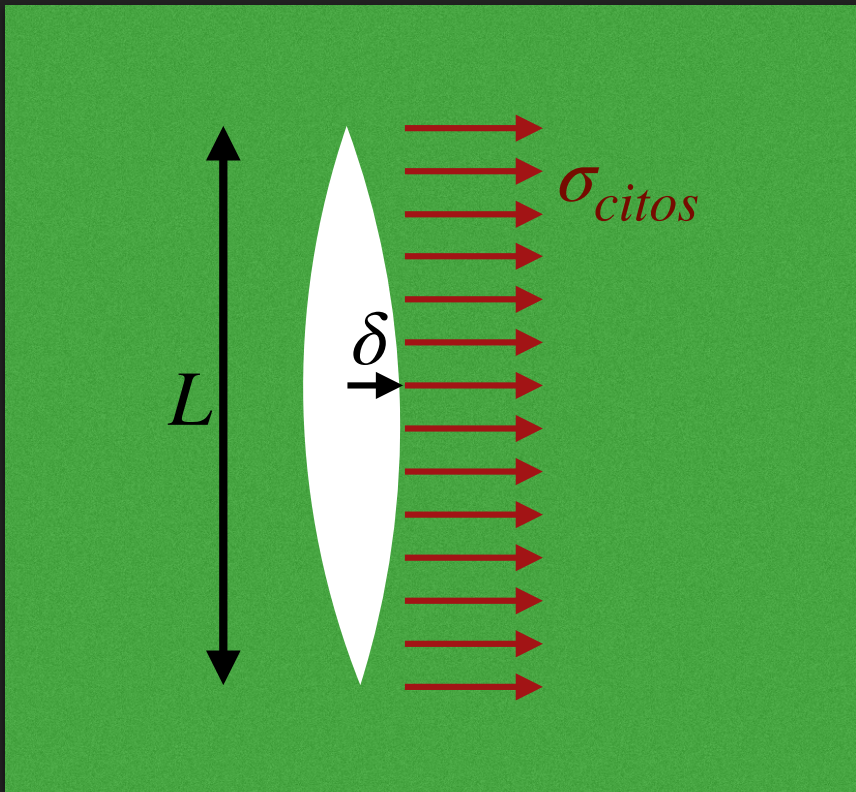
The stresses deform the beads and adopt an ellipsoidal shape

The new lengths give principal axes and the strains of the droplet  $\sigma_{droplet} = \epsilon / Y_{droplet}$

The stresses must be equal across the interface  $\sigma_{citos} = \sigma_{droplet}$



# LASER ABLATION



The cytoskeleton is generating an active stress  $\sigma_{citos}$

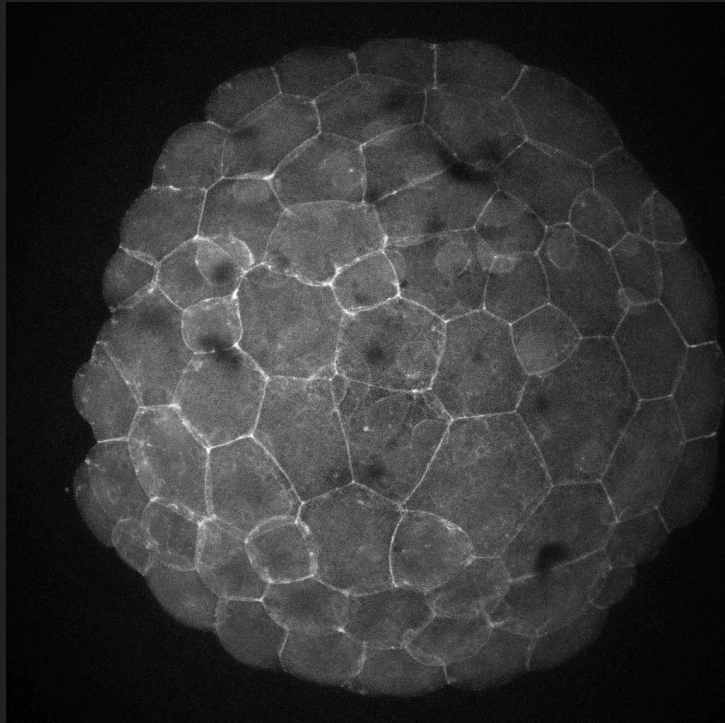
When the membrane is cut, a force appears in the new free surface.

To reach the new equilibrium (net zero force), the tissue contracts, generating an elastic force. The deformation is  $\epsilon = \sigma_{citos}/Y$

The retraction length is proportional to the cut length  $L$ , then

$$\delta \propto \epsilon L = \sigma_{citos} L / Y$$

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