



2025
October, 13-24

Innovative Biotechnological Approaches for Biofilm

Curso Binacional Uruguay - Chile 2025

Instituto de Investigaciones Biológicas Clemente Estable (IIBCE)
Instituto de Neurociencia Biomédica (BNI), ICBM, F-Med, U-Chile

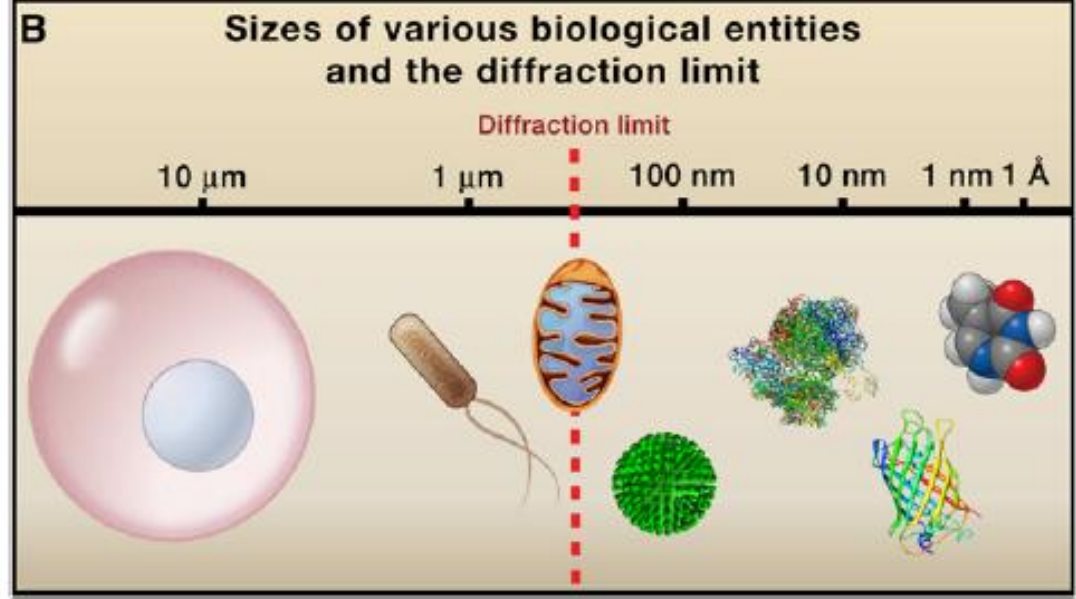
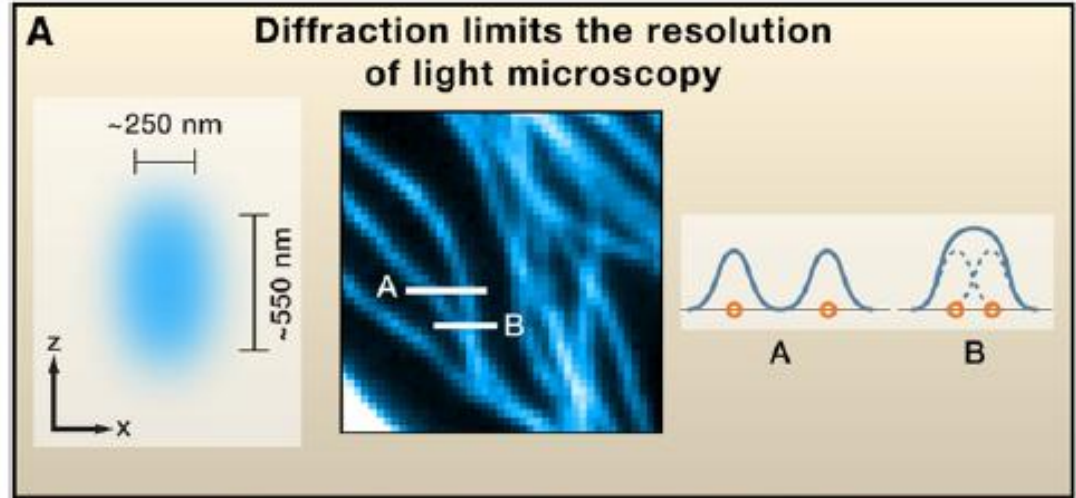
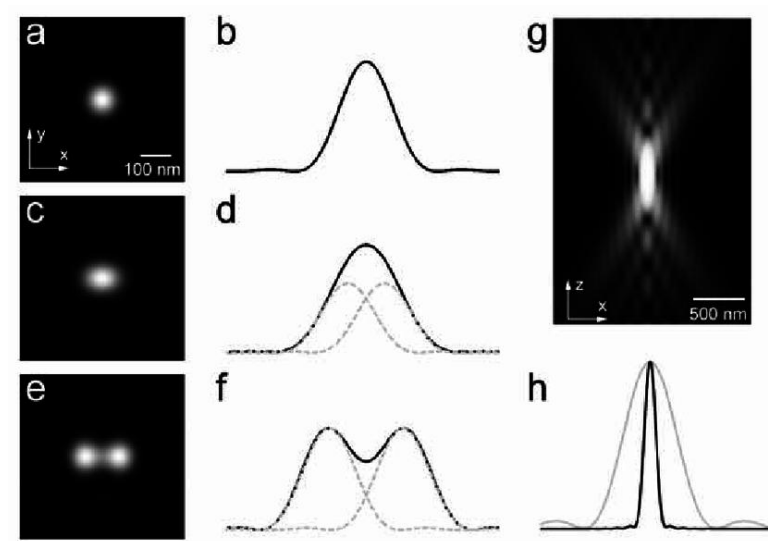
Prof. Dr. Steffen Härtel

www.scian.cl / www.cimt.cl / www.cens.cl / www.bni.cl / www.rsdue.cl

Laboratory for Scientific Image Analysis (SCIAN-Lab)
Centro de Informática Médica y Telemedicina (CIMT)
Centro Nacional en Sistemas de Información en Salud (CENS)
Biomedical Neuroscience Institute (BNI)
Red de Salud Digital de Universidades del Estado (RSDUE)
Institute of Biomedical Sciences (ICBM)
Núcleo Milenio de AutoOrganización y Mecánica de Tejidos (SELFO)

Facultad de Medicina, Universidad de Chile

| -> Diffraction limited Microscopy



Bertocchi, Cristina & Goh, Wah & Zhang, Zhen & Kanchanawong, Pakorn. (2013). Nanoscale Imaging by Superresolution Fluorescence Microscopy and Its Emerging Applications in Biomedical Research. *Critical reviews in biomedical engineering*. 41. 281-308. 10.1615/CritRevBiomedEng.2014010448.

| -> Beyond diffraction

M Goepfert-Mayer
1906-1972

M Gustafson
1960-2011

S Hell
MPI Göttingen
BIOQUANT Hdg

E Betzig
Janelia Farm



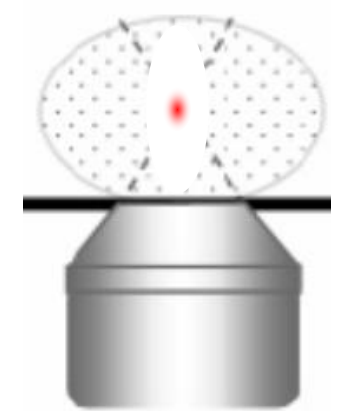
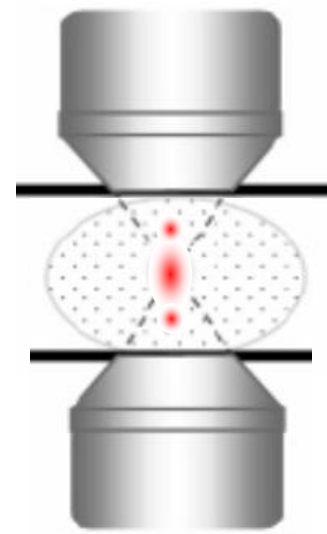
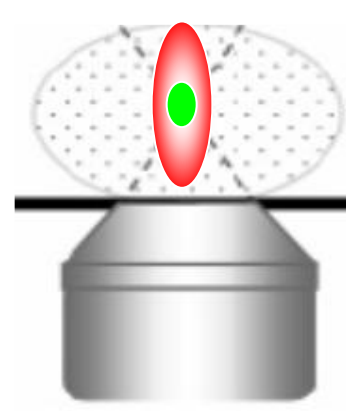
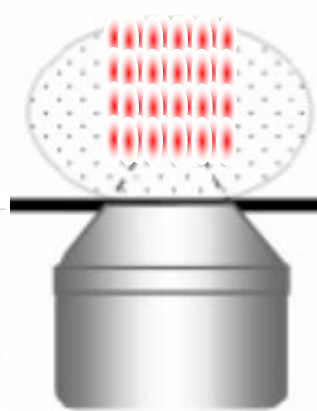
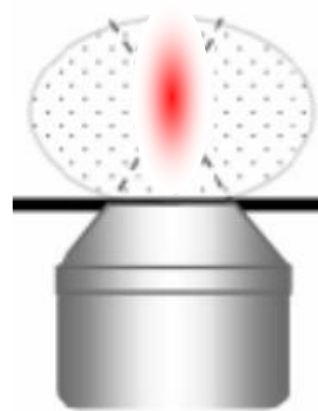
FWHM(xy) $\sim \lambda/2$

$\sim \lambda/4$

$\sim \lambda/\infty$

$\sim \lambda/4$

$\sim \lambda/100$



2-photon

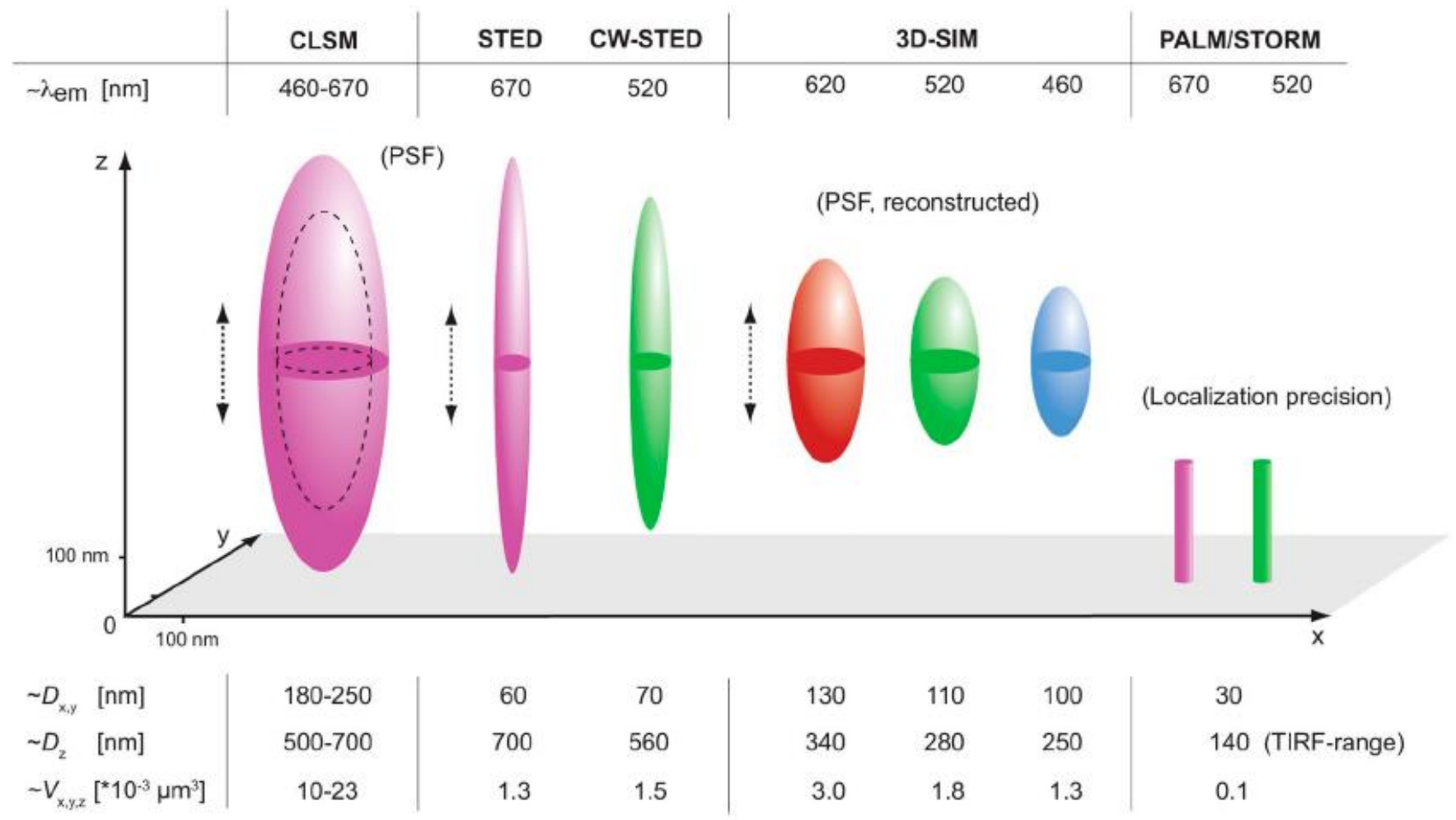
SIM

STED

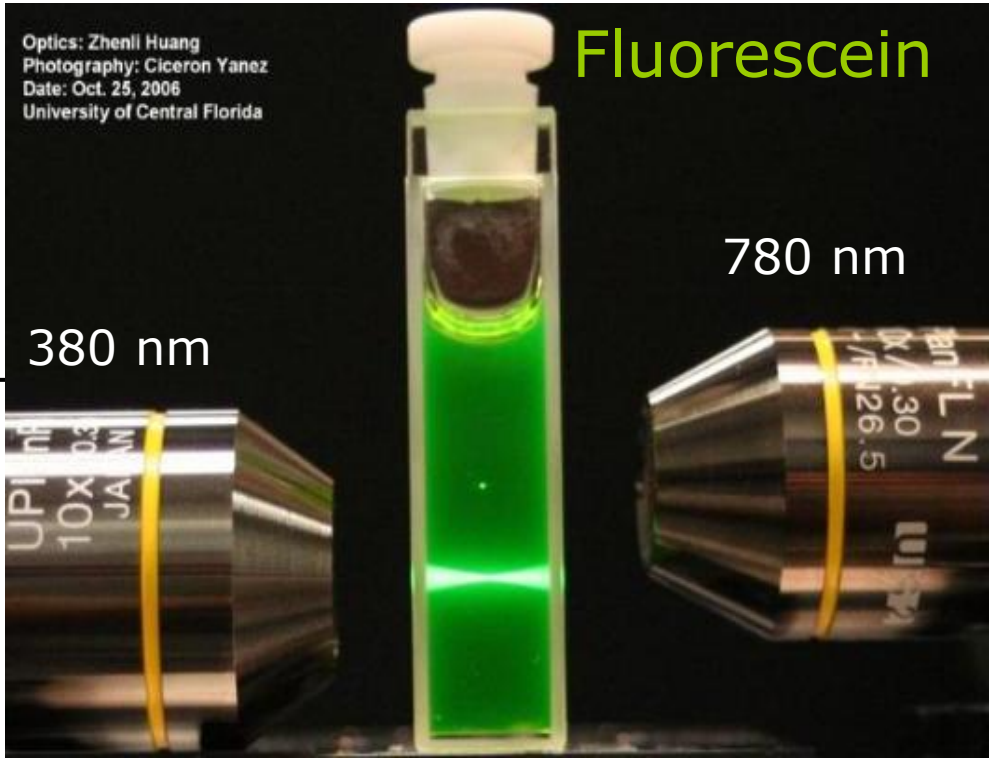
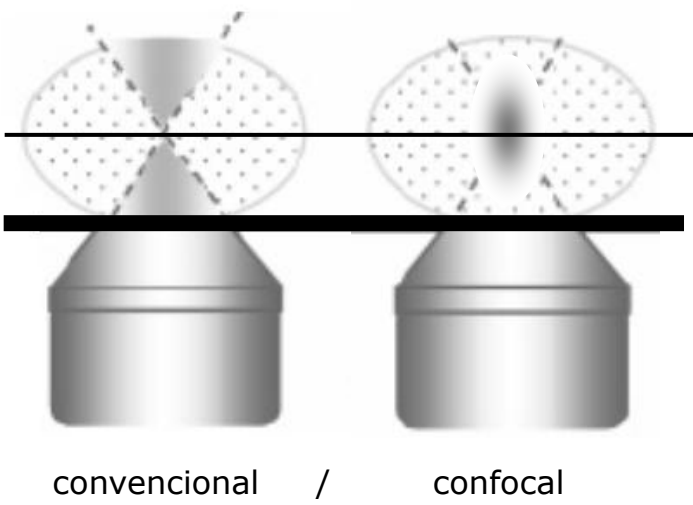
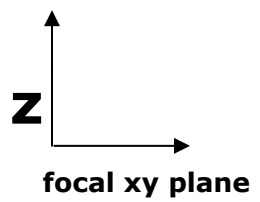
4- π

PALM

|-> PSF overview



| Best localization: confocal microscopy



Fluorescence Imaging Modes in Live-Cell Microscopy

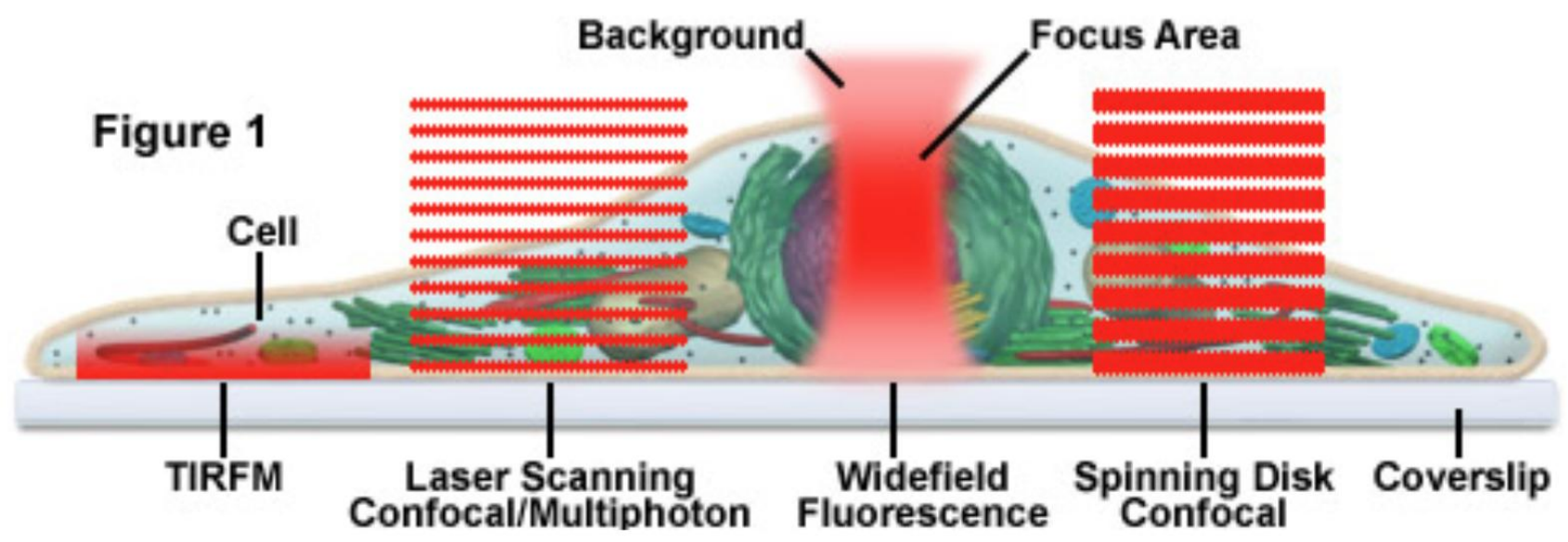


Figure 1

Cell

TIRFM

Laser Scanning Confocal/Multiphoton

Widefield Fluorescence

Spinning Disk Confocal

Coverslip

Background

Focus Area

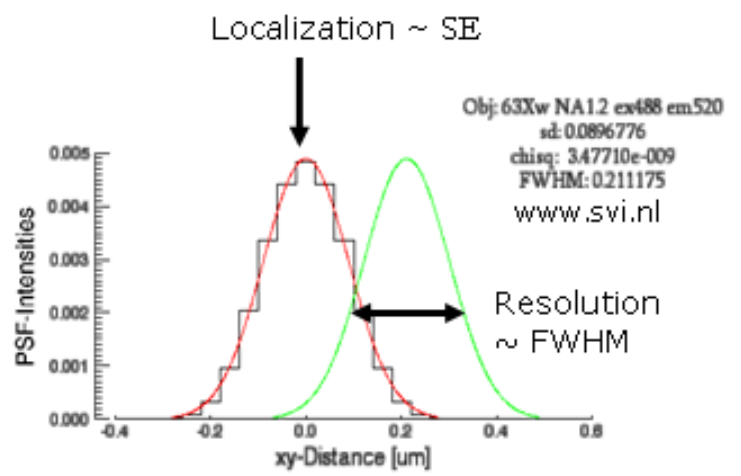
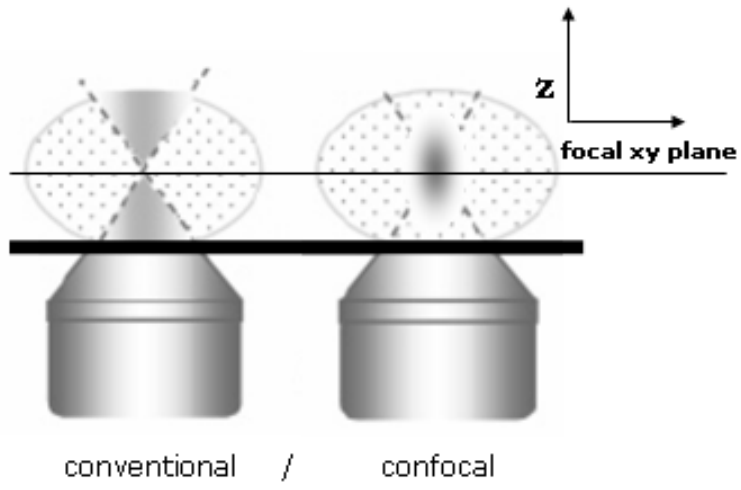
| Diffraction limited microscopy

E. Abbe († 1905)

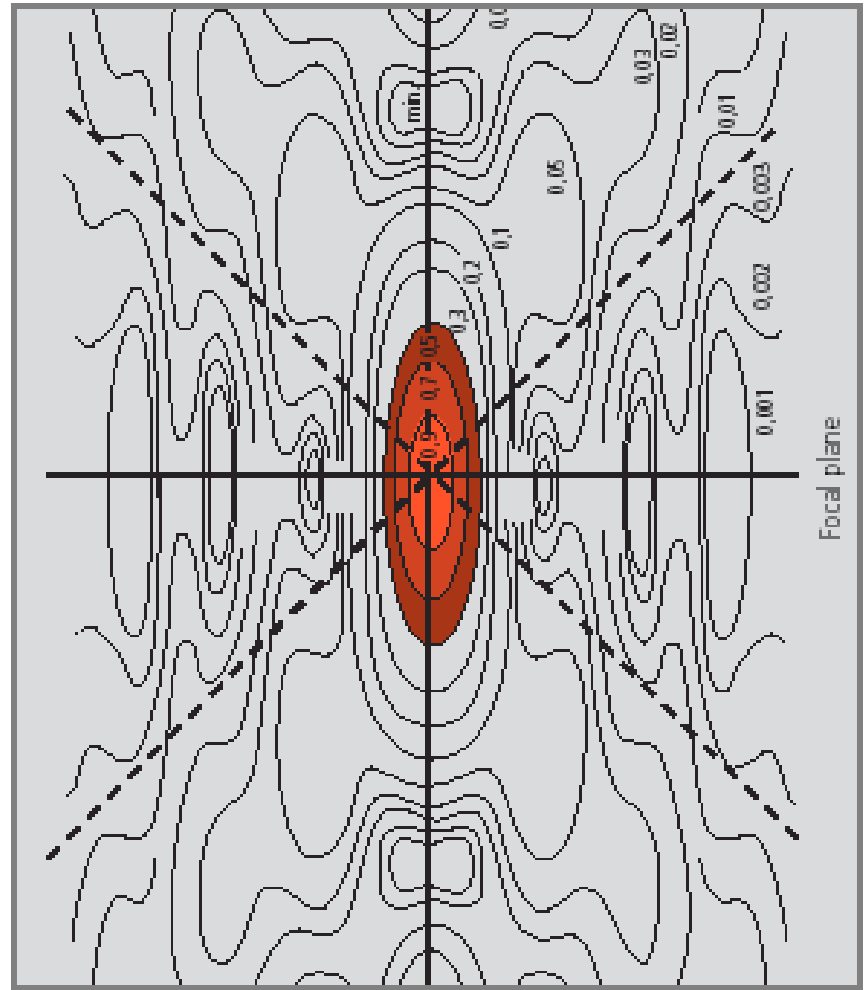
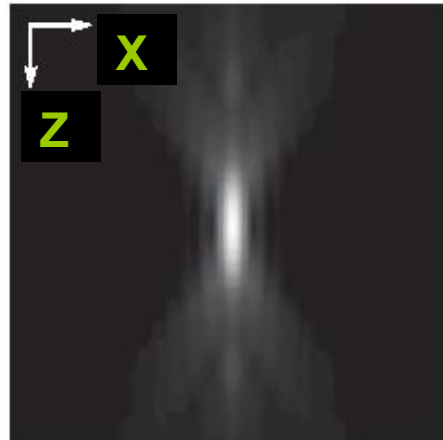
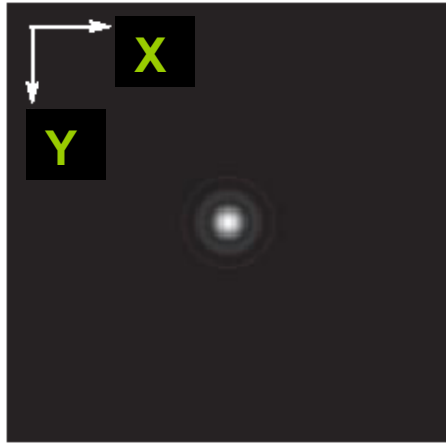


$\lambda / 2 \cdot NA \sim \lambda / 2$ Resolution (Full Width at Half Maximum, FWHM)

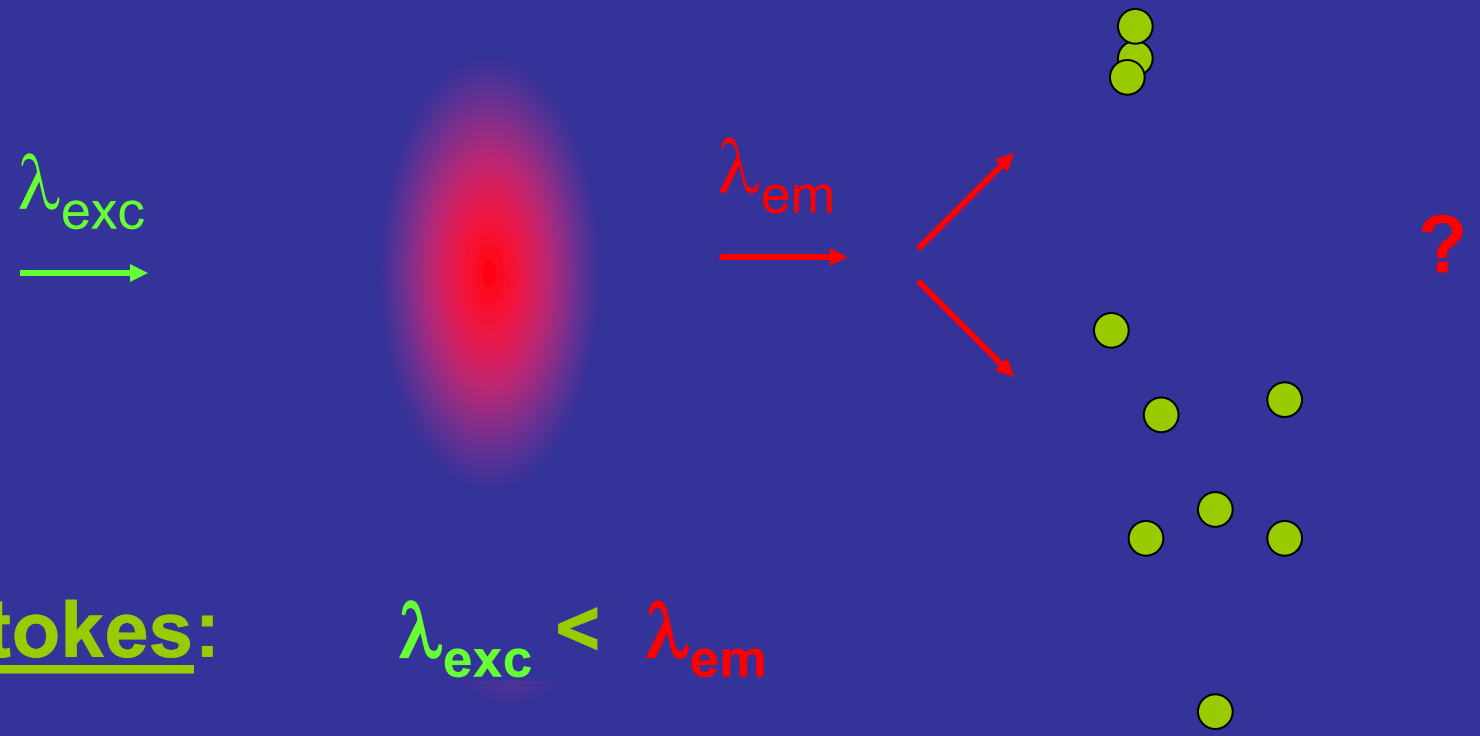
FWHM / $N^{1/2}$ Localization, N number of photons



| -> PSF



| -> Convolution



|-> Convolution

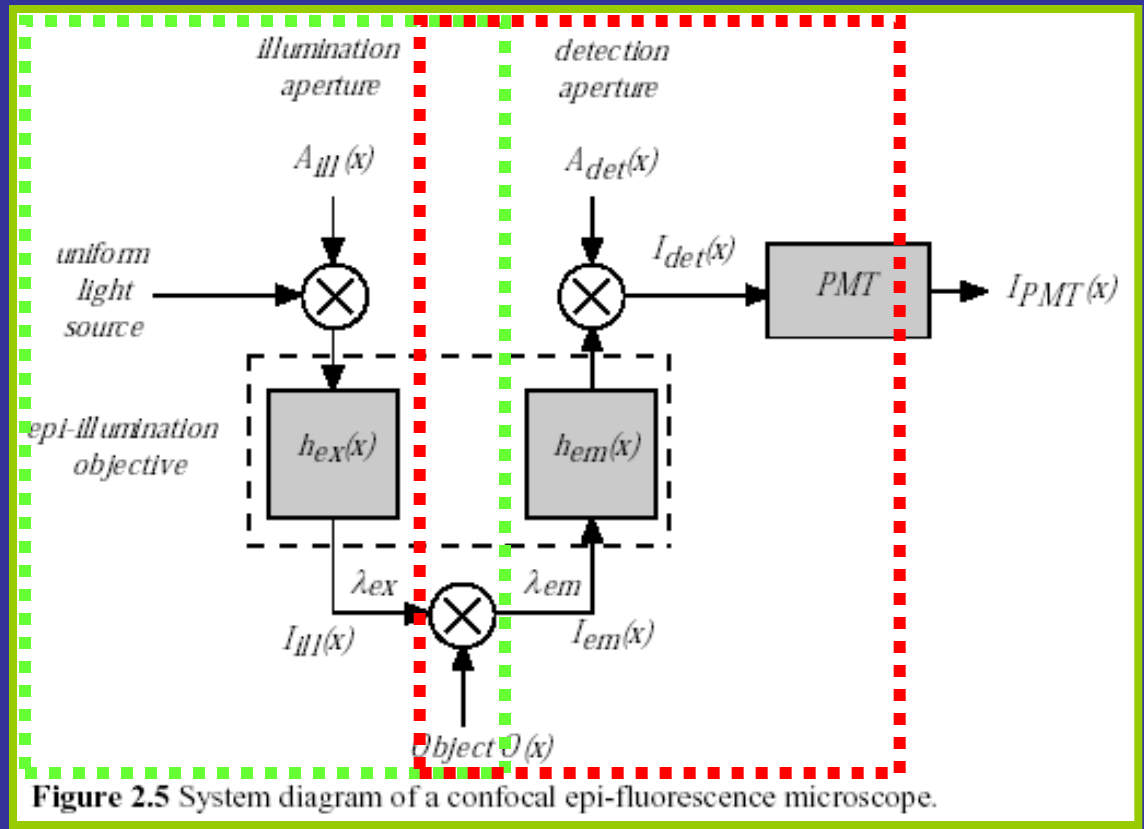
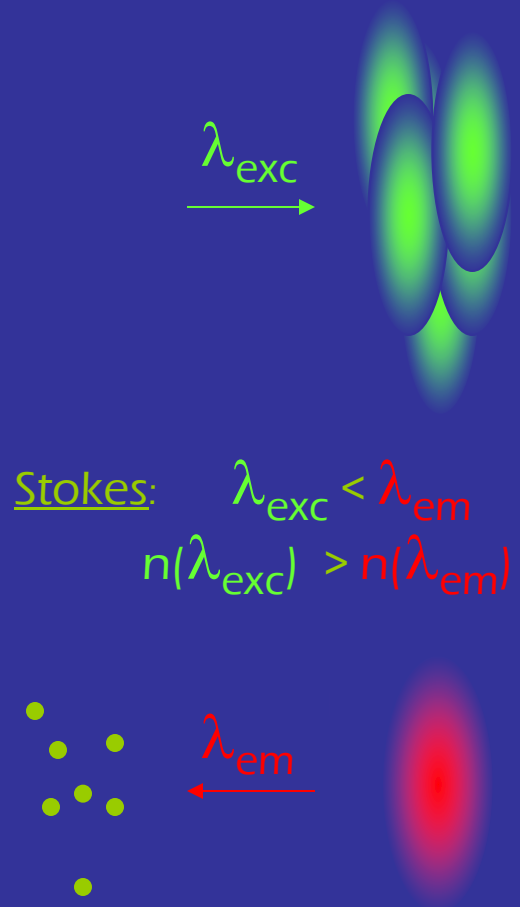
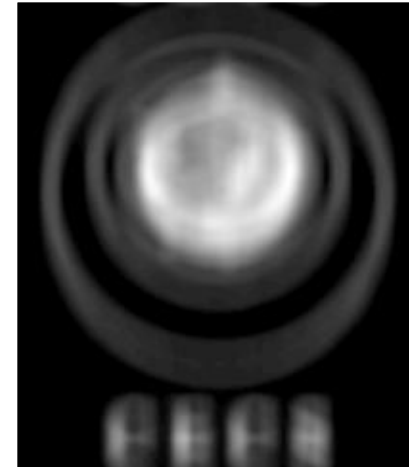
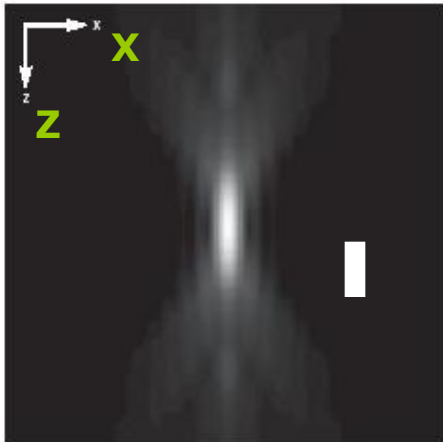


Figure 2.5 System diagram of a confocal epi-fluorescence microscope.

| -> Convolution



PSF:

$\Delta xy \sim 500 \text{ nm}$ | $\Delta z \sim 1500 \text{ nm}$

PSF: Point Spread Function

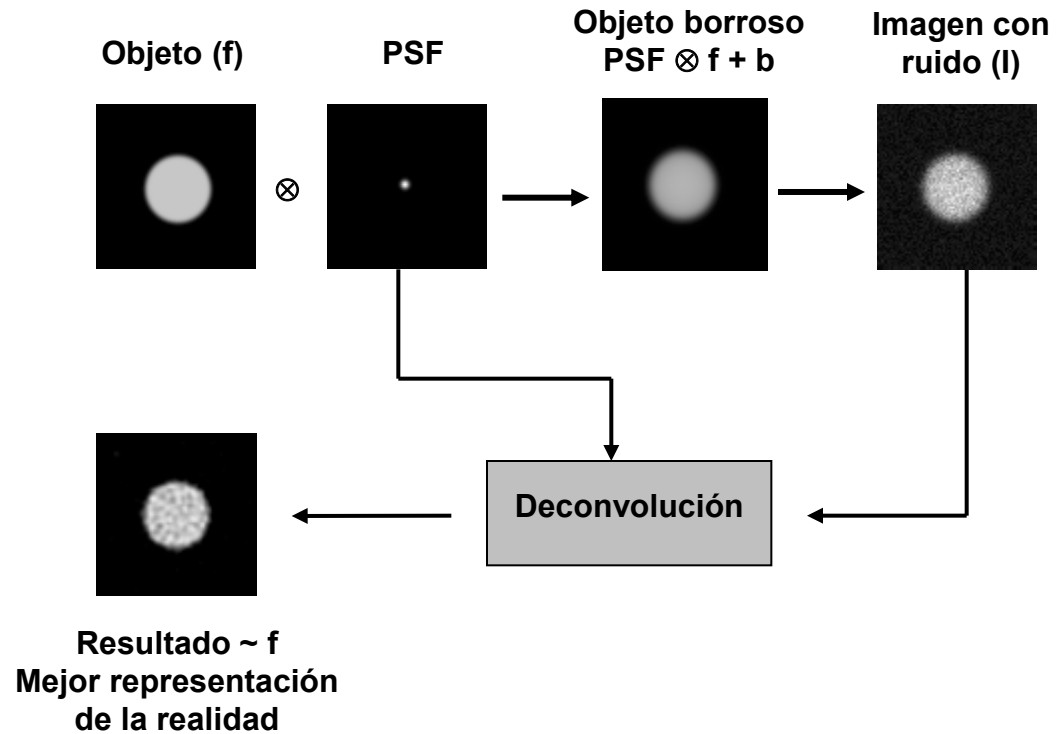
f: Object Function

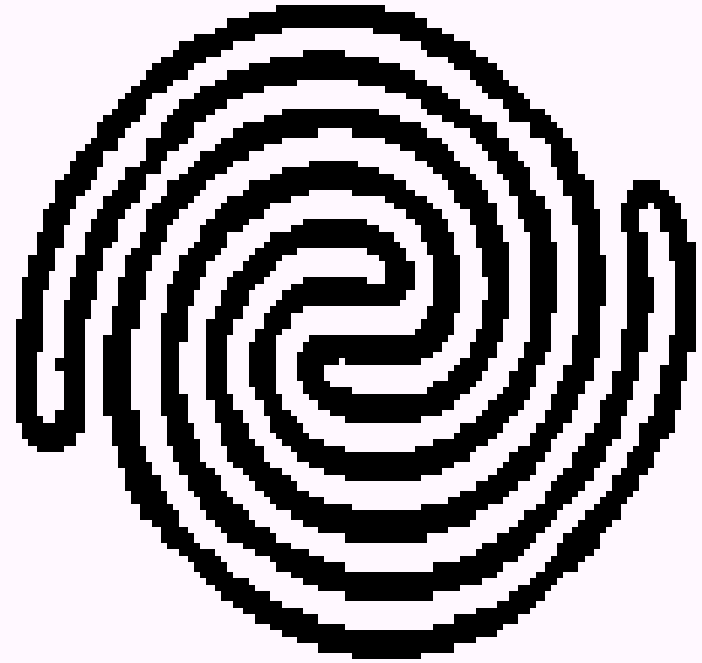
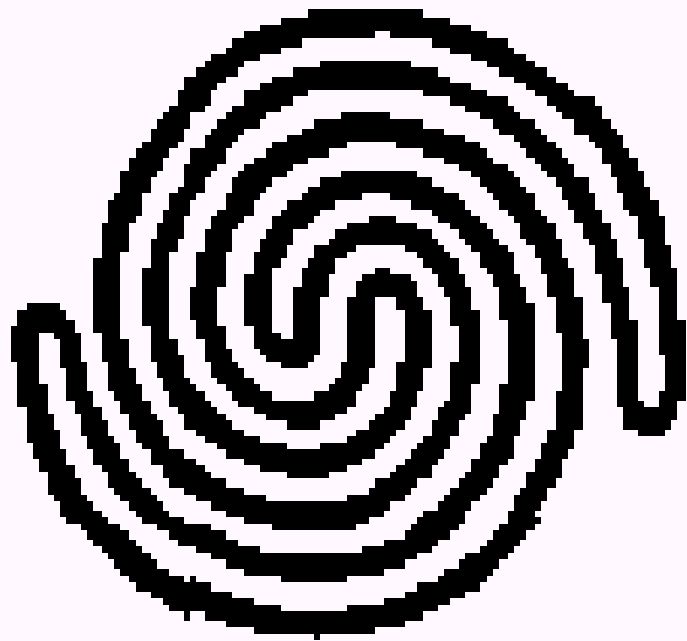
b: Offset Function

I: Image Matrix

N: Noise Function

$$N/PSF(x, y, z) \otimes f(x, y, z) + b(x, y, z) = I(x, y, z)$$

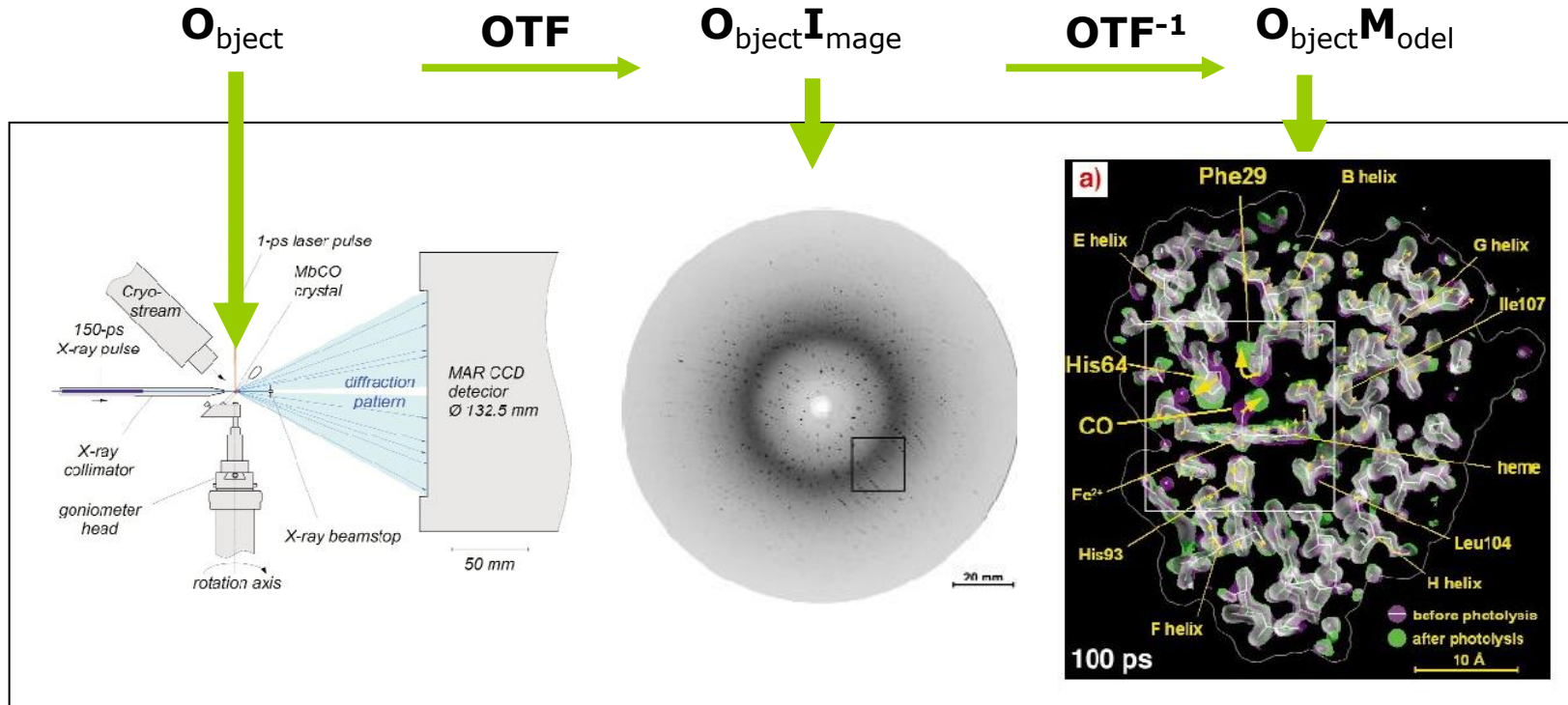




OTF: Object/Optical Transfer Function

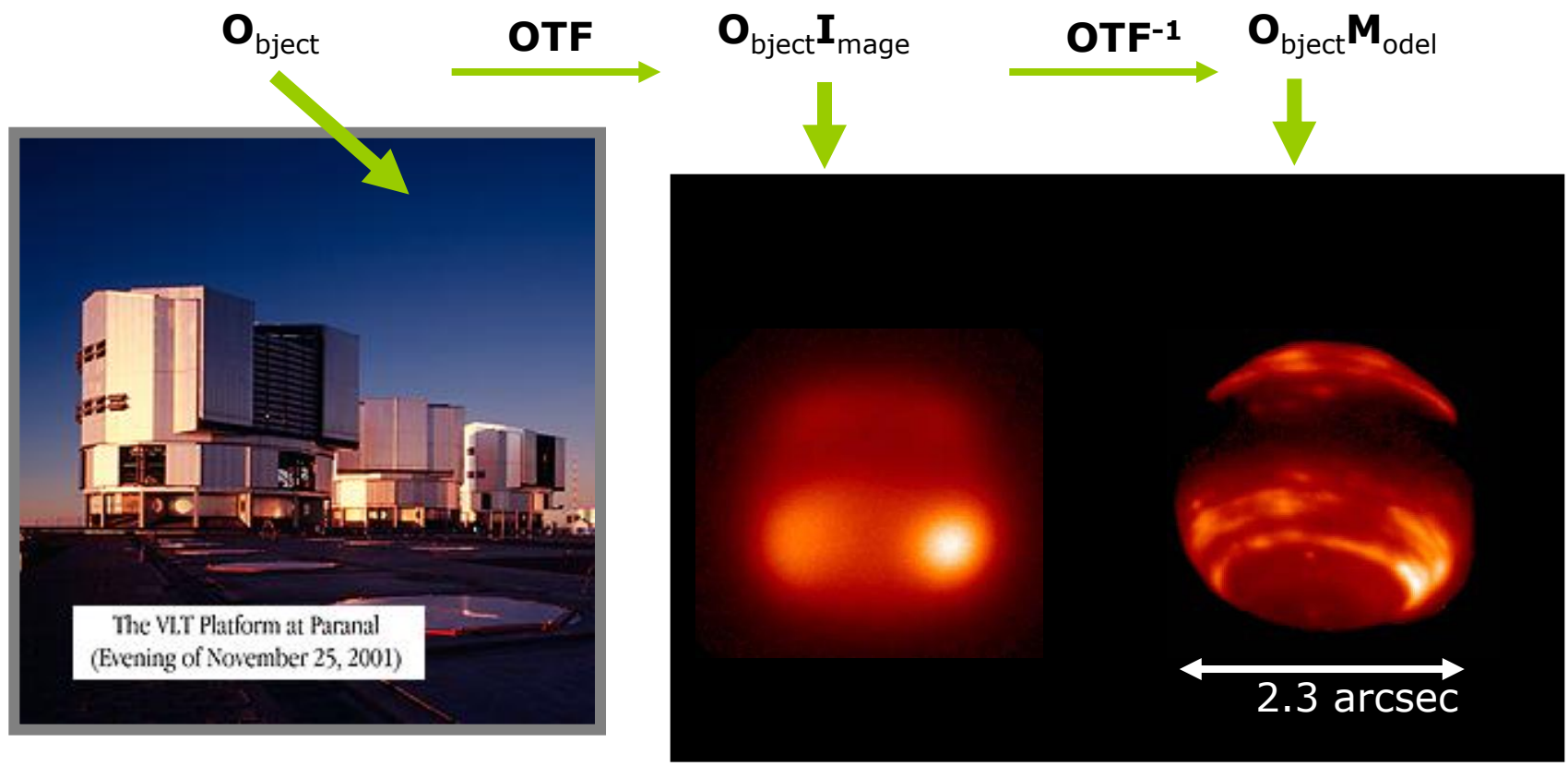
Myoglobin in Action | Picosecond Laue Crystallography Diffraction Data

Schotte et al (2003) Science

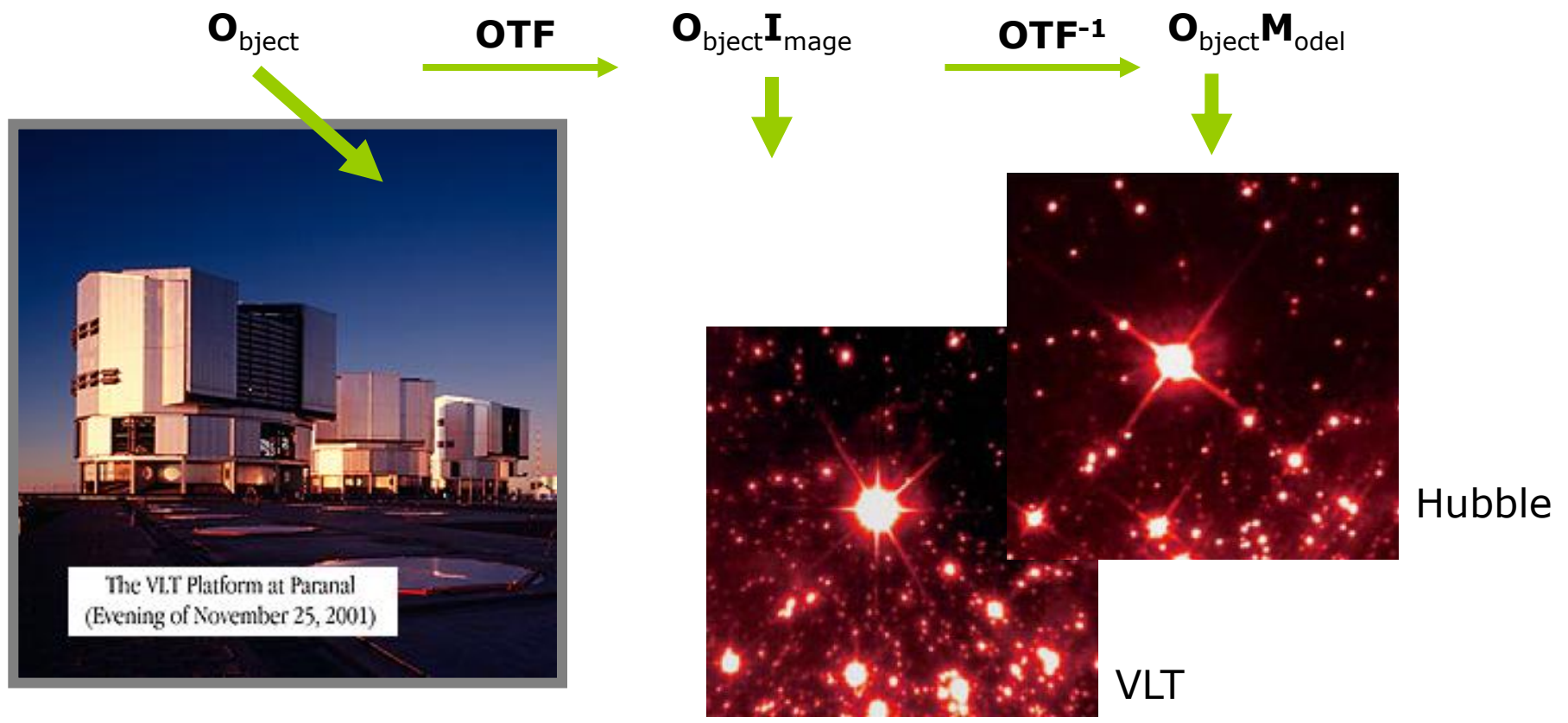


<http://www.youtube.com/watch?v=lnKIBZYarzM>

Diffraction Limited Resolution for a 10m telescope $\sim \lambda/D \sim 0.01$ arcsec
 is limited to ~ 0.5 arcsec by the turbulent atmosphere.
 NAOS creates an artificial star at 90 km altitude in the Earth's mesosphere.
 The Laser Guide Star is used to correct atmospheric effects

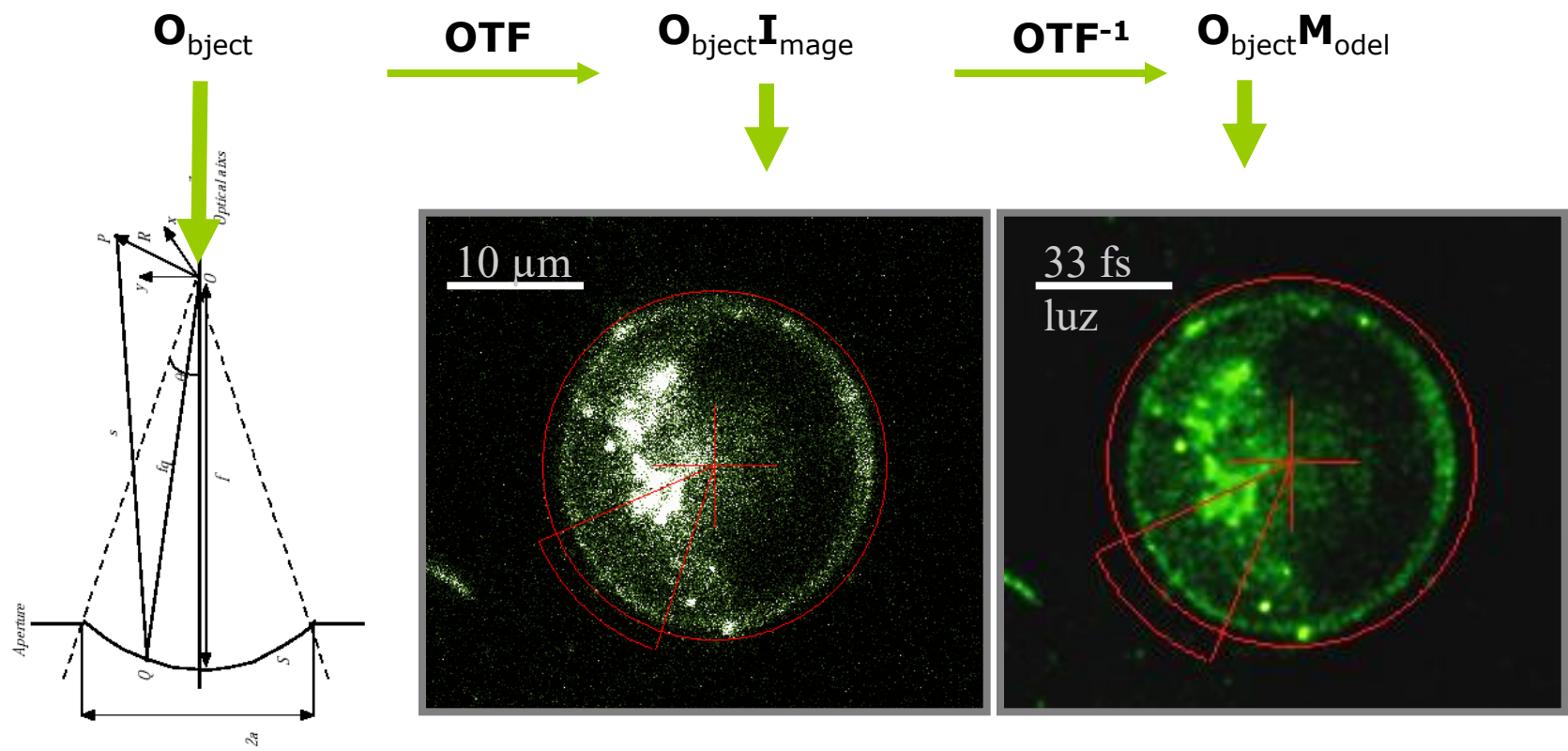


Diffraction Limited Resolution for a 10m telescope $\sim \lambda/D \sim 0.01$ arcsec is limited to ~ 0.5 arcsec by the turbulent atmosphere.

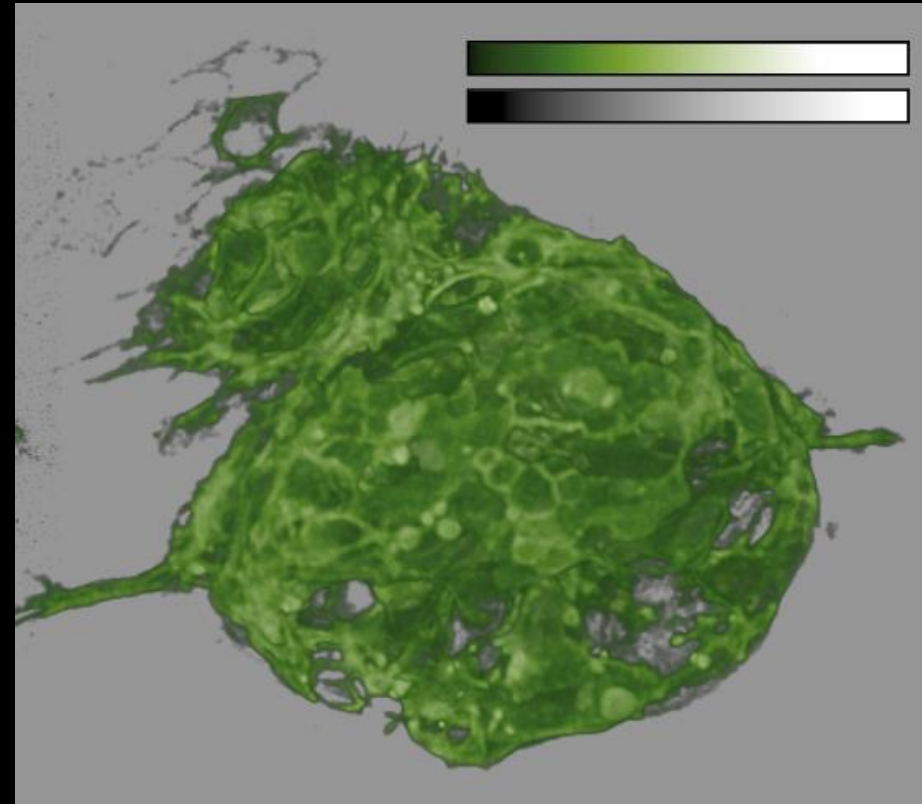
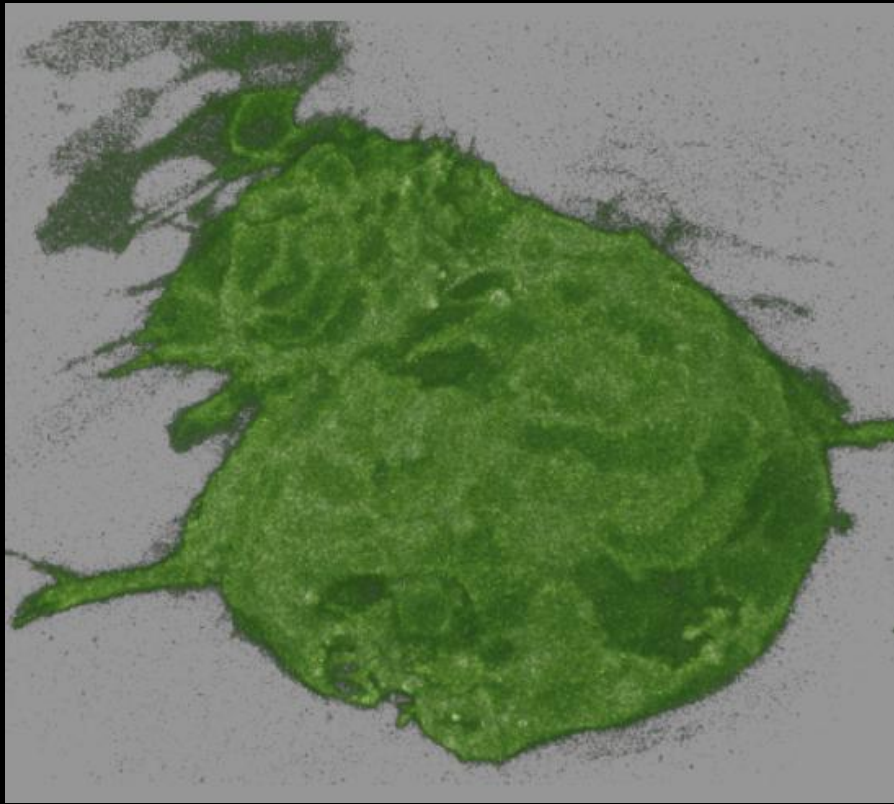


Confocal Microscopy | From Geometric Optics to Diffraction Theory

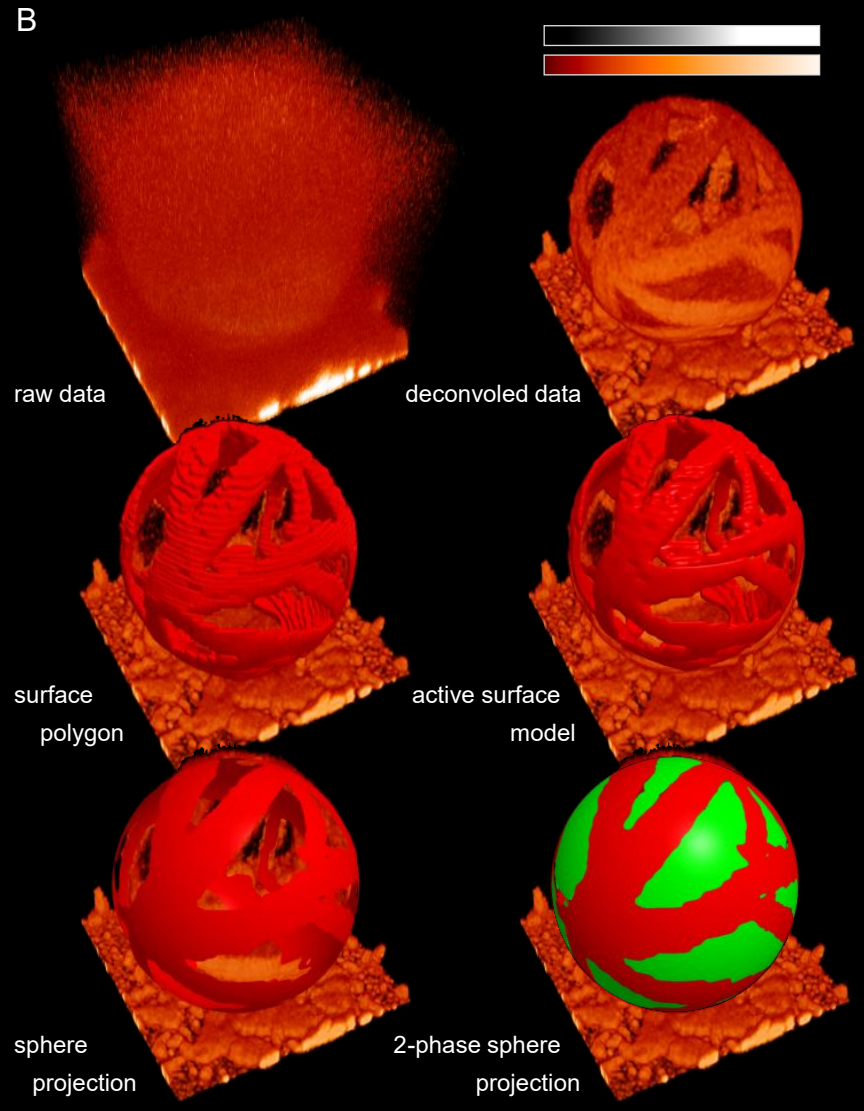
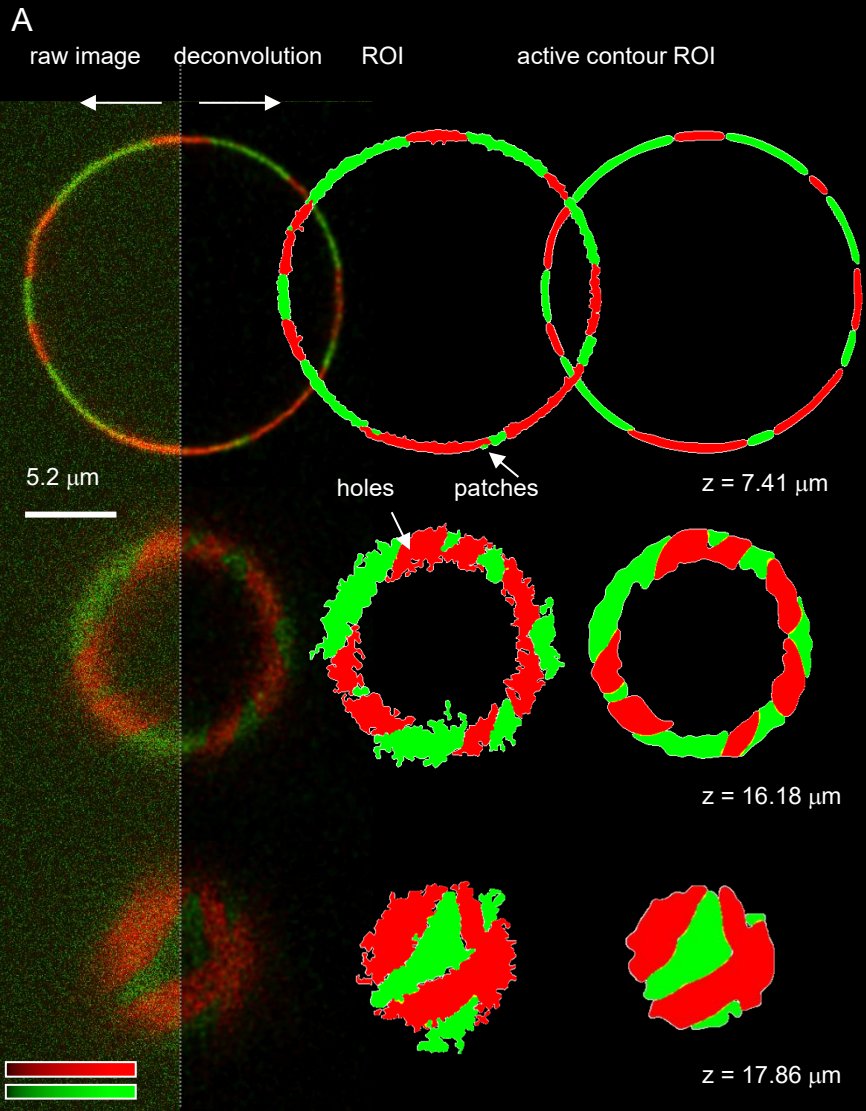
Diffraction: The deviation of an electromagnetic wavefront from the path predicted by geometric optics when the wavefront interacts with a physical object such as an opening or an edge.



|-> Deconvolution



| -> Deconvolution



PSF: Point Spread Function

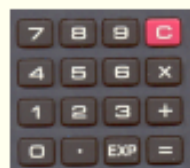
f: Object Function

b: Offset Function

I: Image Matrix

N: Noise Function

$$N / (PSF(x, y, z) \otimes f(x, y, z) + b(x, y, z)) = I(x, y, z)$$



Calculator

[Numerical aperture](#)

confocal

widefield

nipkow

4Pi

Select one

[Excitation wavelength](#)

1.3

[Emission wavelength](#)

488 (nm)

520 (nm)

[Number of excitation photons](#)

1

[Backprojected pinhole radius](#)

250 (nm)

[B.P. distance between pinholes](#)

2.53 Only for Nipkow disks (μm)

[Lens medium refractive index](#)

1.515

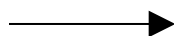
[Specimen medium refractive index](#)

1.45

[Acquisition depth](#)

0 (μm)

Calculate also PSF



PSF: Point Spread Function

f: Object Function

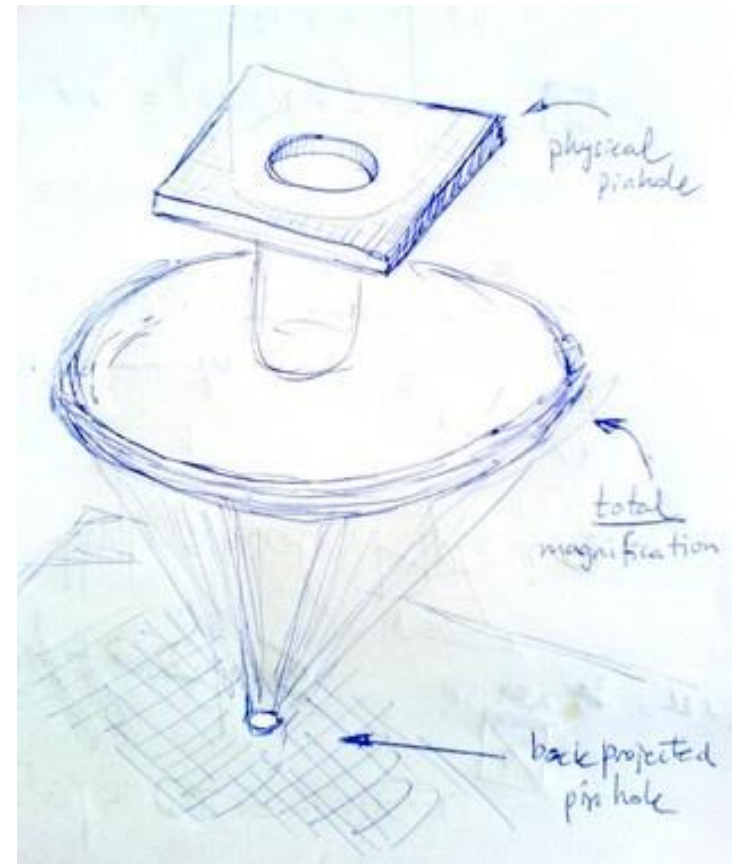
b: Offset Function

I: Image Matrix

N: Noise Function

$$N / (PSF(x, y, z) \otimes f(x, y, z) + b(x, y, z)) = I(x, y, z)$$

Backprojected confocal pinhole



PSF: Point Spread Function

f: Object Function

b: Offset Function

I: Image Matrix

N: Noise Function

$$N/(PSF(x, y, z) \otimes f(x, y, z) + b(x, y, z)) = I(x, y, z)$$

Biorad

- [Biorad MRC 500, 600 and 1024](#)
- [Biorad Radiance](#)

Leica

- [Leica confocals TCS 4d, SP1 and NT](#)
- [Leica confocal SP2](#)
- [Leica confocal SP5](#)

Nikon

- [TE2000-E with the C1 scanning head](#)

Olympus

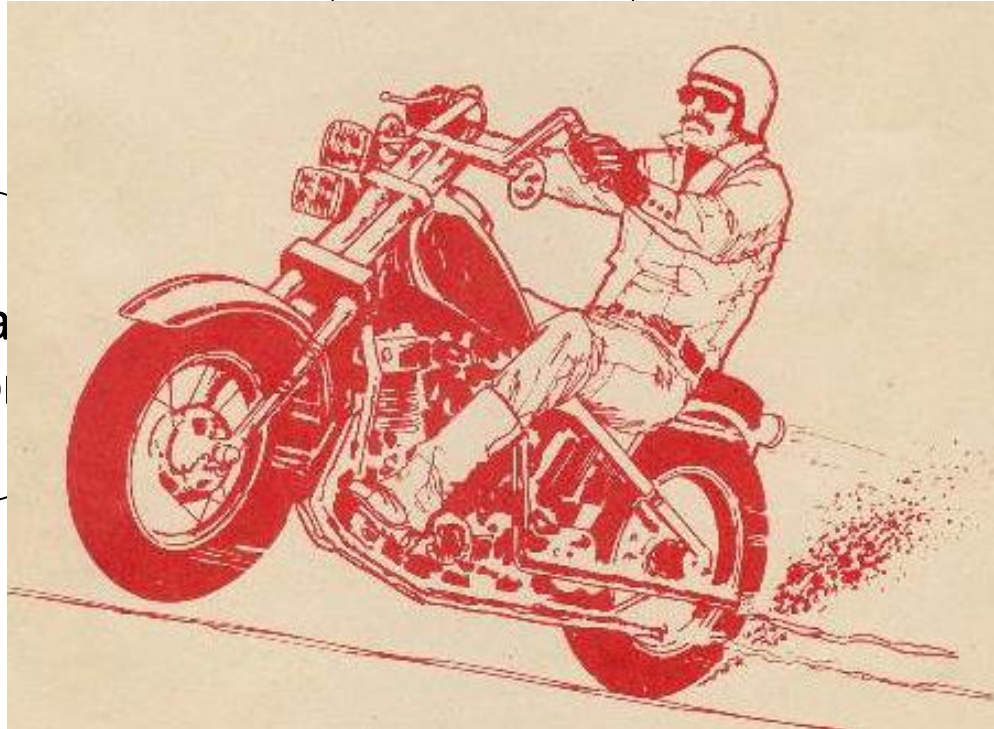
- [Olympus FV300](#)
- [Olympus FV500](#)
- [Olympus FV1000](#)

Zeiss

- [Zeiss LSM410 inverted](#)
- [Zeiss LSM510](#)

| -> Noise

Informa
Theor



atistical
ysics

Literature: eg. Noise Theory and Application to Physics: Philippe Réfrégier, Springer

PSF: Point Spread Function

f: Object Function

b: Offset Function

I: Image Matrix

N: Noise Function

- *Black Body Irradiation (Poisson)*

- *Detector Noise (Gauss)*

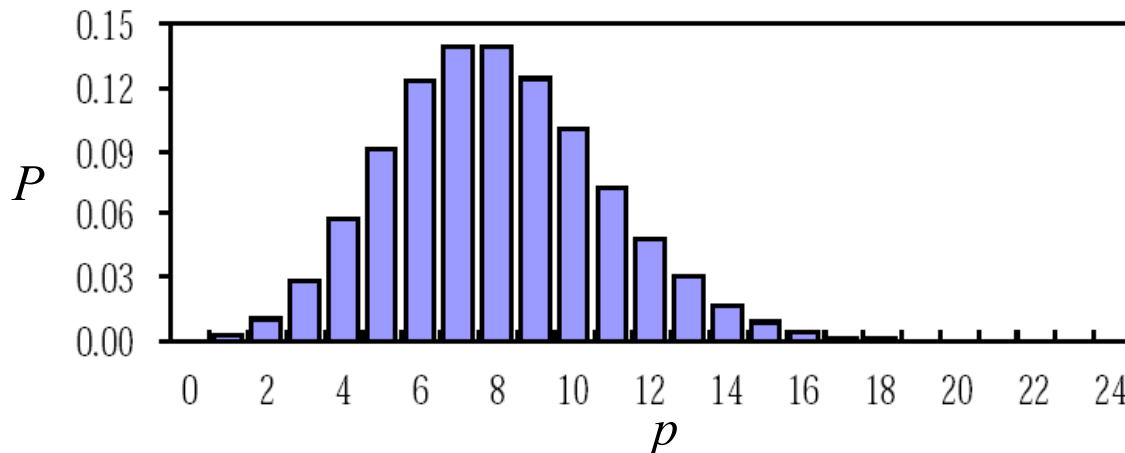
$$N(PSF(x, y, z) \otimes f(x, y, z) + b(x, y, z)) = I(x, y, z)$$

$$P(p, \mu) = \frac{\mu^p}{p!} \cdot e^{-\mu}$$

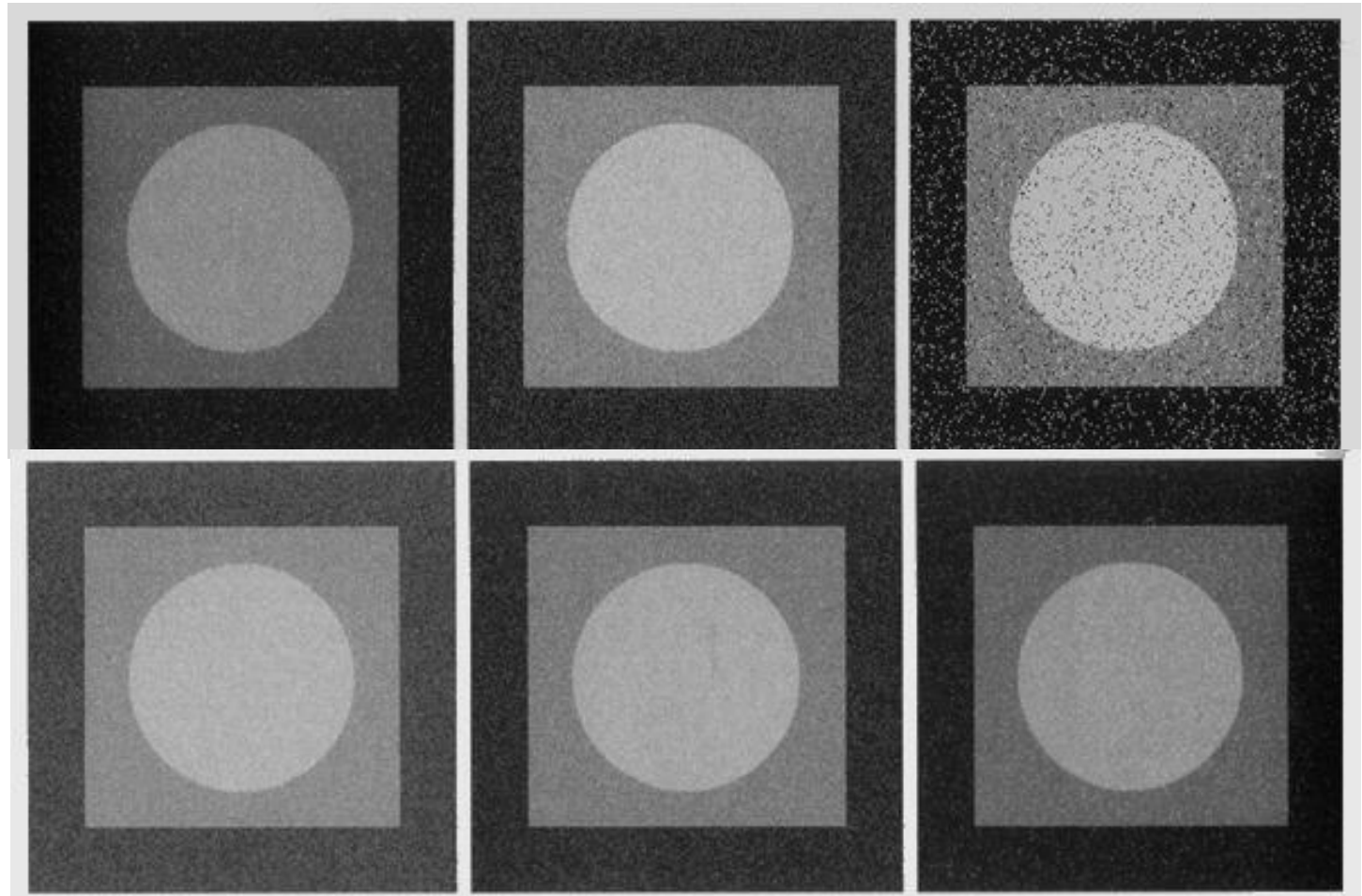
$$1. \bar{p} = \mu = \sigma^2, sd = \sigma = \sqrt{\bar{p}} = \sqrt{\mu}$$

$$2. \text{counting} : \bar{p} \pm \sqrt{\bar{p}}$$

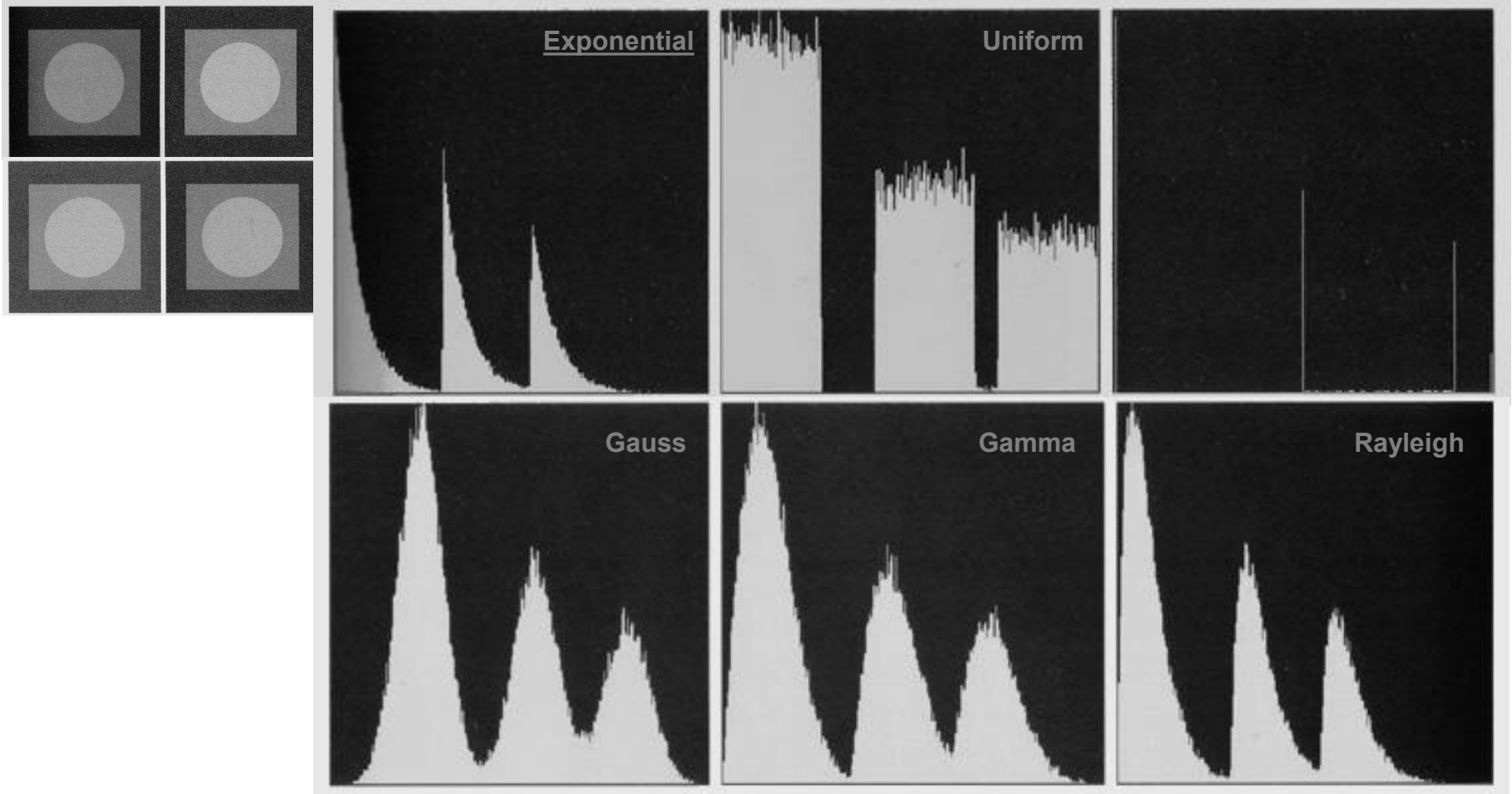
$$3. \text{Poisson (discrete)} \rightarrow \text{Gauss (continuous)} : \mu \rightarrow \infty$$



| -> Noise



| -> Noise



The Signal to Noise ratio (SN) is a number not always easy to estimate. The easiest way to obtain some figures is to look at the textures of bright areas in your object image. In the figure at left you see examples of such textures obtained from originally the same object image to which various levels of poisson noise were added.

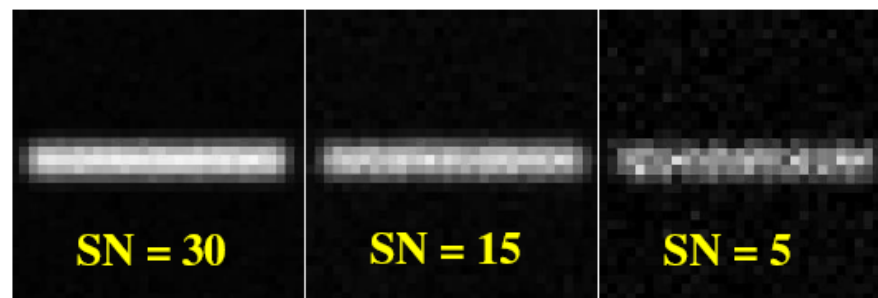
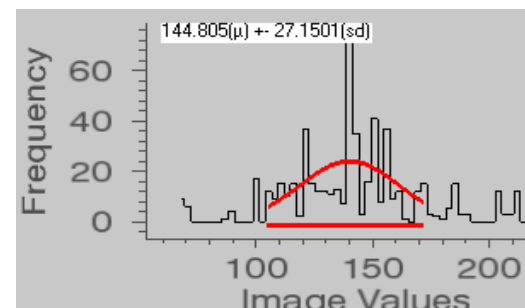
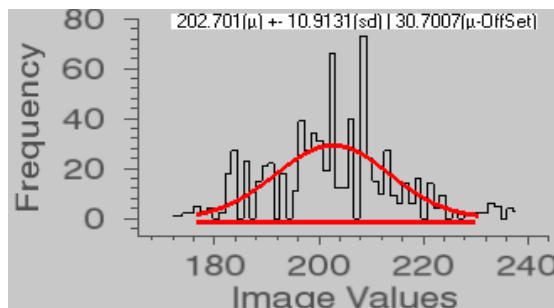
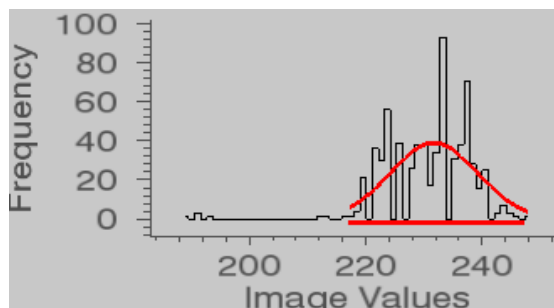


Figure 9. Images with different generated noise levels

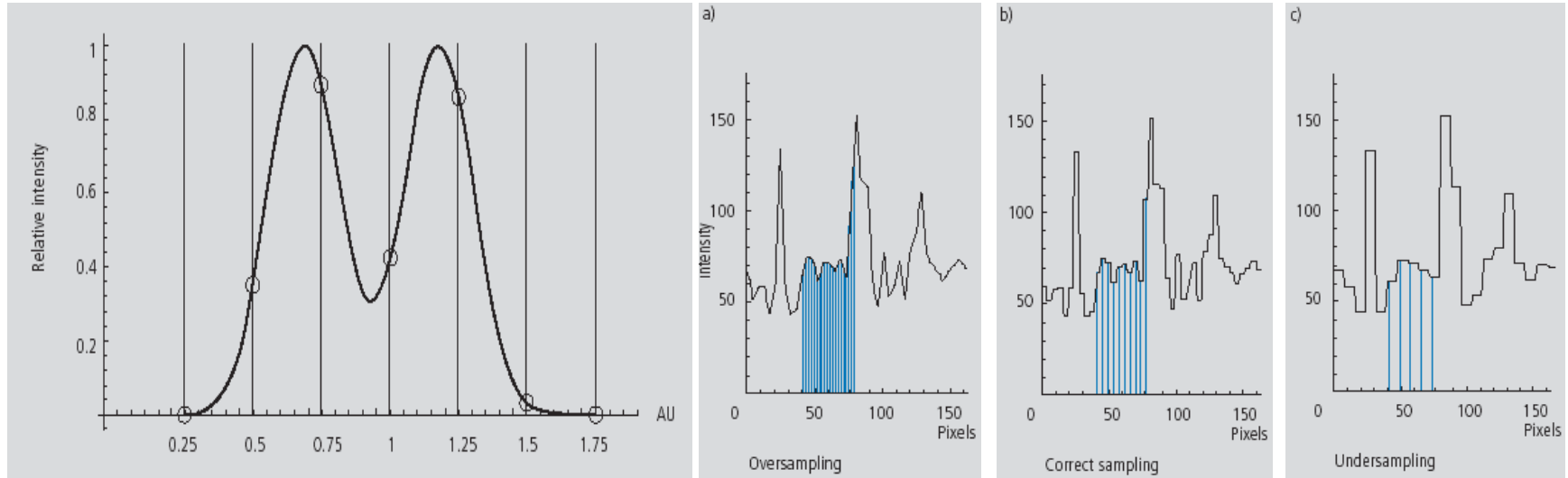


$$SNR = \frac{\bar{I}}{\sigma} = \frac{\bar{I}}{\sqrt{\sigma^2}} = \frac{229}{7.5}$$

$$SNR = \frac{\bar{I}}{\sigma} = \frac{\bar{I}}{\sqrt{\sigma^2}} = \frac{200}{10}$$

$$SNR = \frac{\bar{I}}{\sigma} = \frac{\bar{I}}{\sqrt{\sigma^2}} = \frac{139}{27}$$

| -> Nyquist /Shannon Theorem



- Undersampling loses structures.
- Oversampling waists memory/computation time.

The 'Nyquist /Shannon Theorem' or 'Sampling Theorem' for the digital sampling of analogue signals suggests a Nyquist rate $NR \geq 2v$?

! Diffraction theory calculates lateral NR ~ 20 pixel/ μm (~ 50 nm/pixel) !
... axial NR \sim (~ 150 nm/pixel)

PSF: Point Spread Function

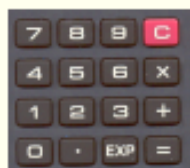
f: Object Function

b: Offset Function

I: Image Matrix

N: Noise Function

$$N(PSF(x, y, z) \otimes f(x, y, z) + b(x, y, z)) = I(x, y, z)$$



Calculator

[Numerical aperture](#)

confocal

widefield

nipkow

4Pi

Select one

[Excitation wavelength](#)

1.3

[Emission wavelength](#)

488 (nm)

[Number of excitation photons](#)

520 (nm)

[Backprojected pinhole radius](#)

1

[B.P. distance between pinholes](#)

250 (nm)

[Lens medium refractive index](#)

2.53 Only for Nipkow disks (μm)

[Specimen medium refractive index](#)

1.515

[Acquisition depth](#)

1.45

Calculate also PSF

0 (μm)

PSF: Point Spread Function

f: Object Function

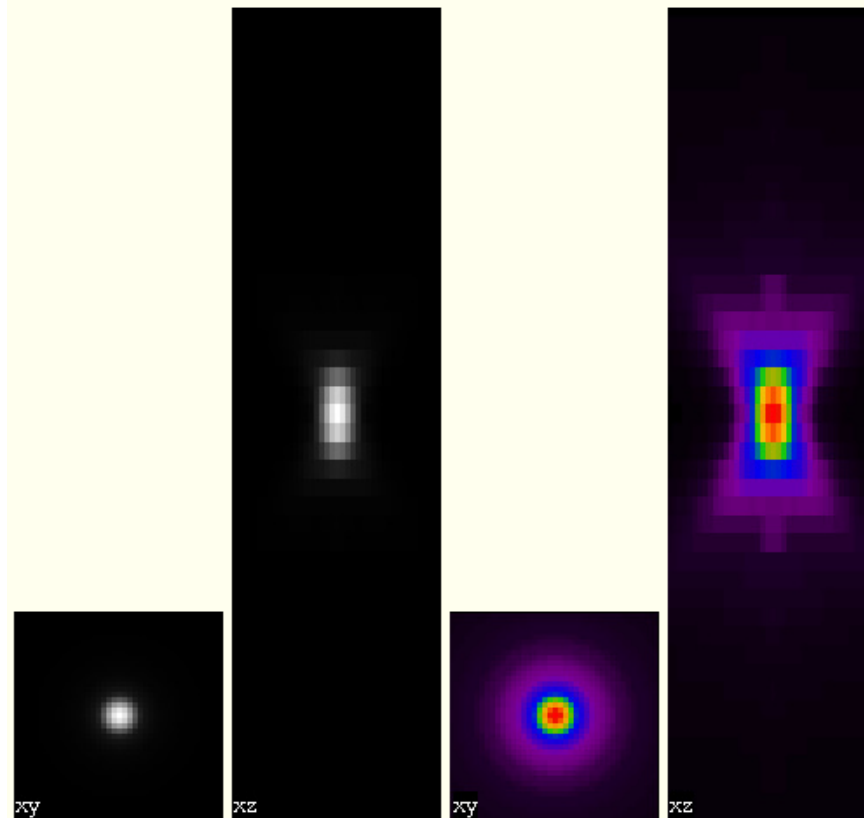
b: Offset Function

I: Image Matrix

N: Noise Function

$$N(PSF(x, y, z) \otimes f(x, y, z) + b(x, y, z)) = I(x, y, z)$$

Nyquist sampling (x,y,z in nm): 46, 46, 165

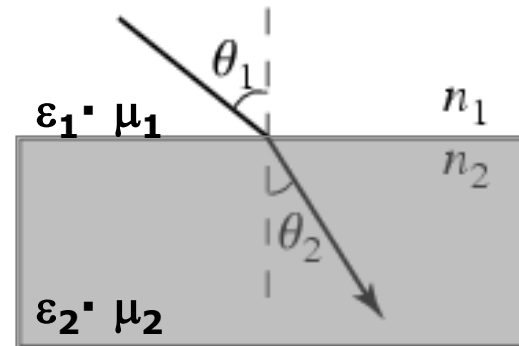


Index of refraction: $n = (\epsilon \cdot \mu)^{1/2} = c/v$,
 ϵ electric permittivity and μ magnetic permeability.

Snell's Law:

$$\sin \theta_1 n_1 = \sin \theta_2 n_2$$

- 1.518 [Zeiss Oil]
- 1.33 [Water]
- 1.0008 [Air]



Refractive Index:

$$RI = n_1/n_2 = v_2/v_1$$

Snell's Law:

$$\sin\theta_1 n_1 = \sin\theta_2 n_2$$

$$n = n(\lambda) !$$

- **1.518 [Zeiss]**
- **1.33 [Water]**
- **1.0008 [Air]**

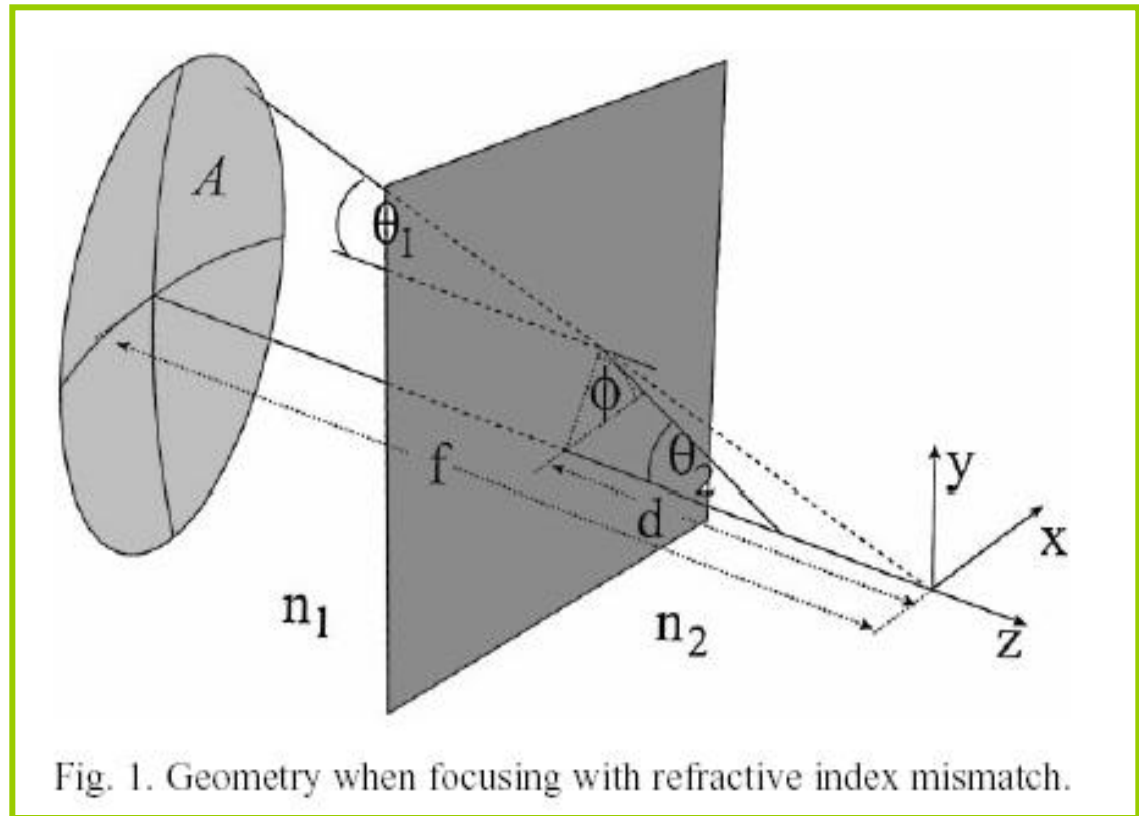
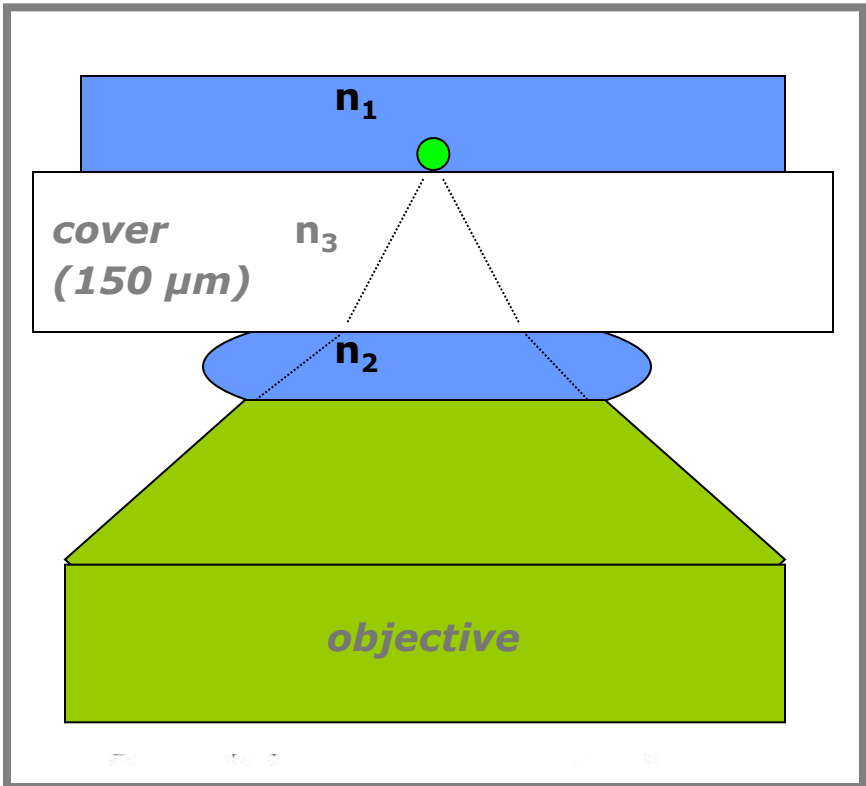


Fig. 1. Geometry when focusing with refractive index mismatch.

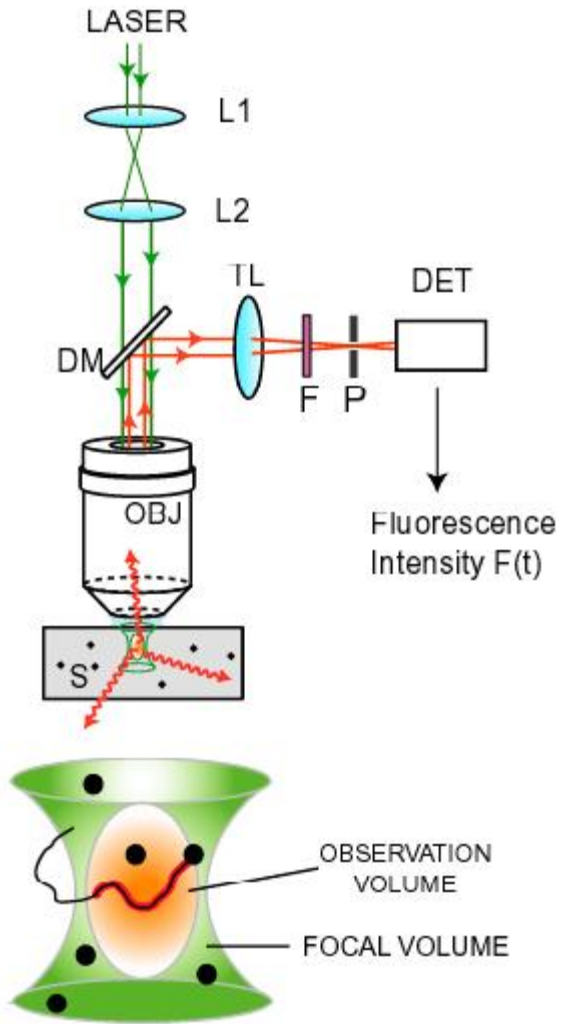
(Egner et al 1998)

● **Micro-esfera: $\varnothing = 6 \mu\text{m}$**



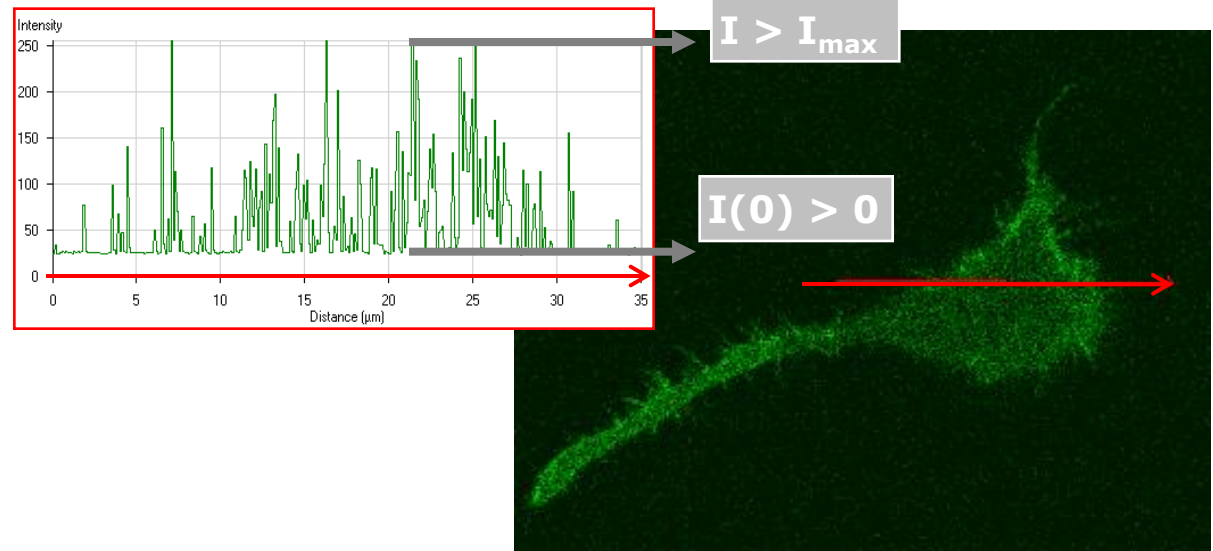
agua/aceite -- *aceite/aceite*
 $n_1 \neq n_2$ $n_1 = n_2$

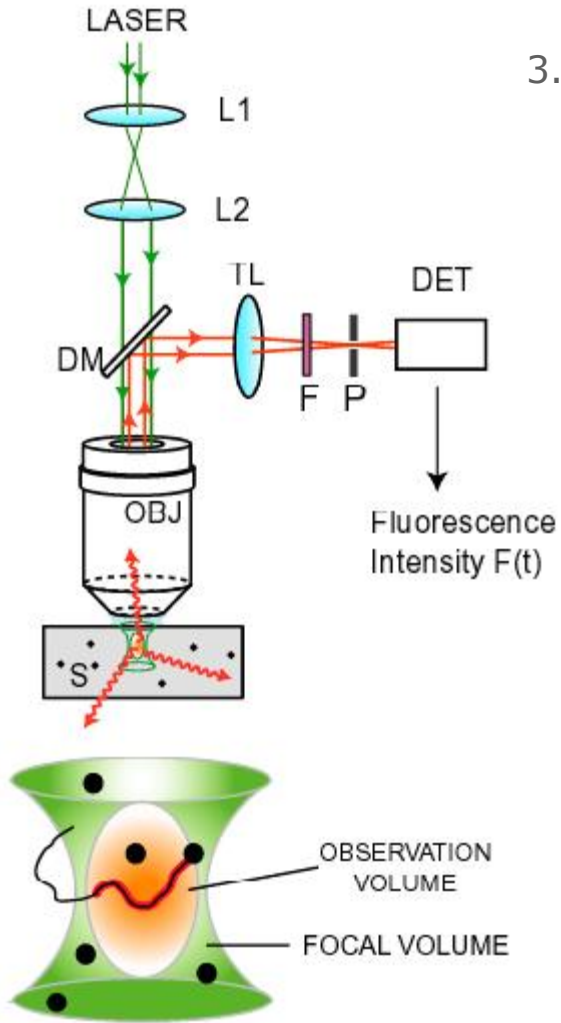
Ley de Snell: $n_i \cdot \sin\theta_i = n_k \cdot \sin\theta_k$
 $n = n(\lambda) !$



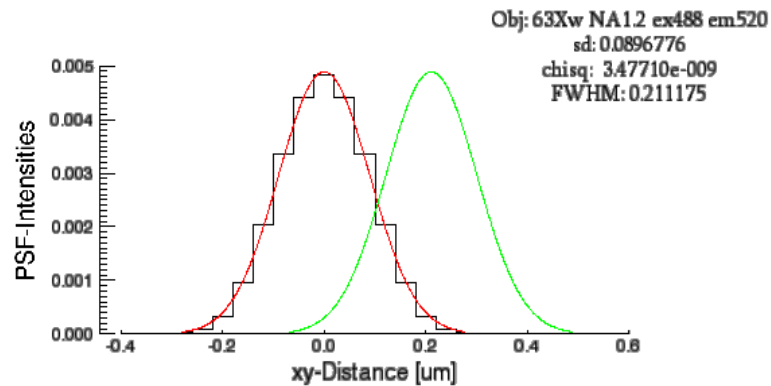
The observation volume (femtoliter) defined by the Point Spread Function must be considered as a mini-spectrofluorimeter.

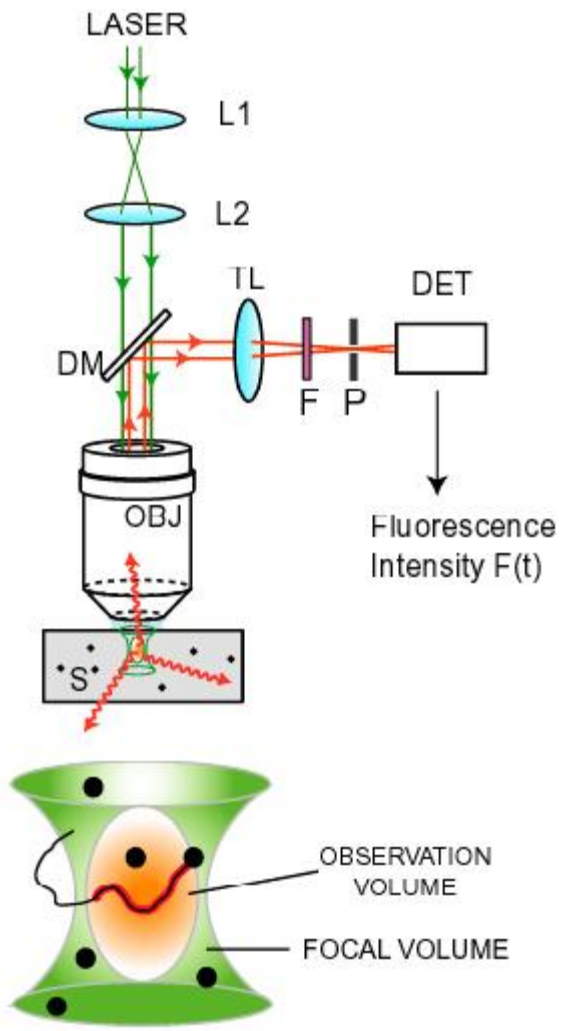
1. You need to consider the Offset $I(0)$ in order to calibrate your signal $I(0) \geq 0$!
2. Never saturate the signal: $I \leq I_{\max}$ (255 for 8 bit) !





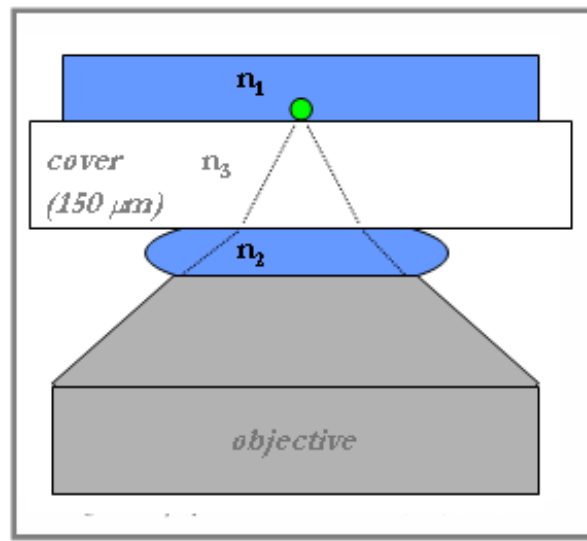
- You need to consider sampling distances in Δx and $\Delta y \approx 50$ nm and $\Delta z \approx 150-300$ nm for later deconvolution, or calculate the explicit sample distances @ <http://support.svi.nl/wiki/NyquistCalculator>





4. Use the right immersion setup !
- $n_1 = n_2$!
- Keep refractive index / index of refraction constant !

● Micro-esfera: $\varnothing = 6 \mu\text{m}$



agua/aceite -- aceite/aceite
 $n_1 \neq n_2$ $n_1 = n_2$
 Ley de Snell: $n_i \cdot \sin\theta_i = n_k \cdot \sin\theta_k$
 $n = n(\lambda)$!